

A plug-and-play framework for curvilinear structure segmentation based on a learned reconnecting regularization

S. Carneiro Esteves, Antoine Vacavant and Odysée Merveille



1. Context

2. Proposed method

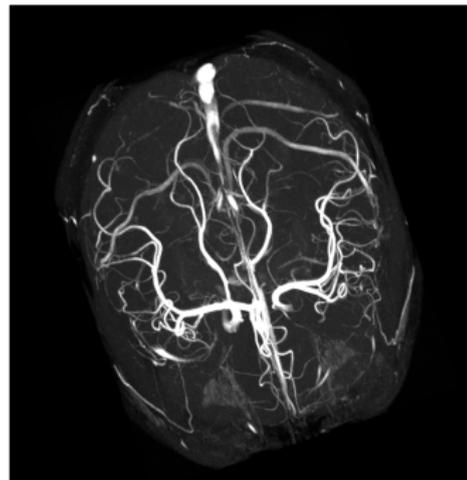
3. Experiences

4. Conclusion and perspectives

Context

Cardiovascular diseases : leading cause of death in the world according to the World Health Organization

→ Visualization of vascular structures *via* angiographic images

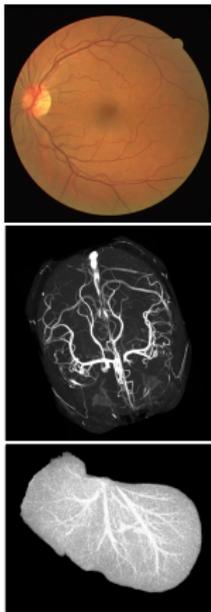


MRI-TOF of the brain

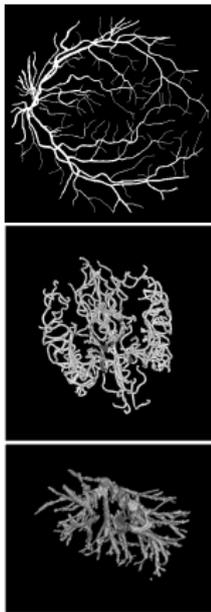
Vascular Network Analysis Importance

- ▶ Improvement in diagnosis and management of diseases
- ▶ Providing tools for visualization and treatment

Context



*Angiographic
images*



*Manual
segmentation*

Need for precise localization
of the vascular network

Segmentation of the vascular
structure from angiographic
images

Structures difficult to
segment

Automatic segmentation methods

Automatic segmentation methods

| Approach | |
|-----------------------------|--|
| Classical | |
| Supervised Deep learning | |

Automatic segmentation methods

| Approach | Global Quality |
|-----------------------------|----------------|
| Classical | - |
| Supervised Deep learning | + |

Automatic segmentation methods

| Approach | Global Quality | Capacity to Generalize |
|-----------------------------|----------------|------------------------|
| Classical | - | + |
| Supervised Deep learning | + | - |

Hybrid methods

- ▶ Bridging Classical and Deep Learning approaches
- ▶ Taking advantages of both approaches

Hybrid methods based on the variational approach

Variational approach definition

$$u^* = \underset{u}{\operatorname{Argmin}} D(u, f) + \lambda R(u)$$

with,

- ▶ $u^* \in \mathbb{R}^n$ the solution image
- ▶ $f \in \mathbb{R}^n$ the initial image
- ▶ $D, R \in \Gamma_0(\mathbb{R}^n)^2$
- ▶ λ the regularization coefficient

$g \in \Gamma_0(\mathbb{R}^n)$ the set of lower semi-continuous , convex et proper functions on \mathbb{R}^n .

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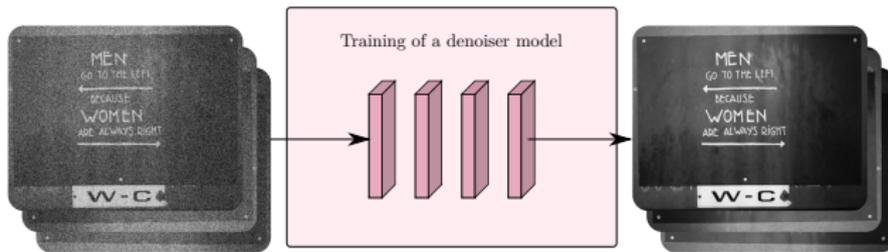
Hybrid methods

- ▶ Replacing R with a learned model
- ▶ Plug the model into the minimization resolution

$g \in \Gamma_0(\mathbb{R}^n)$ the set of lower semi-continuous, convex et proper functions on \mathbb{R}^n .

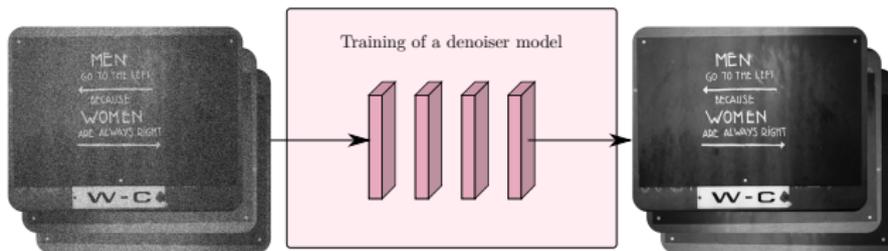
Plug-and-play approach

①

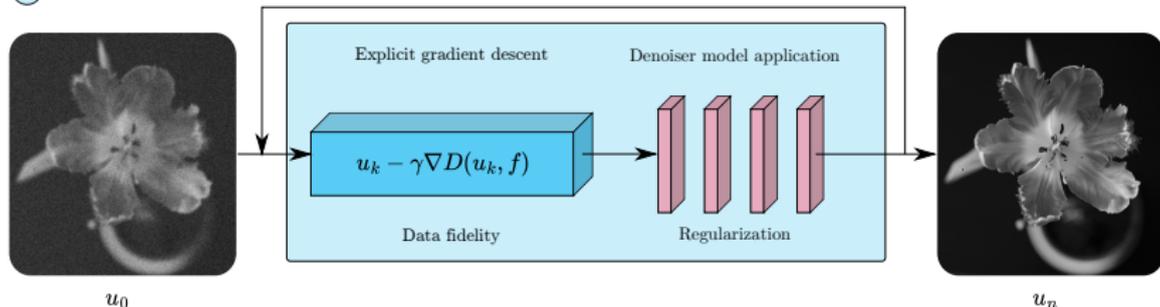


Plug-and-play approach

①



②



No annotation required for main task

Plug-and-play approach

- ▶ Tested on different applications
Demaosaicking, inpainting, deblurring, ...
- ▶ With different resolution algorithms
 HQS^2 , $ADMM^3$, $PDHG^1$, ...
- ▶ Strategies to ensure method convergence ⁴

¹ Meinhardt *et al.* "Learning Proximal Operators: Using Denoising Networks for Regularizing Inverse Imaging Problems", ICCV 2017

² Zhang *et al.* "Learning deep CNN denoiser prior for image restorations", CVPR 2017

³ Le Pendu *et al.* "Preconditioned plug-and-play admm with locally adjustable denoiser for image restoration", SIAM 2023

⁴ Pesquet *et al.* "Learning maximally monotone operators for image recovery.", SIAM 2021

Variational segmentation: Chan model¹

Definition

$$u^* = \underset{u}{\operatorname{argmin}} D(u, f) + \lambda R(u)$$

With :

- ▶ $f \in [0, 1]^n$
- ▶ $u^* \in [0, 1]^n$

c_1 and c_2 foreground and the background constants

¹ Chan *et al.* "Algorithms for finding global minimizers of image segmentation and denoising models", SIAM, 2006.

Variational segmentation: Chan model¹

Definition

$$u^* = \operatorname{argmin}_{u \in [0,1]^n} \langle c, u \rangle_F + \lambda TV(u)$$

With :

- ▶ $f \in [0, 1]^n$
- ▶ $u^* \in [0, 1]^n$
- ▶ $c = (c_1 - f_j)^2 - (c_2 - f_j)^2$
- ▶ $TV(u) = \|\nabla u\|_{2,1}$

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- ▶ $TV(u) = \|\nabla u\|_{2,1}$

Problem reformulation

$$u^* = \underset{u}{\operatorname{argmin}} \langle c, u \rangle_F + \lambda TV(u) + \iota_{[0,1]^n}(u) \quad \iota_{[0,1]^n}(u) = \begin{cases} 0 & \text{if } x \in [0, 1] \\ +\infty & \text{otherwise} \end{cases}$$

c_1 and c_2 foreground and the background constants

¹ Chan *et al.* "Algorithms for finding global minimizers of image segmentation and denoising models", SIAM, 2006.

Primal-Dual method

$$u^* = \underset{u}{\operatorname{argmin}} D(u, f) + g(Lu) + k(u)$$

$$- D(u) = \langle u, c_f \rangle_F$$

$$- k(u) = \iota_{[0,1]^n}$$

$$- g(\cdot) = \lambda \|\cdot\|_{2,1}$$

$$- L = \nabla$$

Resolution:

$$u_{i+1} = \operatorname{prox}_{\tau k}(u_i - \tau(\nabla D(u_i) + L^T v_i))$$

$$v_{i+1} = \operatorname{prox}_{\sigma g^*}(v_i + \sigma L(2u_{i+1} - u_i))$$

τ, σ the gradient descent step sizes

Condat L. " A primal-dual splitting method for convex optimization involving lipschitzian, proximable and linear composite terms", Journal of Opt. Theory and Applications, 2013.

Variational segmentation of vascular structures

→ TV^1 tend to make thin structures disappeared

¹ Rudin *et al.* "Nonlinear total variation based noise removal algorithms", Physica D: Nonlinear Phenomena, 1992

² Merveille *et al.* "nD variational restoration of curvilinear structures with prior-based directional regularization",

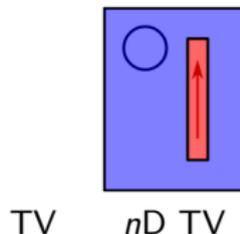
Variational segmentation of vascular structures

→ TV^1 tend to make thin structures disappeared

nD directional TV^2

$$R(u) = || \nabla_m u ||_{2,1},$$

$$\nabla_m u = \bar{\mathcal{V}}(f) \nabla_d u + (1 - \bar{\mathcal{V}}(f)) \nabla u,$$



- ▶ $\bar{\mathcal{V}}$ a prior on the presence of tubular structures
- ▶ ∇_d the directional gradient

Estimation of structures direction thanks to the prior in order to integrate it in the gradient computation

¹ Rudin *et al.* "Nonlinear total variation based noise removal algorithms", Physica D: Nonlinear Phenomena, 1992

² Merveille *et al.* "nD variational restoration of curvilinear structures with prior-based directional regularization",

Variational segmentation of vascular structures

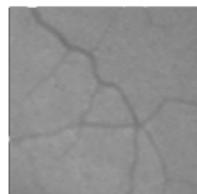
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Image



Groundtruth



TV



nD TV

¹ Rudin *et al.* "Nonlinear total variation based noise removal algorithms", Physica D: Nonlinear Phenomena, 1992

² Merveille *et al.* "nD variational restoration of curvilinear structures with prior-based directional regularization",

Variational segmentation of vascular structures

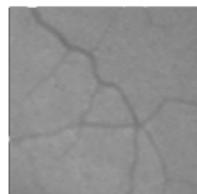
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Image



Groundtruth



TV



nD TV

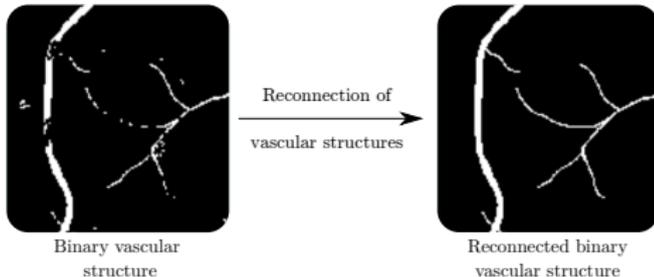
Connectivity is not preserved

¹ Rudin *et al.* "Nonlinear total variation based noise removal algorithms", Physica D: Nonlinear Phenomena, 1992

² Merveille *et al.* "nD variational restoration of curvilinear structures with prior-based directional regularization",

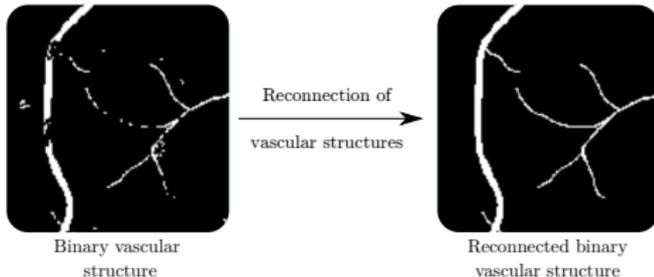
Idea

1. Learn a model that reconnects vascular structures



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1. Learn a model that reconnects vascular structures



2. Plug it into a variational segmentation resolution as a regularization term

1. Context

2. Proposed method

3. Experiences

4. Conclusion and perspectives

Proposed method

What do I need to learn to reconnect vascular structures ?

- ▶ An annotated dataset
- ▶ An architecture to train

Proposed method

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Proposed method

What do I need to learn to reconnect vascular structures ?

- ▶ **An annotated dataset**
- ▶ An architecture to train

Dataset creation

- ▶ Easy to disconnect
 - ▶ Independant toward the modality
- **Use of binary structures**

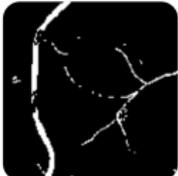
Proposed method

① Dataset creation



Binary curvilinear structure

Disconnection
→
generation



Disconnected binary curvilinear structure

Proposed method

① Dataset creation



Binary curvilinear structure

Disconnection
generation

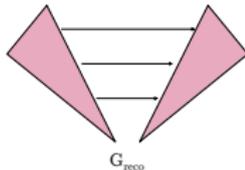


Disconnected binary curvilinear structure

② Reconnecting regularization term learning



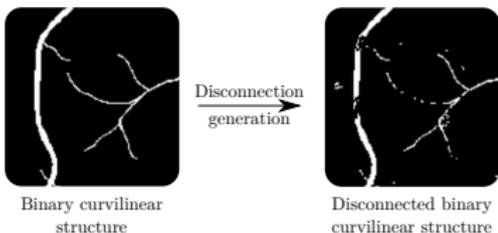
Disconnected binary curvilinear structure



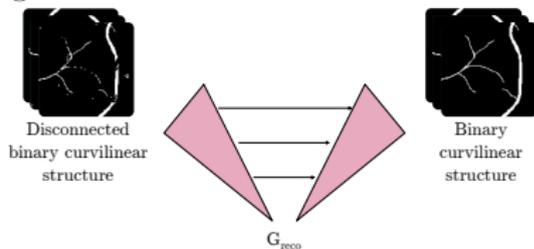
Binary curvilinear structure

Proposed method

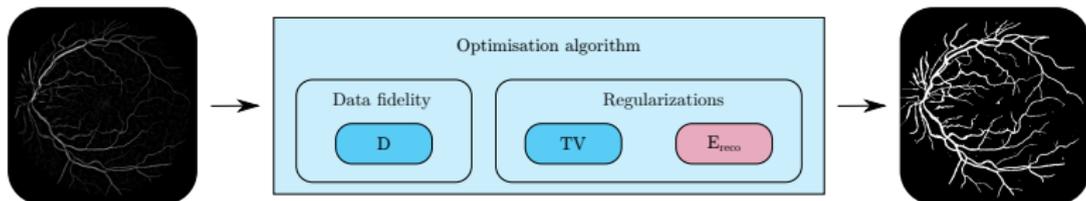
1 Dataset creation



2 Reconnecting regularization term learning

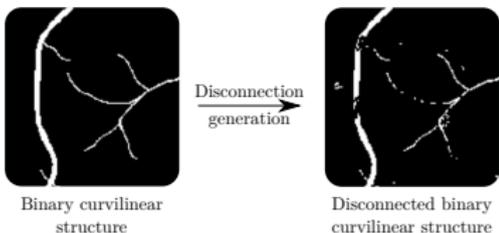


3 Plug and play segmentation

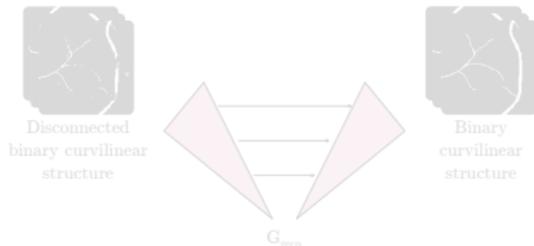


Proposed method

1 Dataset creation



2 Reconnecting regularization term learning



3 Plug and play segmentation



1. Dataset creation

Observations

Segmentations



Groundtruth



1. Dataset creation

Observations



Hypothesis

- ▶ The thinner the vessel, the more likely it is to become disconnected
- ▶ The thinner the vessel, the bigger the disconnection
- ▶ Artefact presence

1. Dataset creation

Inputs of the algorithm

1. Dataset creation

Inputs of the algorithm

- ▶ A binary vascular structure:
 - ▶ A manual annotation
 - ▶ A synthetic vascular tree

1. Dataset creation

Inputs of the algorithm

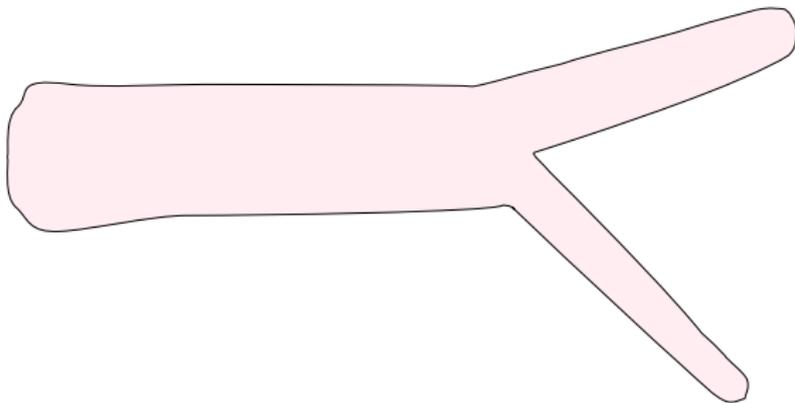
- ▶ A binary vascular structure:
 - ▶ A manual annotation
 - ▶ A synthetic vascular tree
- ▶ The number of disconnections to create

1. Dataset creation

Inputs of the algorithm

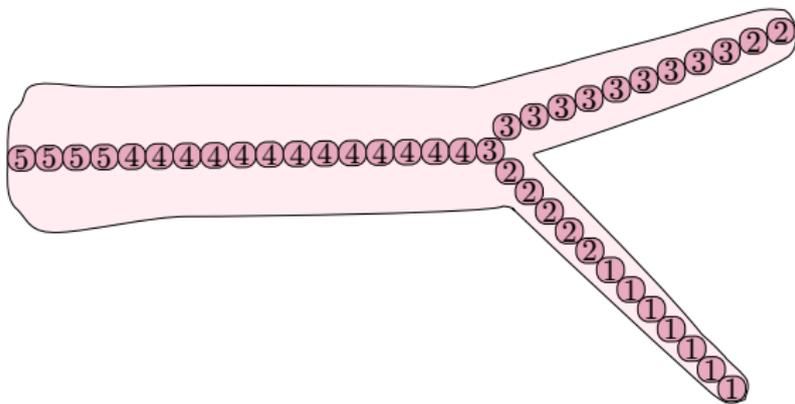
- ▶ A binary vascular structure:
 - ▶ A manual annotation
 - ▶ A synthetic vascular tree
- ▶ The number of disconnections to create
- ▶ The mean size s of disconnections

1. Dataset creation



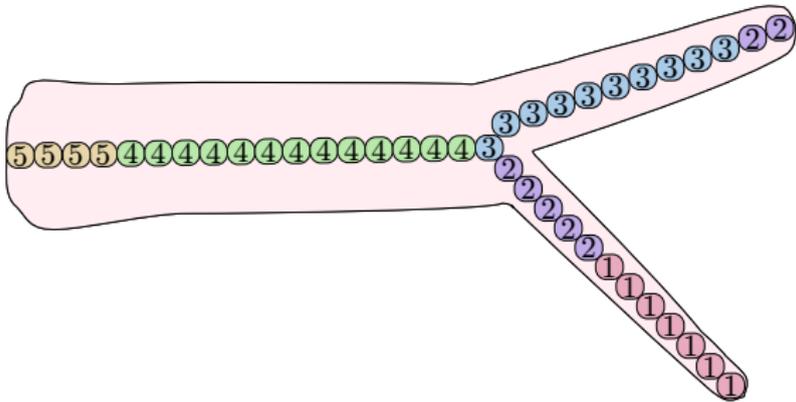
Binary vascular structure

1. Dataset creation



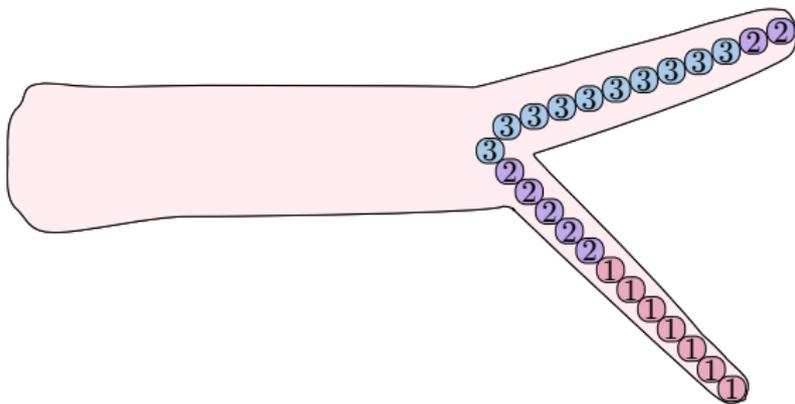
Extraction of the structure radius on the centerlines

1. Dataset creation



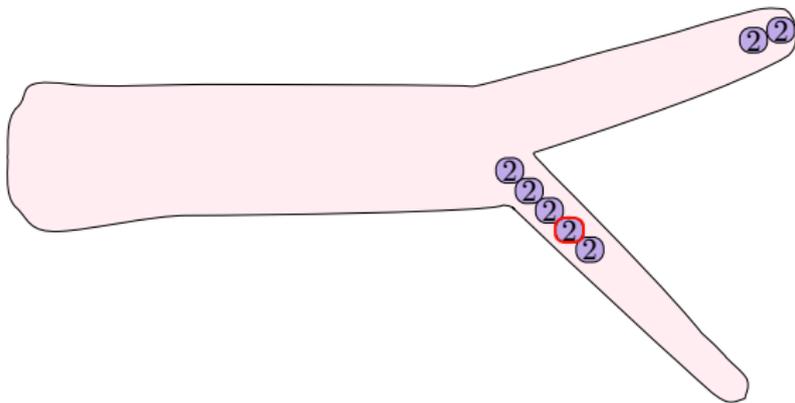
Classification of each centerline pixel in m classes in function of their radius

1. Dataset creation



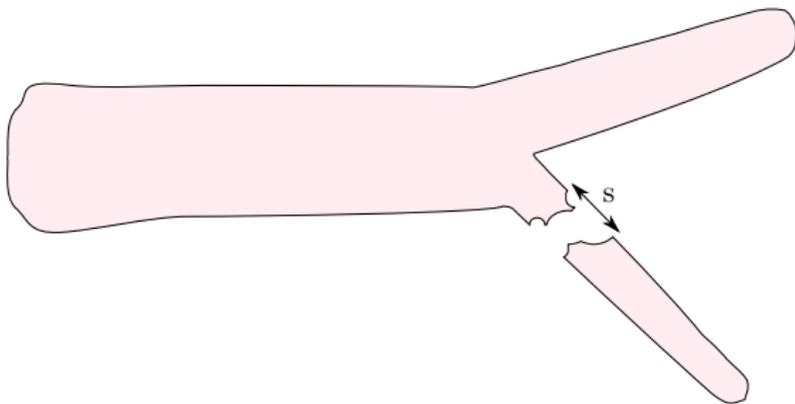
Selection of 3 classes with the thinnest structures

1. Dataset creation



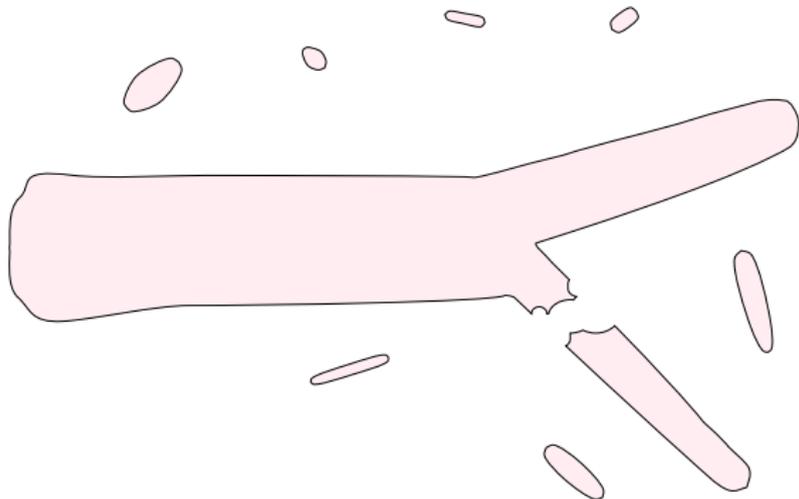
Draw a class and then a pixel from the centerline to select the center of a disconnection

1. Dataset creation



Disconnect the structure at the selected pixel

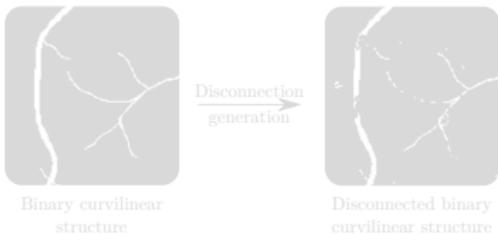
1. Dataset creation



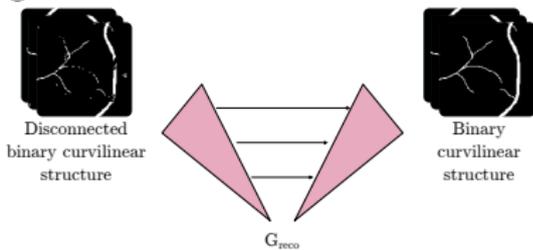
Add fragments

Proposed method

① Dataset creation



② Reconnecting regularization term learning



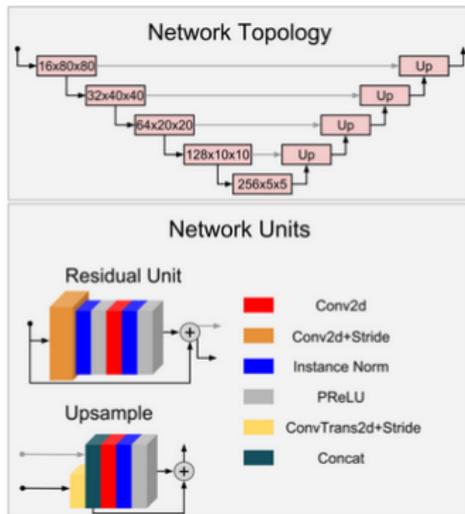
③ Plug and play segmentation



2. Reconnecting regularization term learning

Model architecture: Residual U-Net¹

- ▶ Reconnection of binary vascular structures similar to segmentation task
- ▶ U-Net architecture : the gold standard for biomedical image segmentation



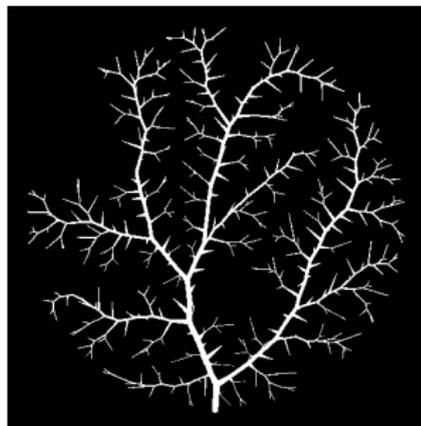
Residual U-Net architecture

¹ Kerfoot *et al.* " Left-ventricle quantification using residual u-net", International Workshop on Statistical Atlases and Computational Models of the Heart, 2018

2. Reconnecting regularization term learning

Loss function:

- ▶ Unbalanced classes (background, structure)

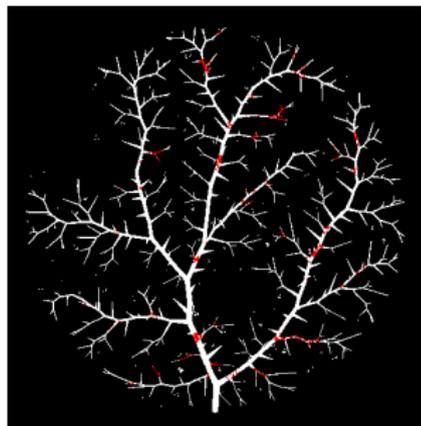


Example of a connected vascular structure

2. Reconnecting regularization term learning

Loss function:

- ▶ Unbalanced classes (background, structure)
- ▶ Fragments : small part of the vascular structure (6% of the structure in 2D)

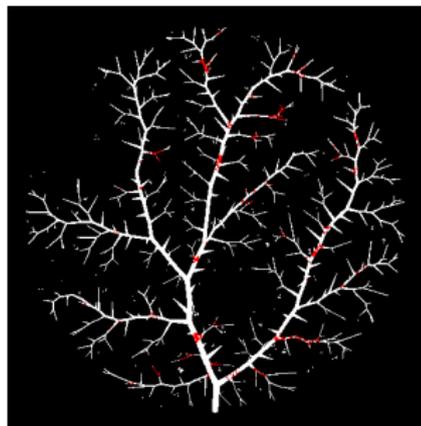


Example of a structure with the disconnections highlighted

2. Reconnecting regularization term learning

Loss function:

- ▶ Unbalanced classes (background, structure)
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Example of a structure with the disconnections highlighted

Dice loss not adapted

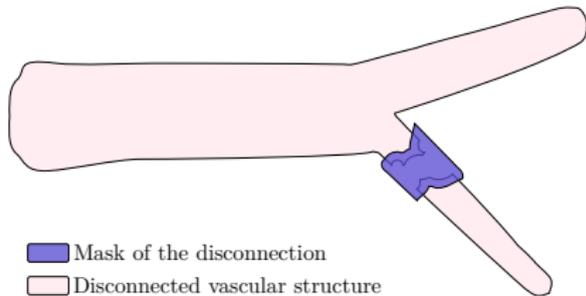
2. Reconnecting regularization term learning

Proposed Dice loss :

$$\mathcal{L}(x, y) = \mathcal{D}(x, y) + \mathcal{D}(x, y; M),$$

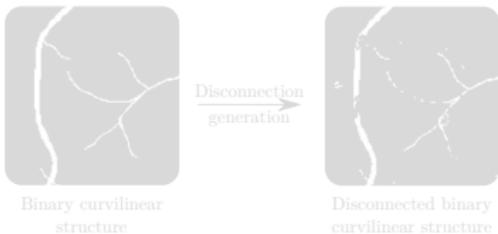
avec :

- ▶ $x \in [0, 1]^n$ a disconnected image composed of n pixels
- ▶ $y \in \{0, 1\}^n$ its annotation,
- ▶ $M \in \{0, 1\}^n$ the mask containing the missing fragments and their neighbors.

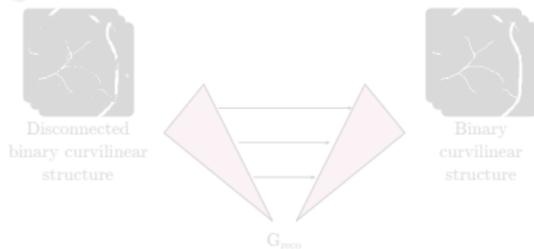


Proposed method

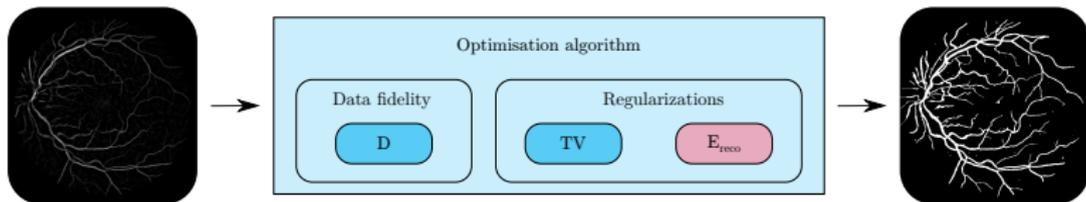
① Dataset creation



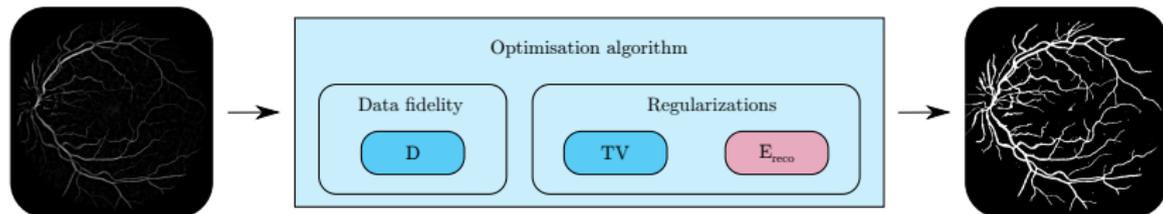
② Reconnecting regularization term learning



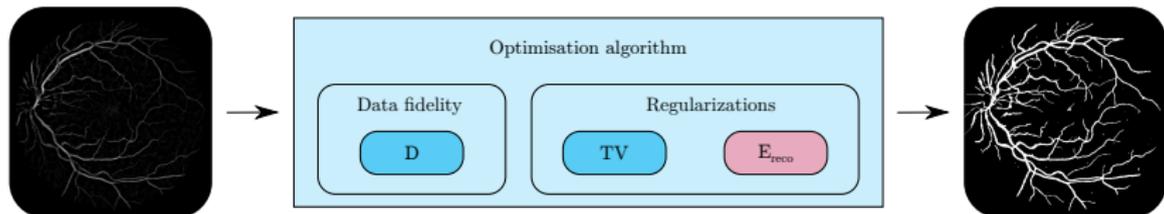
③ Plug and play segmentation



3. Plug and play segmentation



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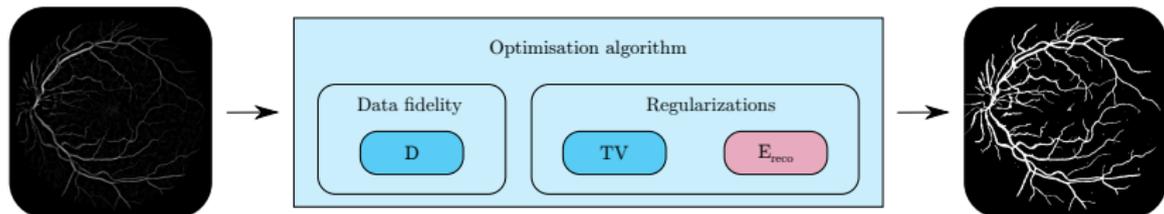


Our model

$$G_{\text{reco}} : \{0, 1\}^n \rightarrow [0, 1]^n$$

Applicable to binary or near-binary
images

3. Plug and play segmentation

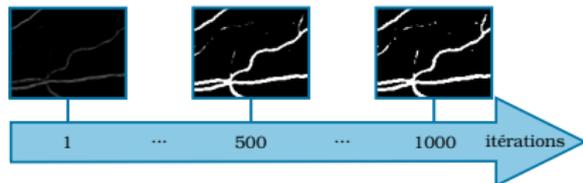


Our model

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Applicable to binary or near-binary images

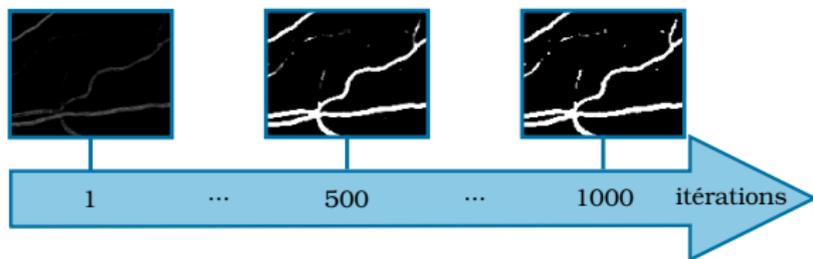
Variational optimisation scheme



u_i evolution through iterations

3. Plug and play segmentation

Variational optimisation scheme



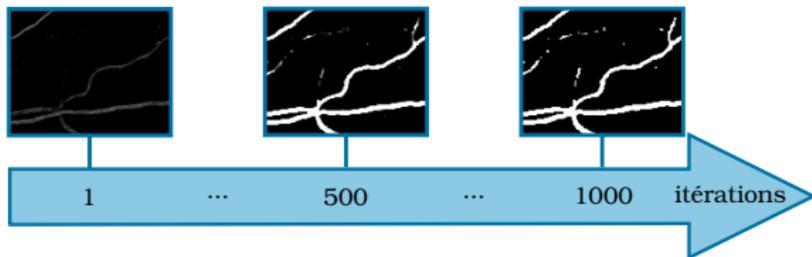
u_i evolution through iterations

$\underset{u}{\text{Argmin}} \langle c, u \rangle_F + \lambda TV(u) + \iota_{[0,1]^n}(u)$ as a first step

$\underset{u}{\text{Argmin}} \langle c, u \rangle_F + \lambda TV(u) + E_{\text{reco}}(u)$ when u is near binary

3. Plug and play segmentation

Variational optimisation scheme



u_i evolution through iterations

$$\underset{u}{\text{Argmin}} \langle c, u \rangle_F + \lambda TV(u) + \iota_{[0,1]^n}(u) \quad \text{if } i < \alpha$$

$$\underset{u}{\text{Argmin}} \langle c, u \rangle_F + \lambda TV(u) + E_{\text{reco}}(u) \quad \text{if } i \geq \alpha$$

3. Plug and play segmentation

Primal-dual algorithm:

$$u_{i+1} = \text{prox}_{\tau k}(u_i - \tau(\nabla D(u_i) + L^T v_i))$$

$$v_{i+1} = \text{prox}_{\sigma g^*}(v_i + \sigma L(2u_{i+1} - u_i))$$

Proposed algorithm :

$$u_{i+1} = \Phi(u_i - \tau(\nabla D(u_i) + L^T v_i))$$

$$v_{i+1} = \text{prox}_{\sigma g^*}(v_i + \sigma L(2u_{i+1} - u_i)),$$

$$\Phi(x) = \begin{cases} \text{prox}_{\iota_{[0,1]^n}}(x) & \text{if } i < \alpha \\ G_{\text{reco}}(P(x)) & \text{otherwise} \end{cases}$$

- ▶ $D(u) = \langle u, c_f \rangle_F$
- ▶ $g(\cdot) = \lambda \|\cdot\|_{2,1}$
- ▶ $L = \nabla$
- ▶ $P(\cdot)$ the projection in the image set
- ▶ α the iteration from which G_{reco} is plugged

1. Context

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4. Conclusion and perspectives

Experiences

Compared methods

- ▶ Chan Model with the TV¹
- ▶ Chan Model with the nD directional TV²
- ▶ Our proposed method combining the Chan model with G_{reco}

→ Optimization of the regularization coefficient for each model

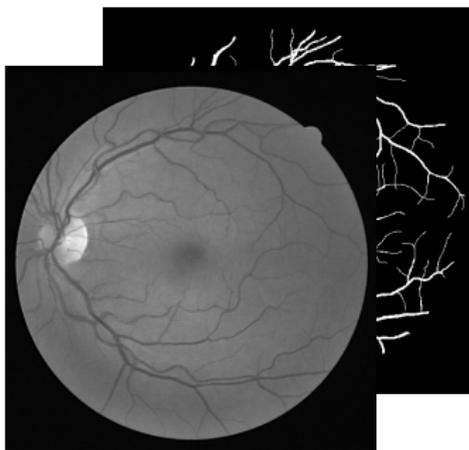
¹ Chan et al. "Algorithms for finding global minimizers of image segmentation and denoising models", SIAM, 2006

² Merveille et al. "nD variational restoration of curvilinear structures with prior-based directional regularization", IEEE TIP, 2019

Datasets

Evaluation Dataset

DRIVE ¹ : 20 retinographies
and their annotations

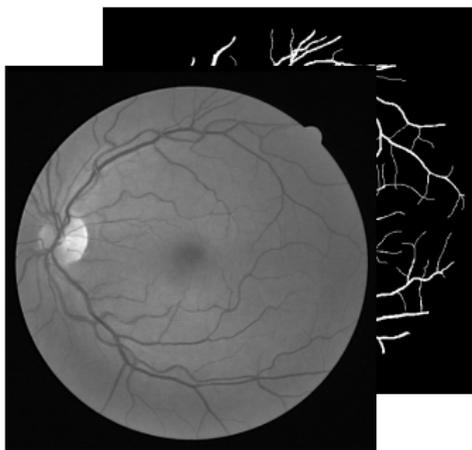


¹ Staal *et al.* "Ridge-based vessel segmentation in color images of the retina", Trans. on Medical Imaging, 2004
² Kerautret *et al.* "OpenCCO: An Implementation of Constrained Constructive Optimization for Generating 2D and 3D Vascular Trees". Image Processing On Line, 2023

Datasets

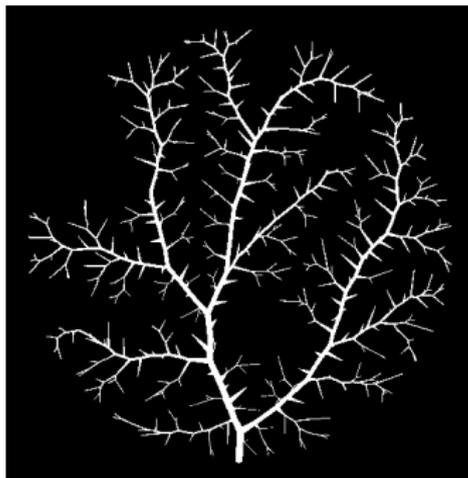
Evaluation Dataset

DRIVE ¹ : 20 retinophotographies
and their annotations



Training Dataset

OpenCCO² : 80 synthetic vascular
trees



¹ Staal *et al.* "Ridge-based vessel segmentation in color images of the retina", Trans. on Medical Imaging, 2004

² Kerautret *et al.* "OpenCCO: An Implementation of Constrained Constructive Optimization for Generating 2D and 3D Vascular Trees". Image Processing On Line, 2023

Quantitative evaluation of vascular segmentations

Matthews correlation coefficient (MCC)

$$MCC = \frac{VP \times VN - FP \times FN}{\sqrt{(VP + FP)(VP + FN)(VN + FP)(VN + FN)}}$$

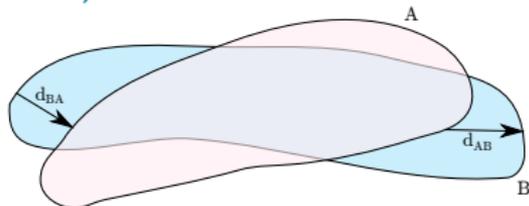
Quantitative evaluation of vascular segmentations

Matthews correlation coefficient (MCC)

$$\text{MCC} = \frac{VP \times VN - FP \times FN}{\sqrt{(VP + FP)(VP + FN)(VN + FP)(VN + FN)}}$$

Average Symmetric Surface Distance (ASSD)

$$\text{ASSD}(A, B) = \frac{\sum d_{AB} + \sum d_{BA}}{|A| + |B|}$$



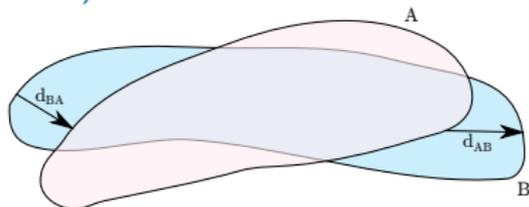
Quantitative evaluation of vascular segmentations

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Average Symmetric Surface Distance (ASSD)

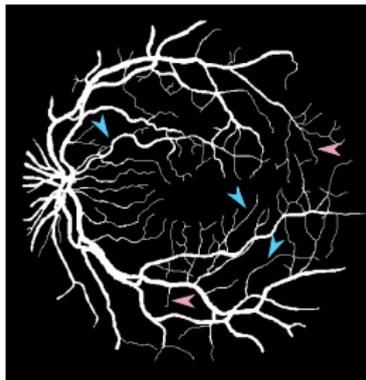
$$\text{ASSD}(A, B) = \frac{\sum d_{AB} + \sum d_{BA}}{|A| + |B|}$$



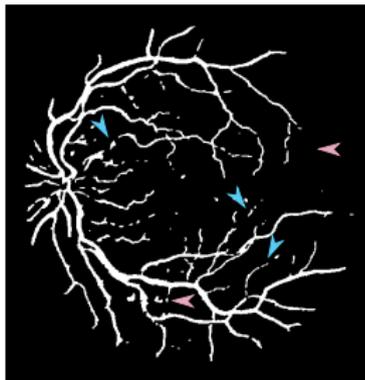
Number of connected components β_0

$$\epsilon_{\beta_0} = \left| \frac{\beta_0 - \beta_{0\text{GT}}}{\beta_{0\text{GT}}} \right|$$

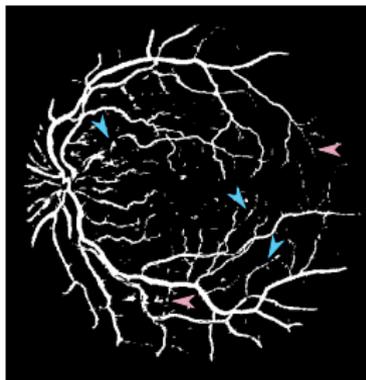
Analysis



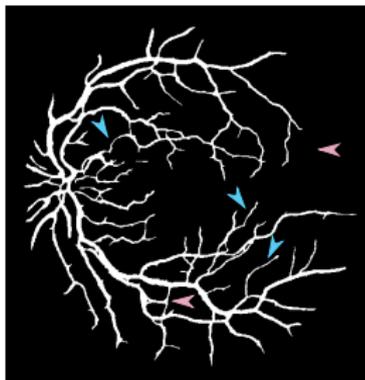
Groundtruth



TV



Directional TV

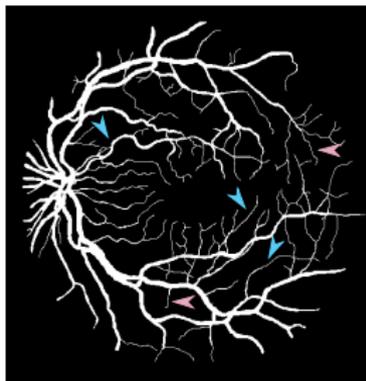


Proposed method

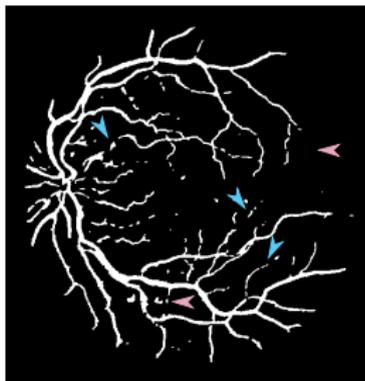
| | MCC ↑ | ASSD ↓ | ϵ_{β_0} ↓ |
|------------------------|-------------------------|--------------------|-------------------------|
| TV | 0.732 ± 0.026 | 2.017 ± 0.452 | 22.668 ± 15.203 |
| nD TV | 0.733 ± 0.026 | 1.896 ± 0.497 | 23.458 ± 17.921 |
| $G_{\text{reco, CCO}}$ | 0.742 ± 0.023 | 2.386 ± 0.0.627 | 2.325 ± 2.274 |

- ▶ Better structure detection
- ▶ A better-connected structure

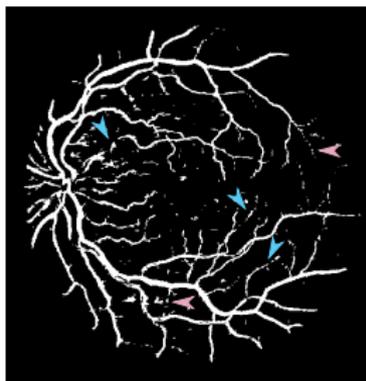
Analysis



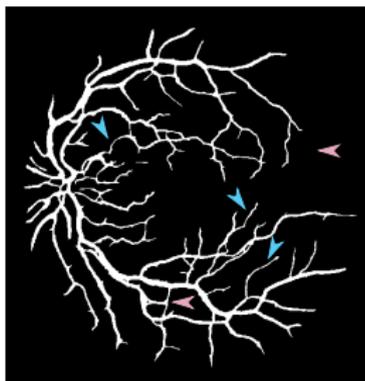
Groundtruth



TV



Directional TV



Proposed method

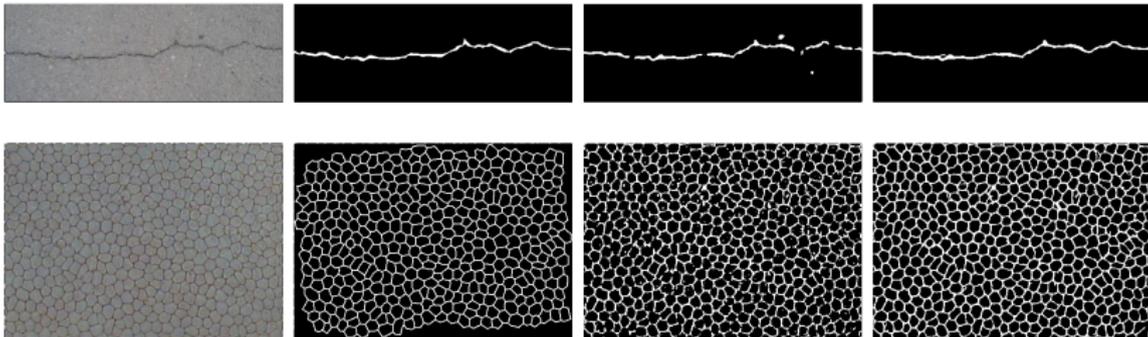
| | MCC \uparrow | ASSD \downarrow | ϵ_{β_0} \downarrow |
|------------------------|-----------------------------|-----------------------------|-----------------------------------|
| TV | 0.732 ± 0.026 | 2.017 ± 0.452 | 22.668 ± 15.203 |
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- ▶ Better structure detection
- ▶ A better-connected structure
- ▶ Disappearance of certain vascular fragments.

Generalization

Plug and play segmentation with G_{reco} trained on OpenCCO on two datasets containing curvilinear structures :

- ▶ Road cracks
- ▶ Cells from the corneas of pigs' eyes



(a) Original image

(b) Groundtruth

(c) TV

(d) Our method

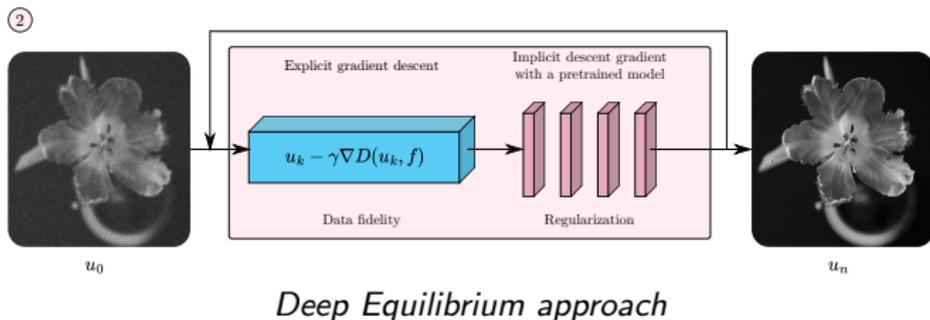
1. Context
2. Proposed method
3. Experiences
4. Conclusion and perspectives

Conclusion

- ▶ Development of a plug-and-play segmentation method
 - ▶ Unsupervised and generalizable
 - ▶ Connectivity preservation

Limits and perspectives

- ▶ No convergence assurance
Idea : Learn a maximally monotone operator¹
- ▶ Injecting the reconstructor model from an iteration α
Idea : adopt a Deep Equilibrium approach²



¹ Pesquet *et al.* "Learning maximally monotone operators for image recovery.", SIAM 2021

² Gilton *et al.* "Deep equilibrium architectures for inverse problems in imaging", IEEE Trans. on Computational Imaging, 2021

Thank you !