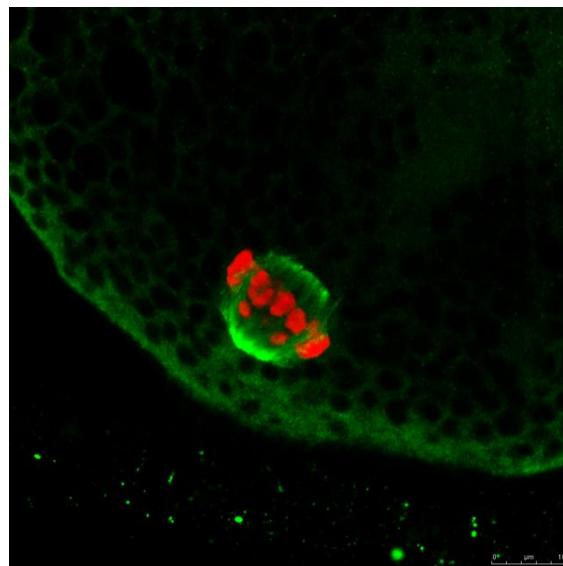
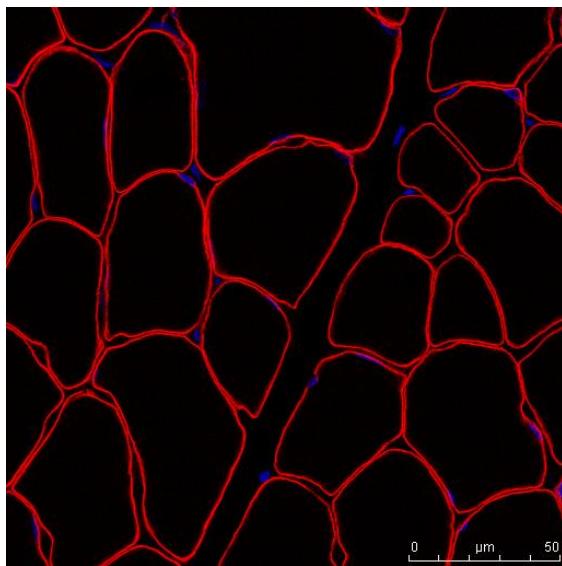




Microscopie confocale - 2010

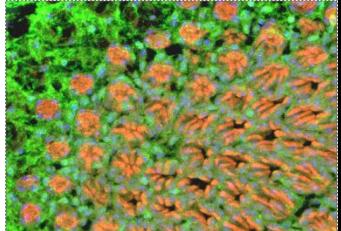


Microscopie Confocale

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Historique

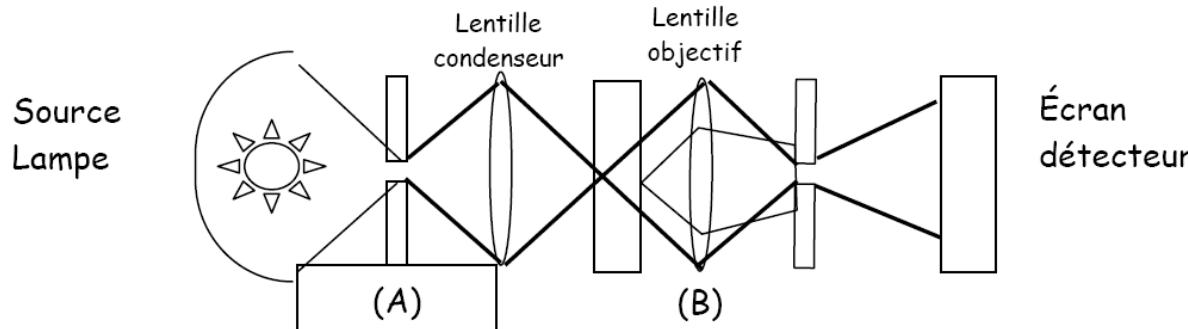
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XVII : naissance de la microscopie photonique (découverte d'agents pathogènes : tuberculose, peste..)

1957 : Naissance de la microscopie confocale avec Marvin Minsky

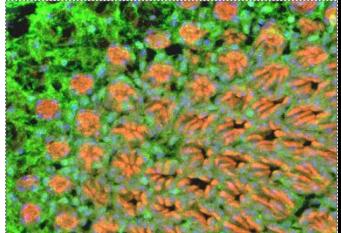


conjuguer le plan de la source lumineuse et celui de l'image filtrée



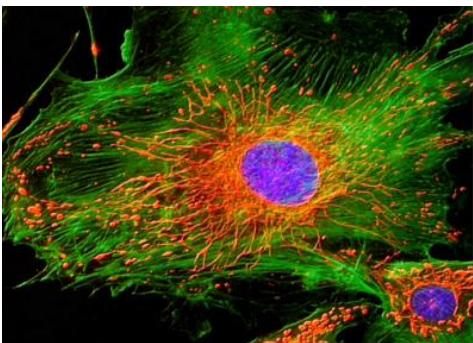
1980 : Émergence de la microscopie confocale

besoins en biologie cellulaire + progrès technologiques (source laser, développement de l'électronique, informatique...)



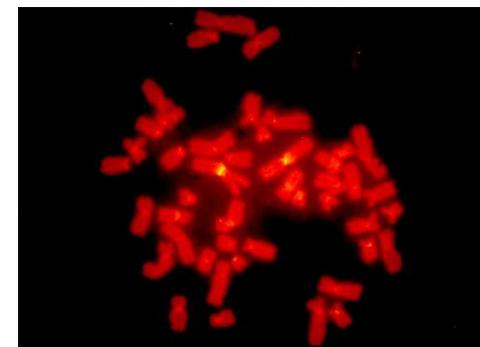
Historique

Structures

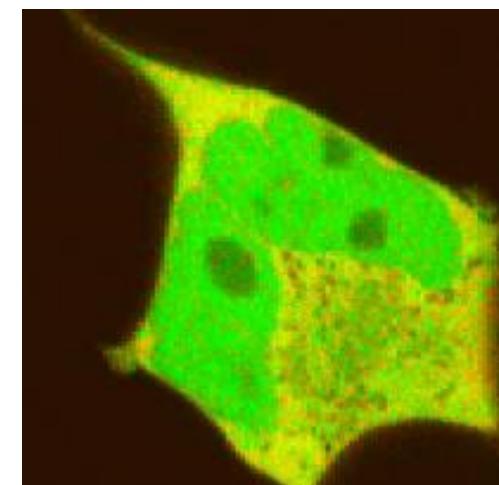
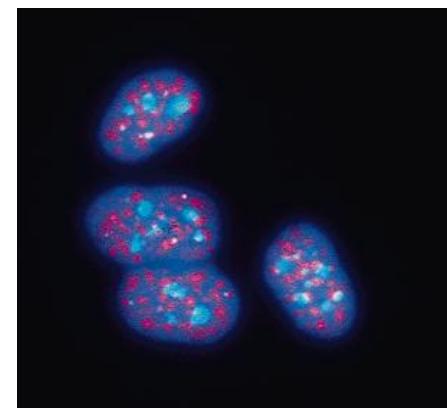
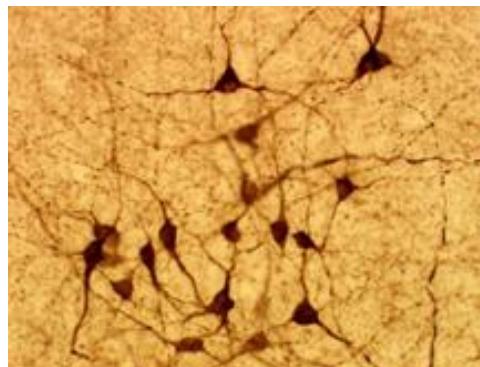
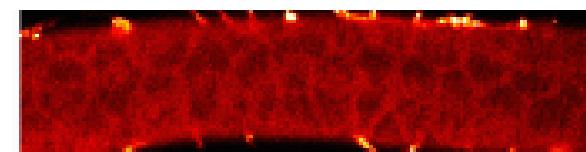


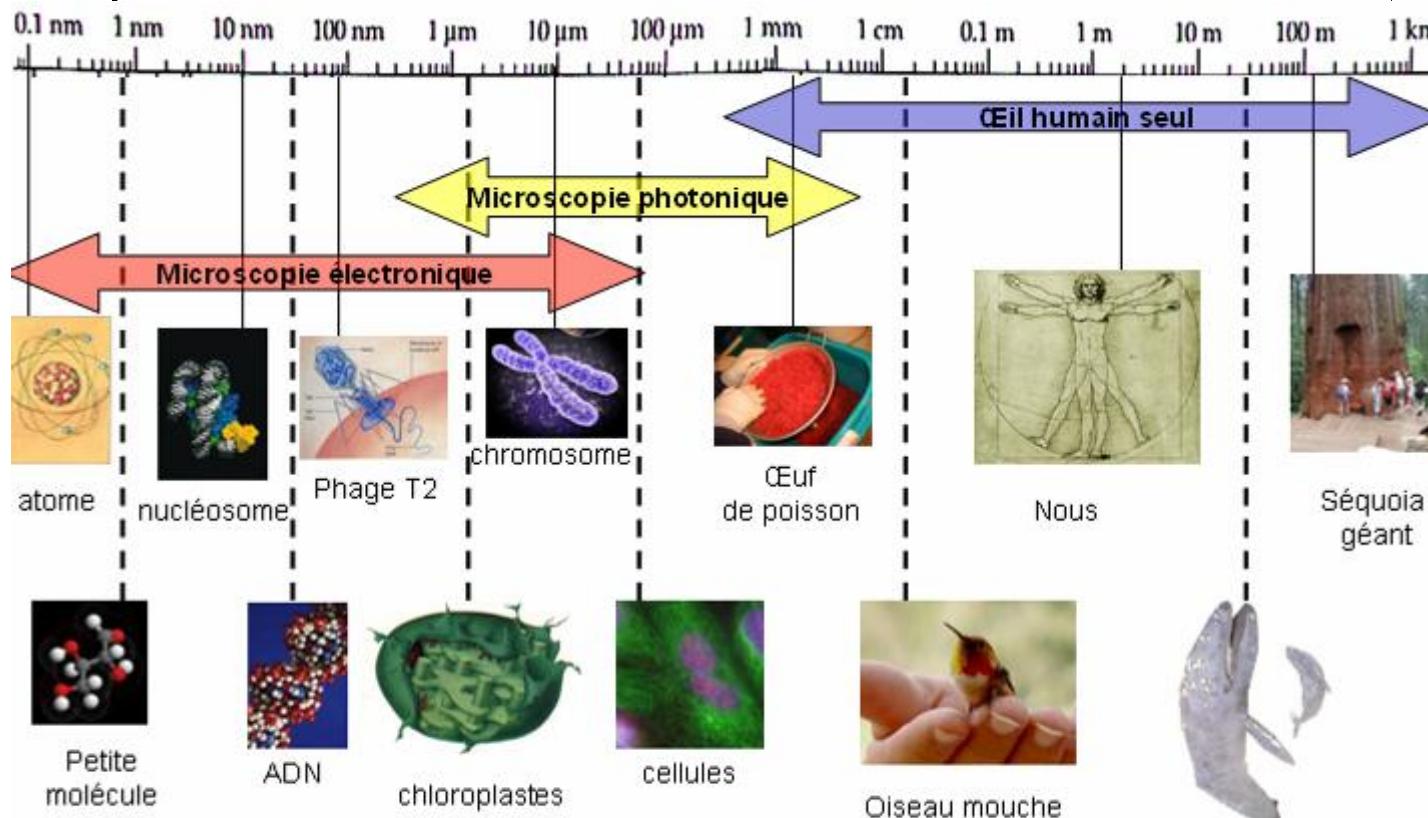
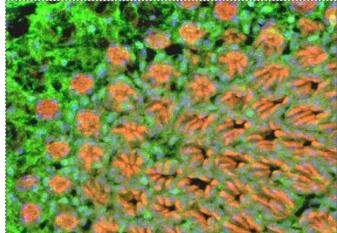
Question biologique ?

Localisations



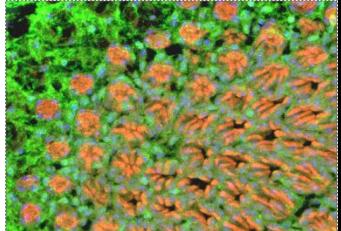
dynamiques





NECESSITE

- Grossissement: voir des petits détails
- Résolution : pouvoir distinguer 2 éléments très proches
- Contraste : possibilité de distinguer un élément d'un autre



Historique

- **Microscopes de fluorescence à champ large**
(Wide field fluorescence microscopes)

Capteurs CCD à haute résolution et sensibilité

Déconvolution possible pour éliminer les signaux hors plan focal
Fondamentale, video-microscopie rapide

- **Microscopes confocaux à balayage laser**
(Confocal laser scanning microscopes)

Détecteurs : photomultiplicateurs

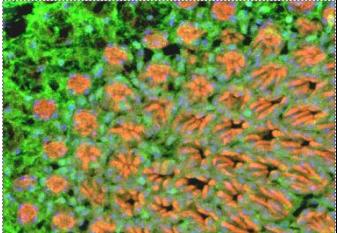
Diaphragme (pinhole) confocal pour sélectionner la fluorescence émise dans le plan focal, colocalisation, **3D**

- **Microscopes à balayage laser et excitation bi- (multi-) photonique**
(Two- (or multi-) photon laser scanning microscopes)

Avantages : excitation restreinte au volume focal, résolution temporelle

Microscopie Confocale

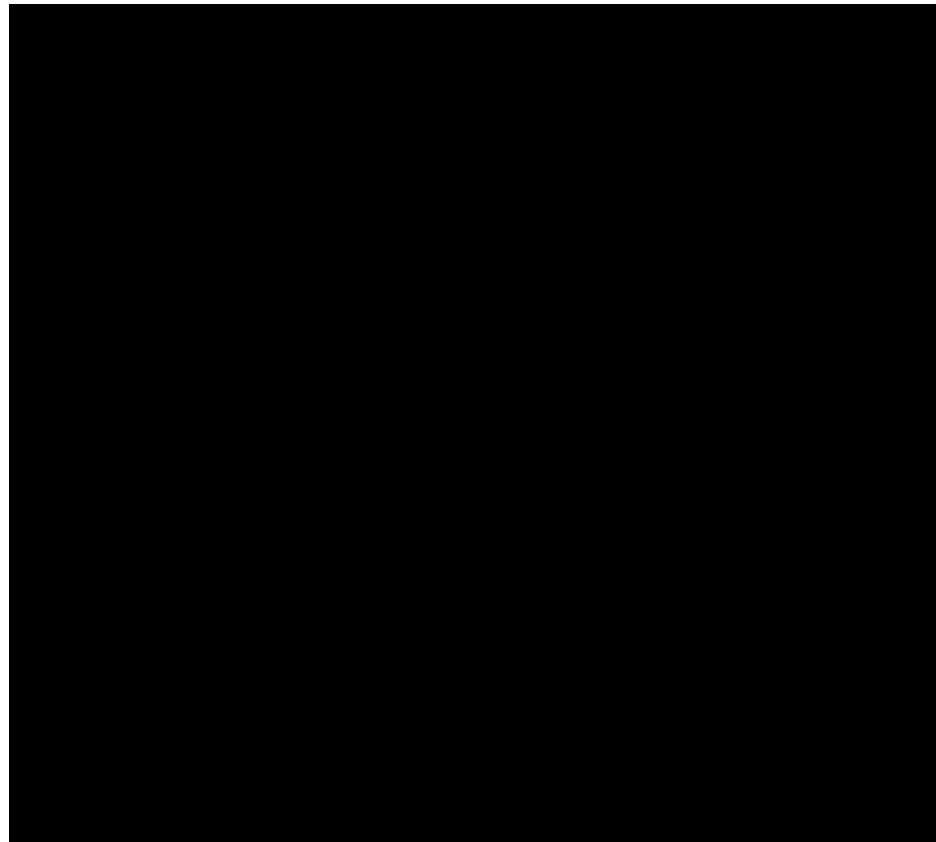
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Fluorescence

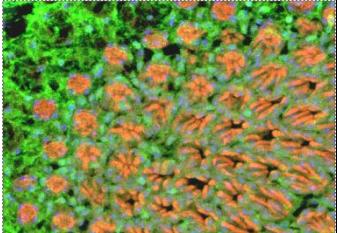
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Principe d'excitation / émission



$$E = h\nu = hc/\lambda$$

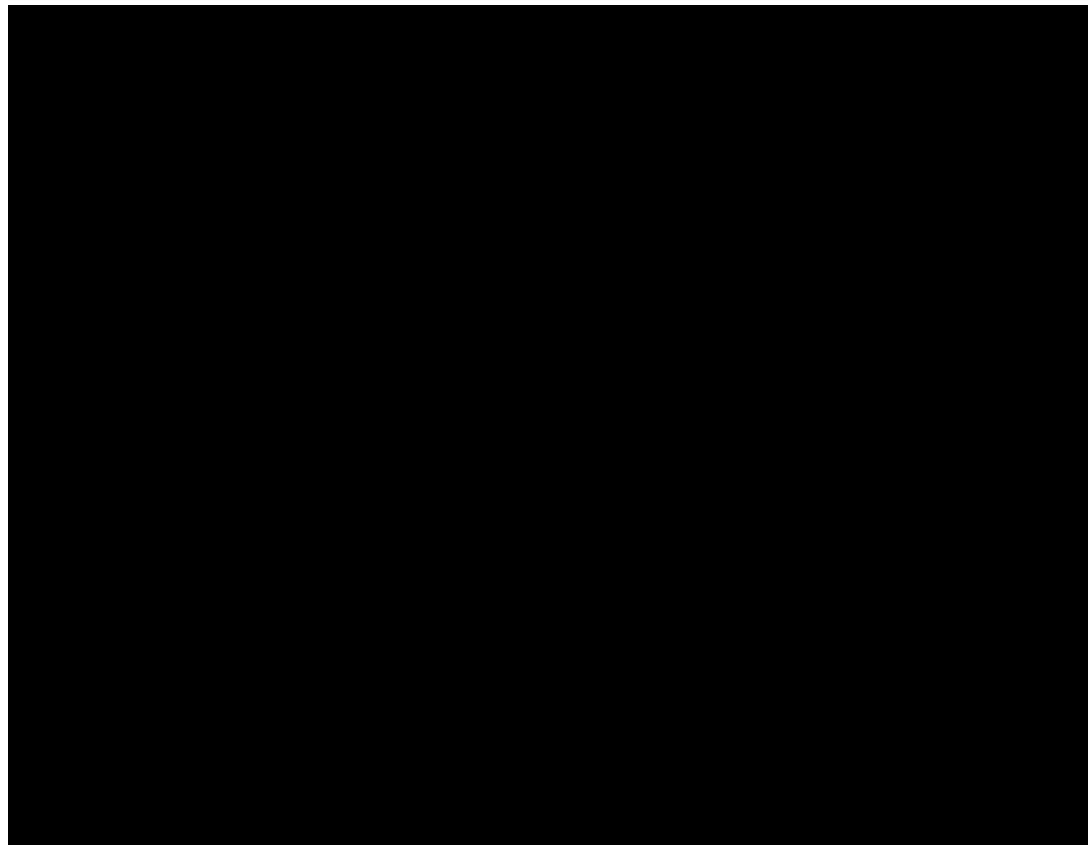
Prof. Alexander Jablonski, 1935

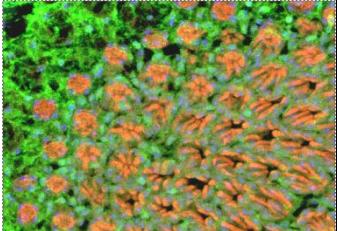


Fluorescence

Leica
MICROSYSTEMS

Principe du filtrage de la lumière

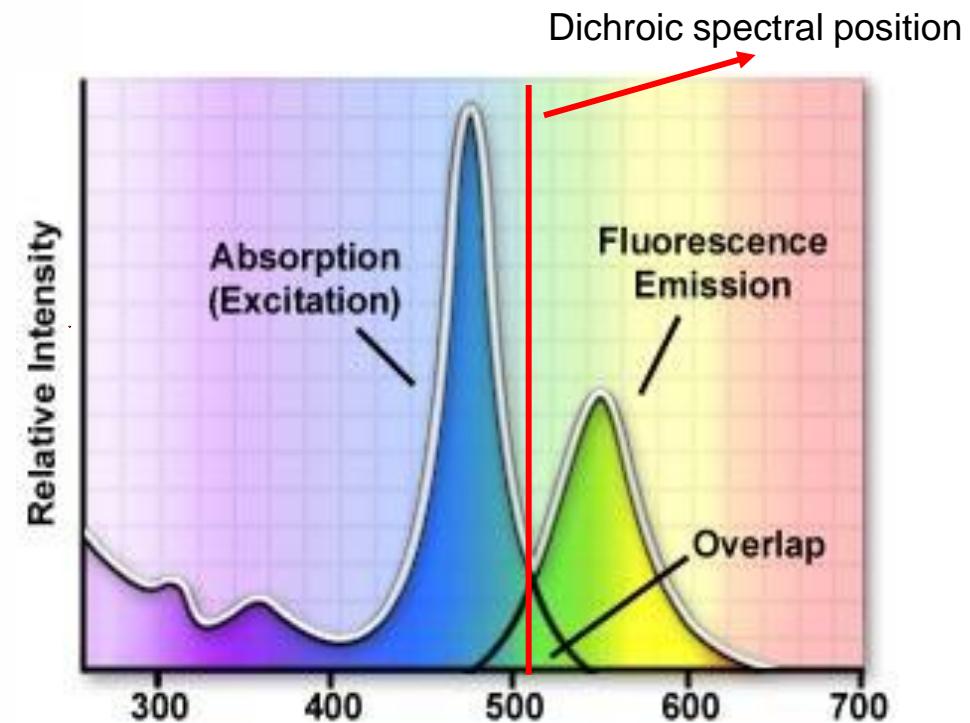
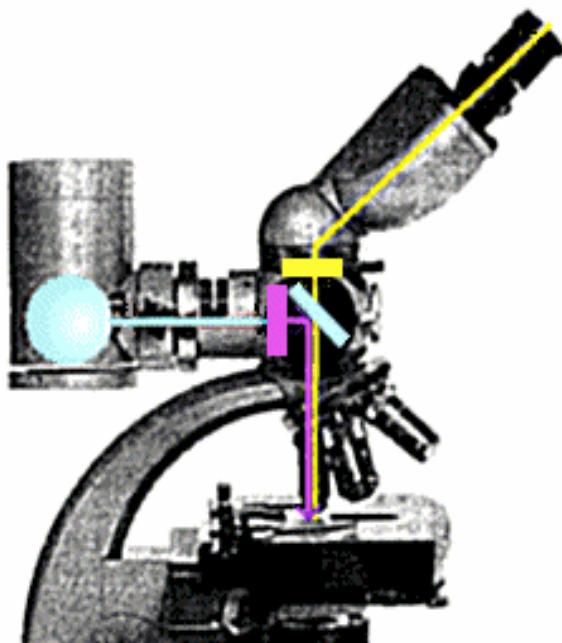


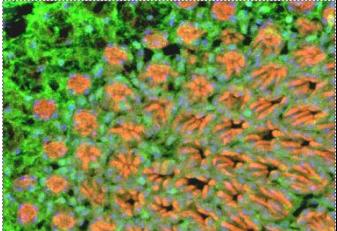


Fluorescence

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Application au microscope : dichroïque

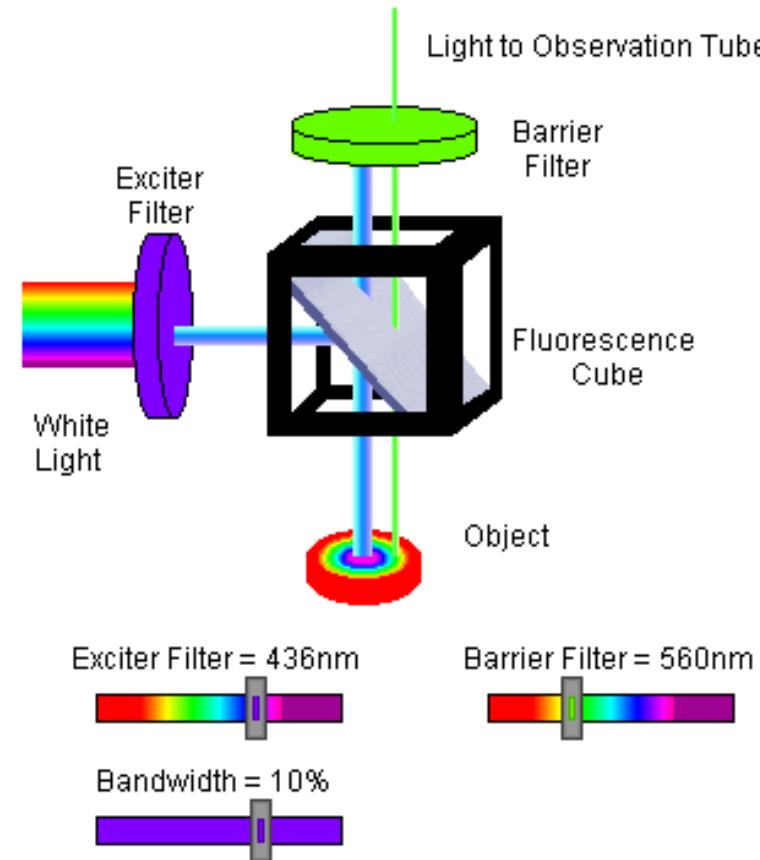
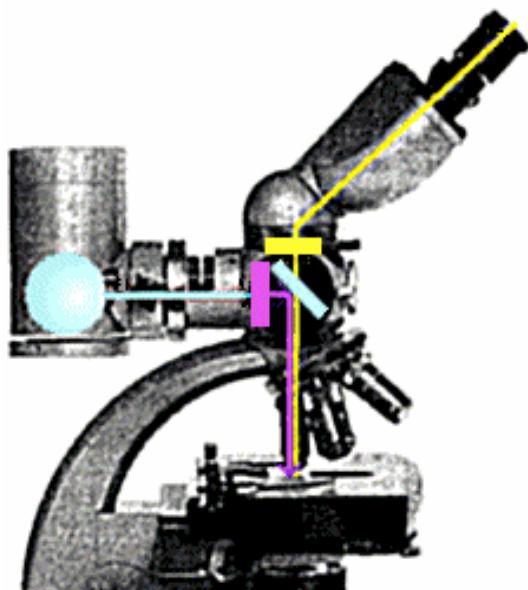


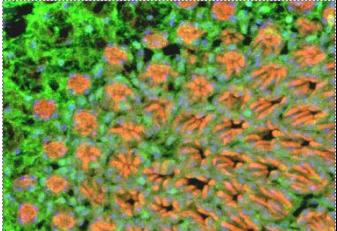


Fluorescence

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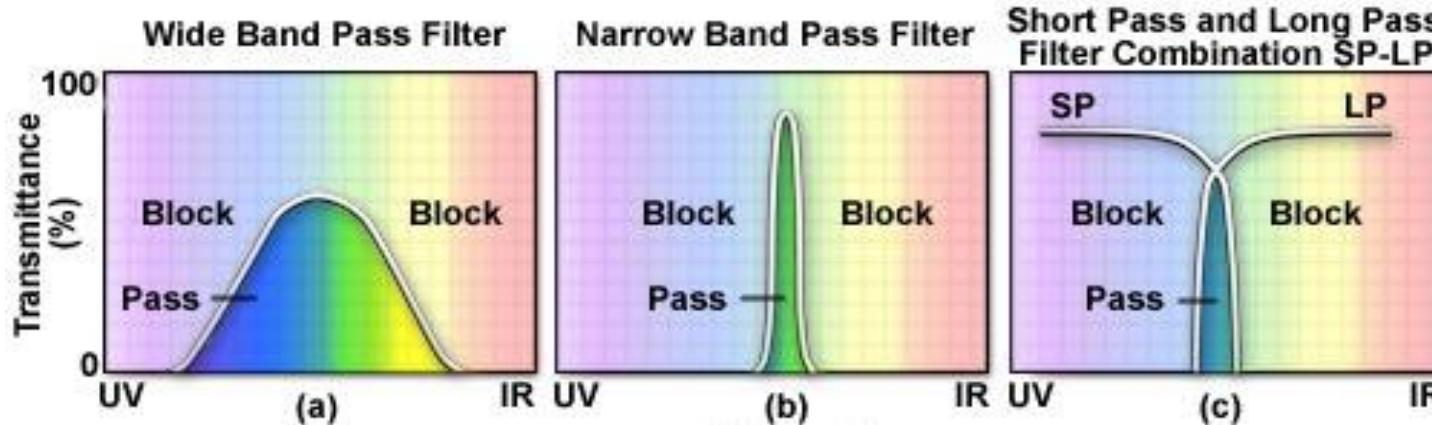
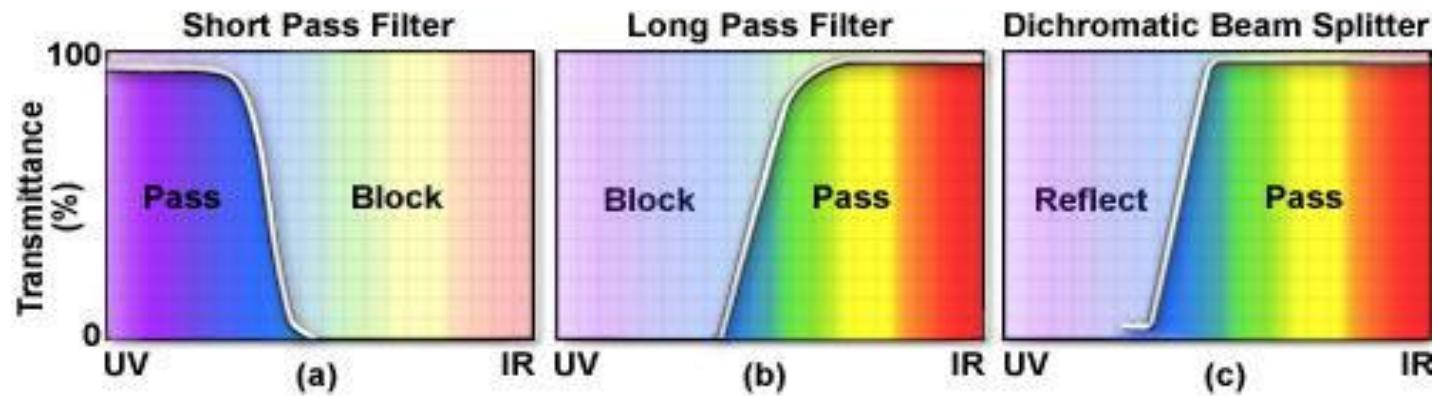
Prof. Ploem's invention

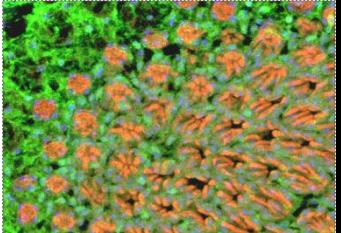




Fluorescence

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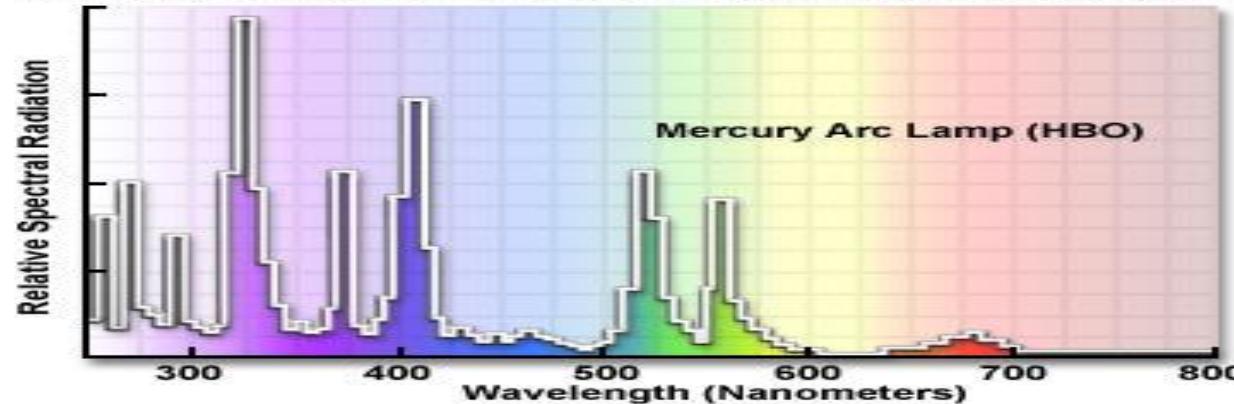


Fluorescence

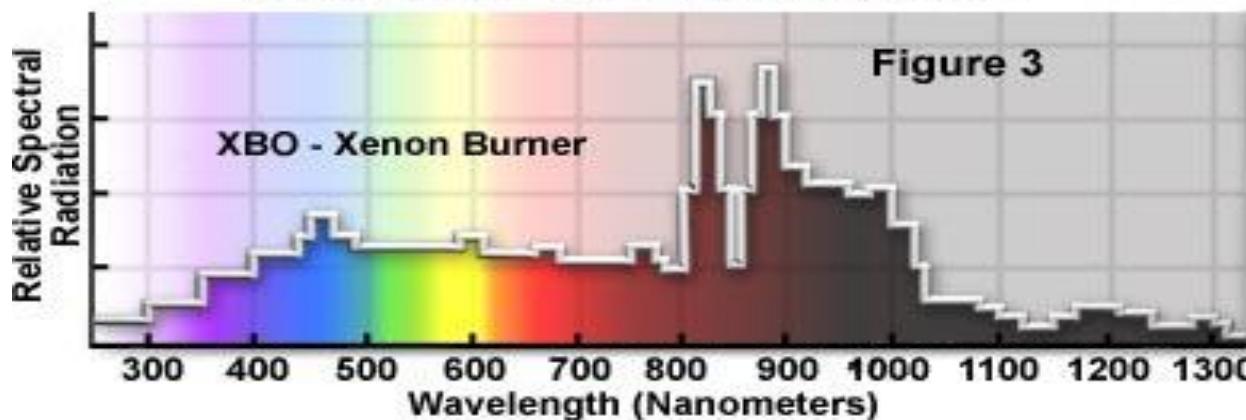
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Exemple de lampes à fluorescence

Mercury Arc Lamp UV and Visible Emission Spectrum



Xenon Arc Lamp Emission Spectrum

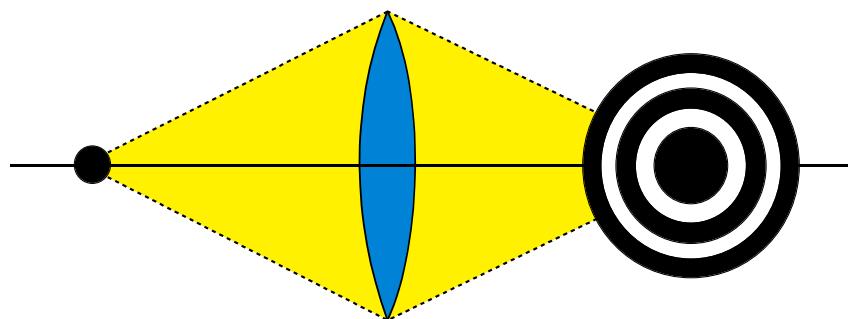


Microscopie Confocale

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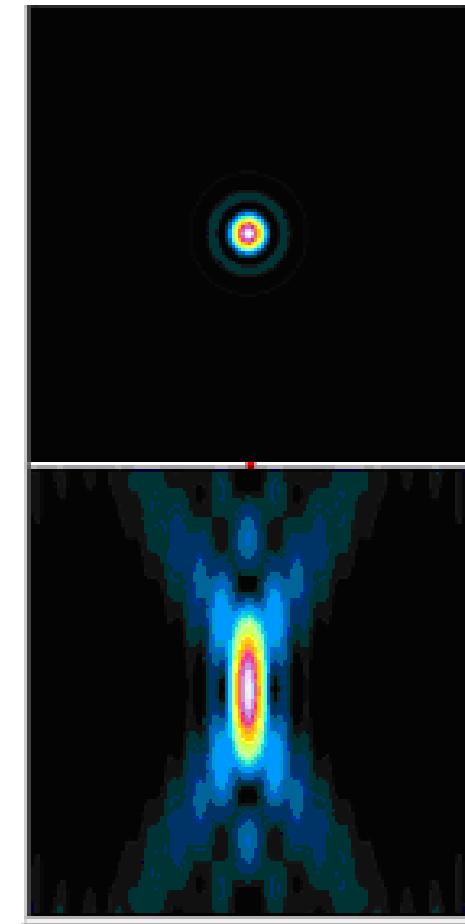
Résolution



Airy disc

$$D_0 = 1.22 * \lambda / \text{NA} \text{ (lateral)}$$

Limited by Diffraction

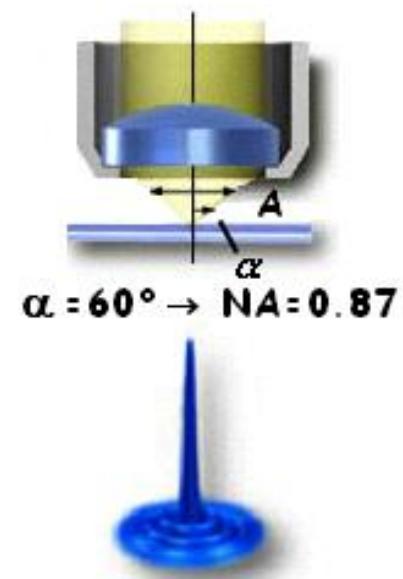
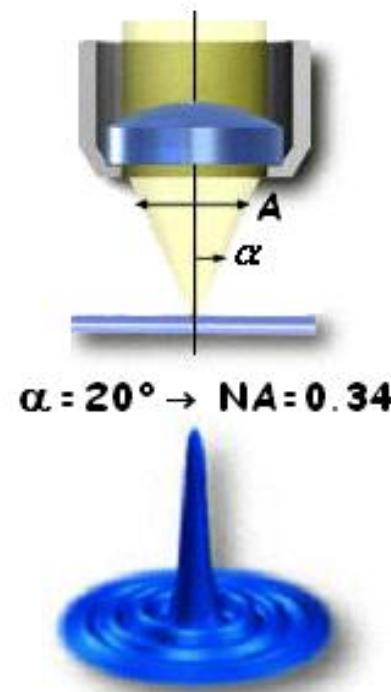
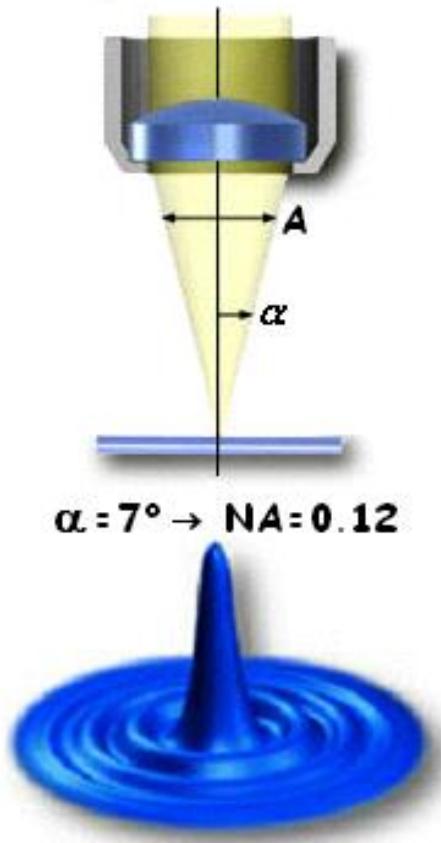




Résolution

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$$NA = n \sin\alpha$$



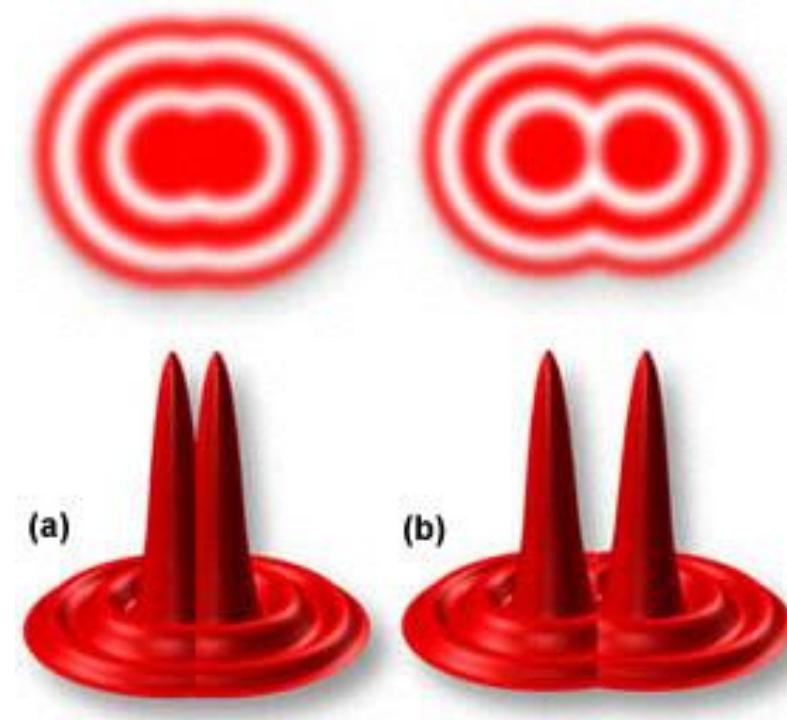
Point Spread Function (PSF)



Résolution

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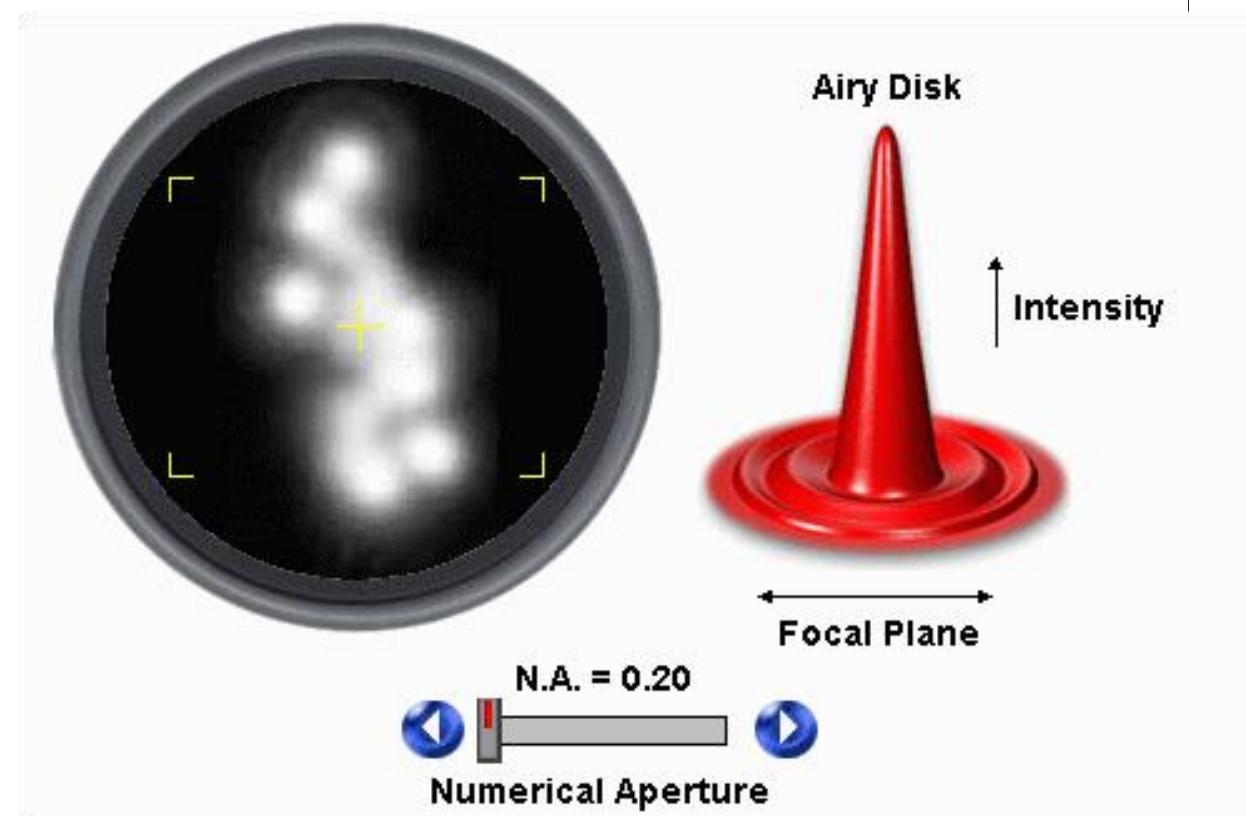
$$\text{Res} = 0.61 * \lambda / \text{NA}$$





Résolution

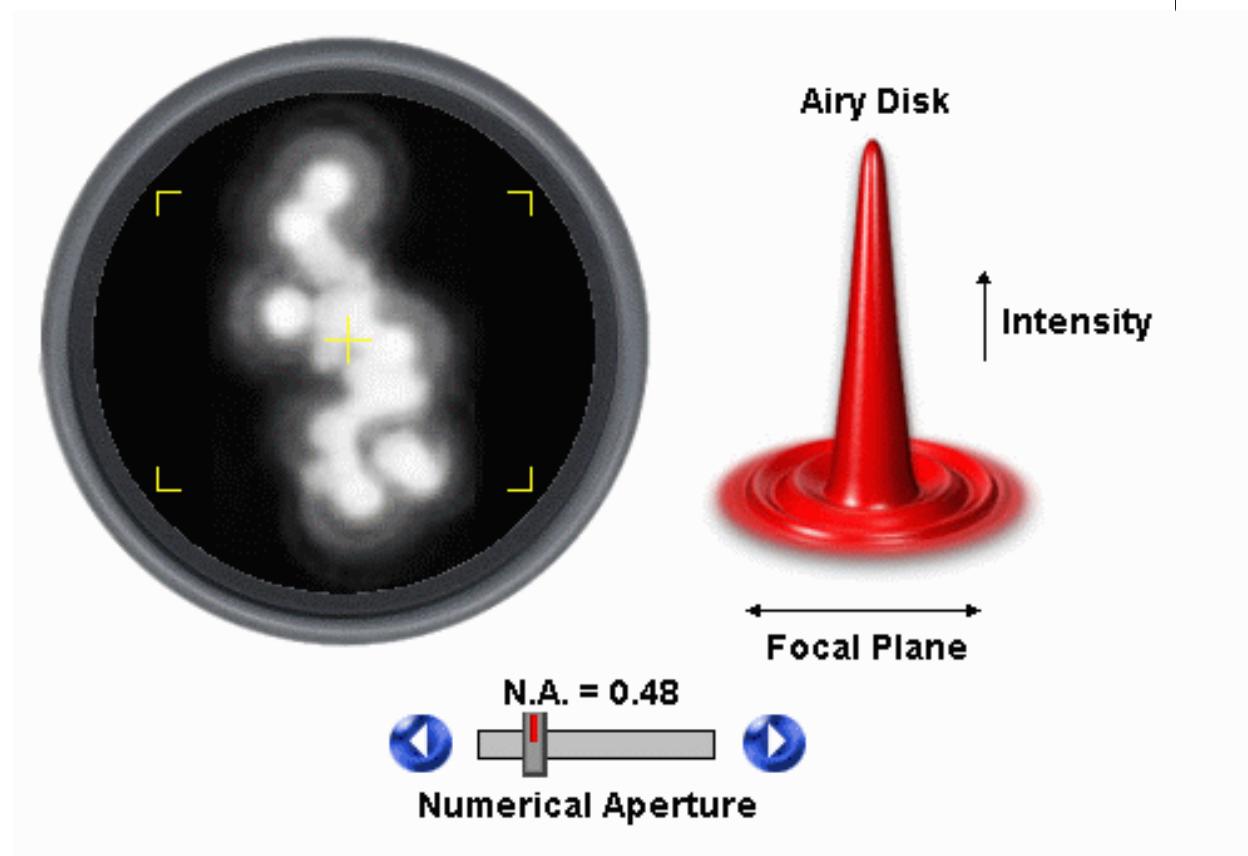
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Résolution

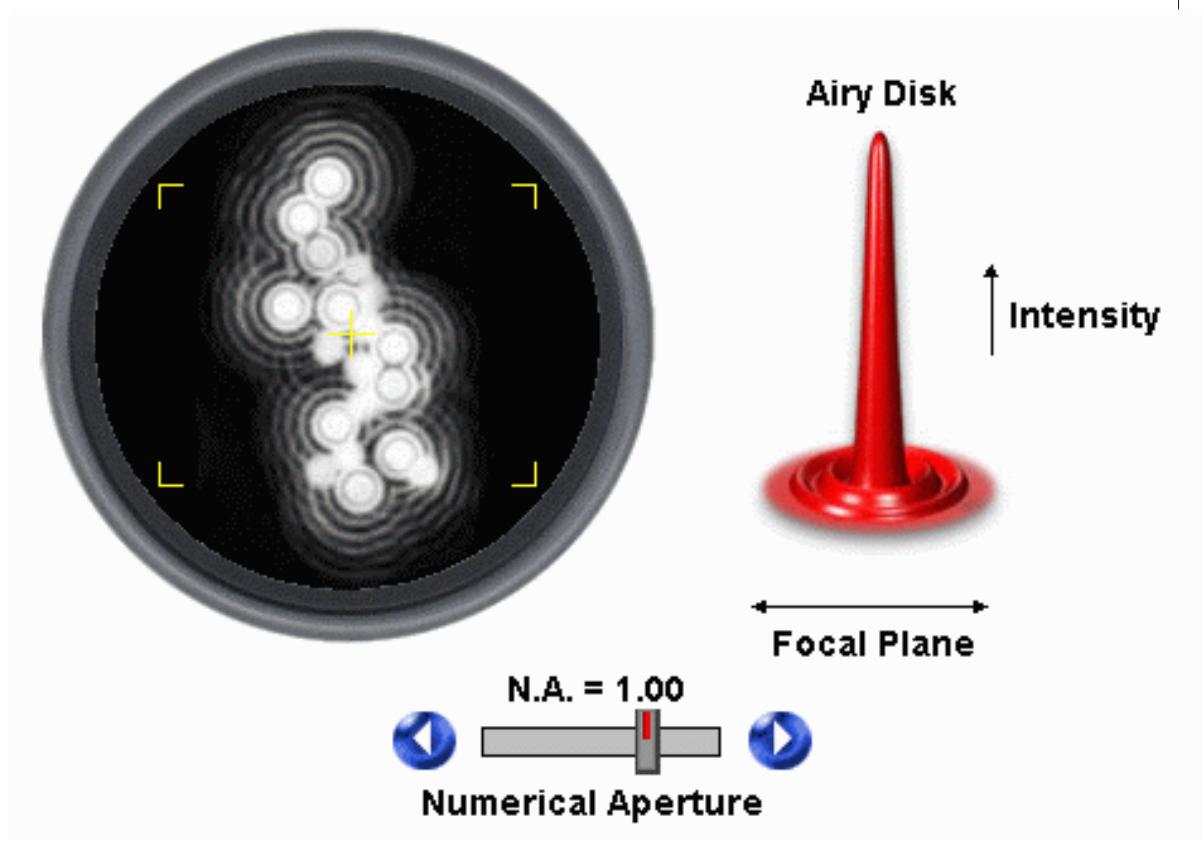
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Résolution

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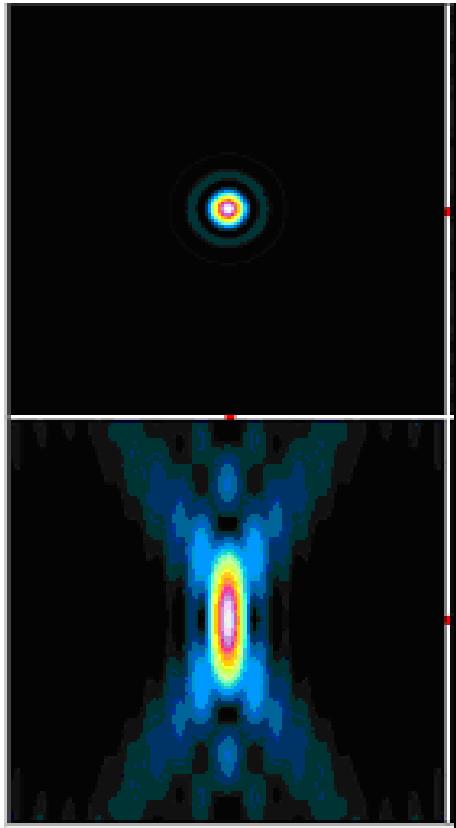




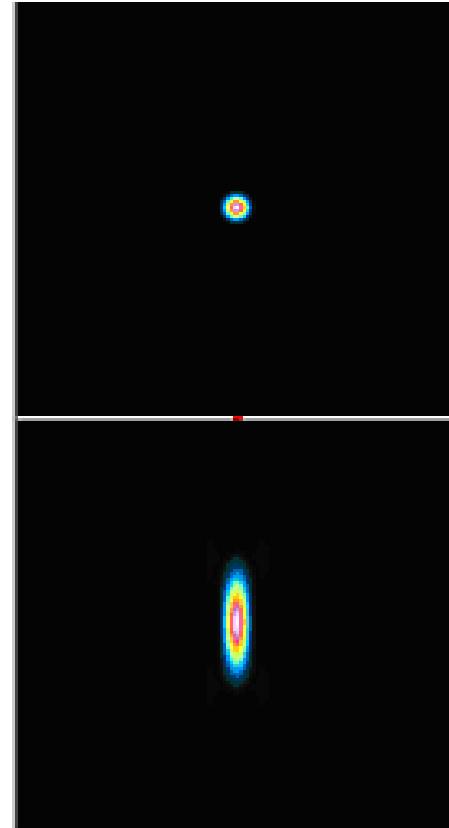
Résolution

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Conventional



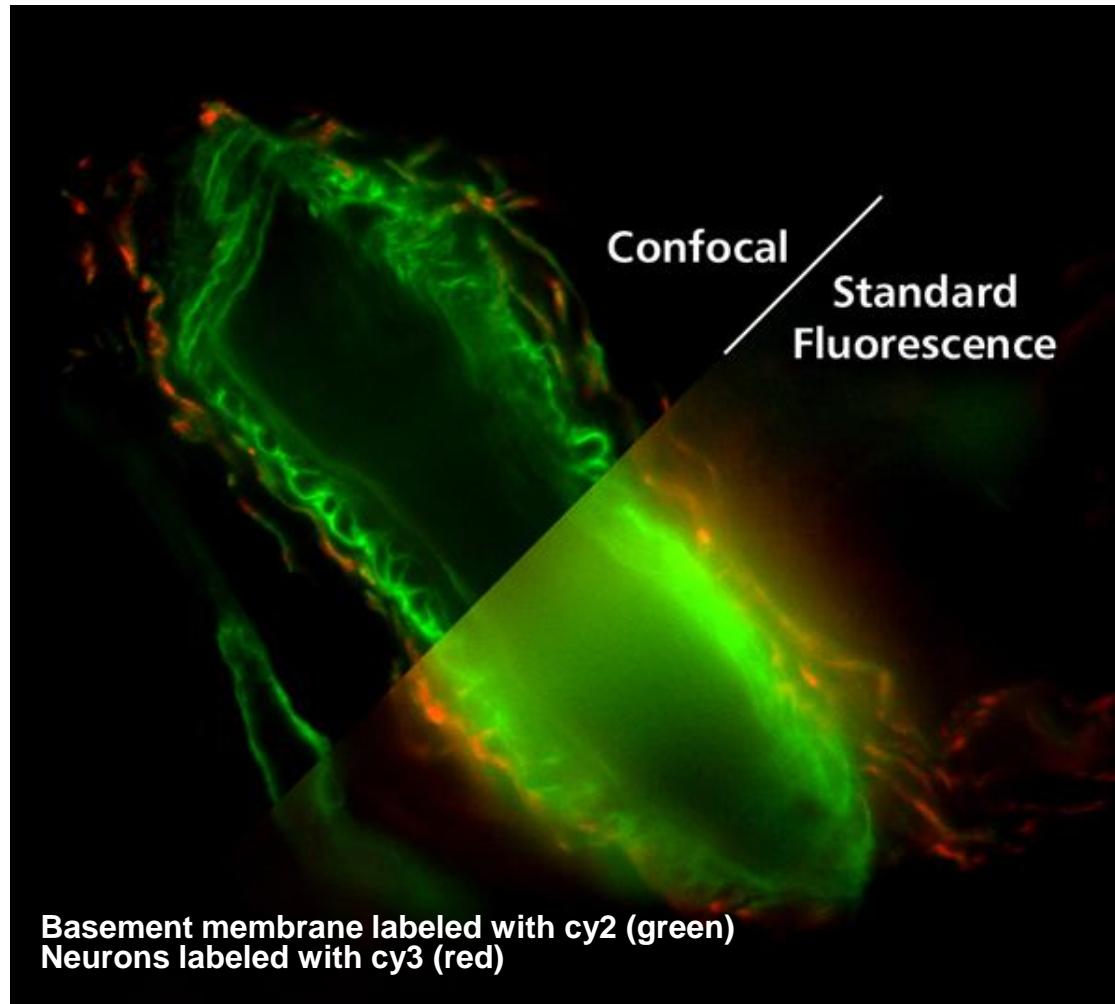
Confocal





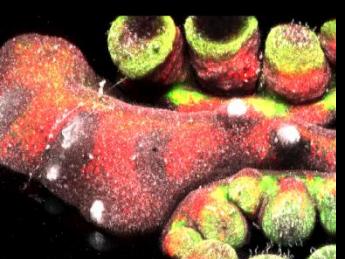
Résolution

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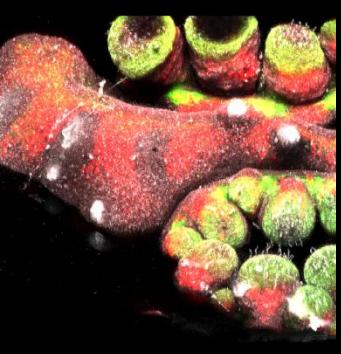


Microscopie confocale

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Fundamento





Microscopie confocale

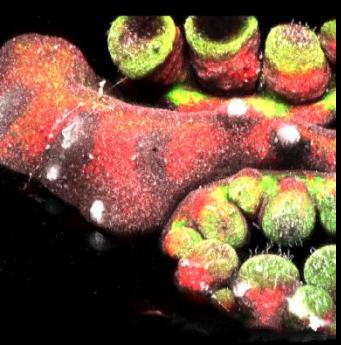
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Sectionnement optique de l'échantillon

Suppression de la fluorescence en dehors du plan focal

Amélioration de la résolution latérale et axiale

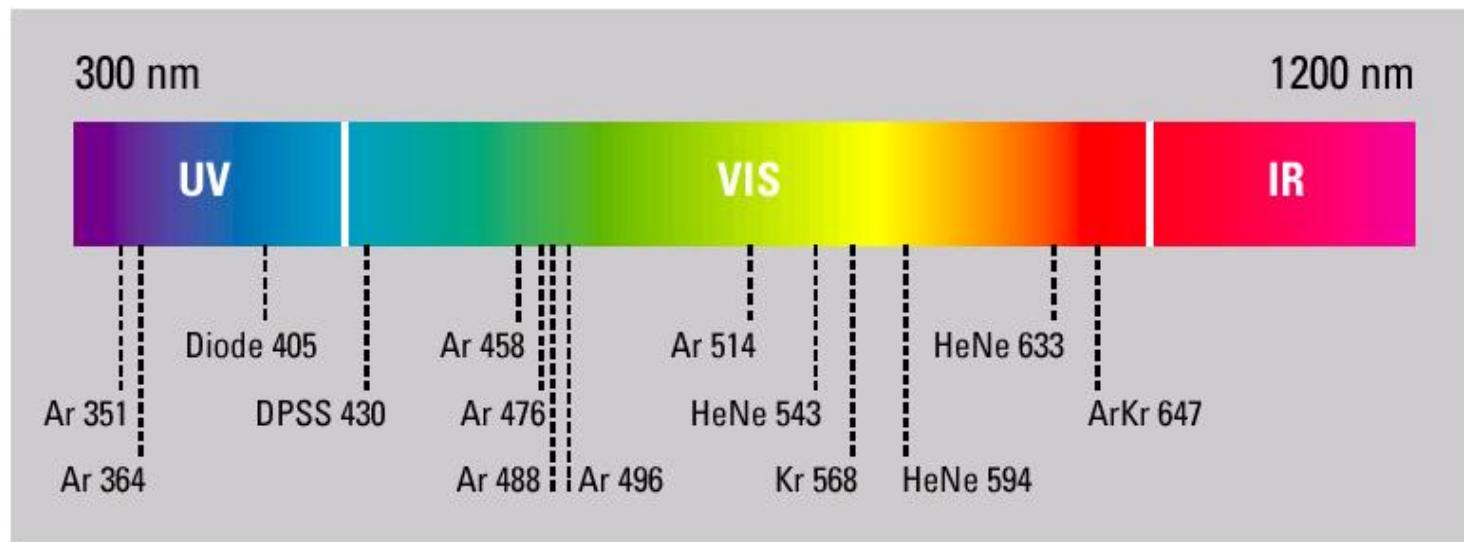
Amélioration du contraste

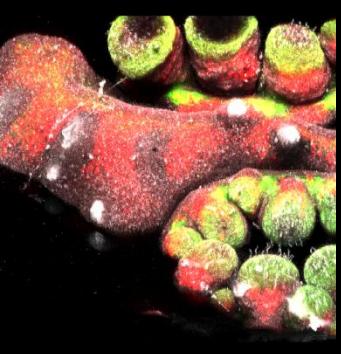


Microscopie confocale

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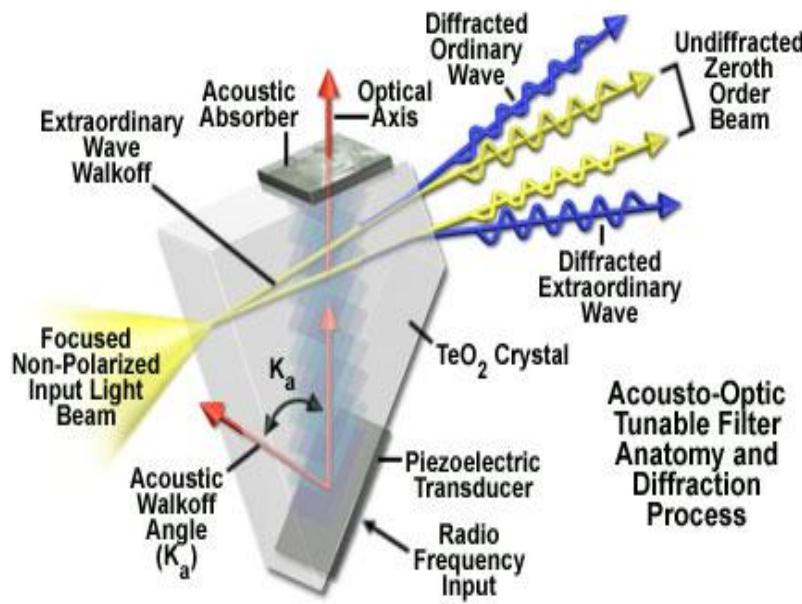
LASER





Microscopie confocale

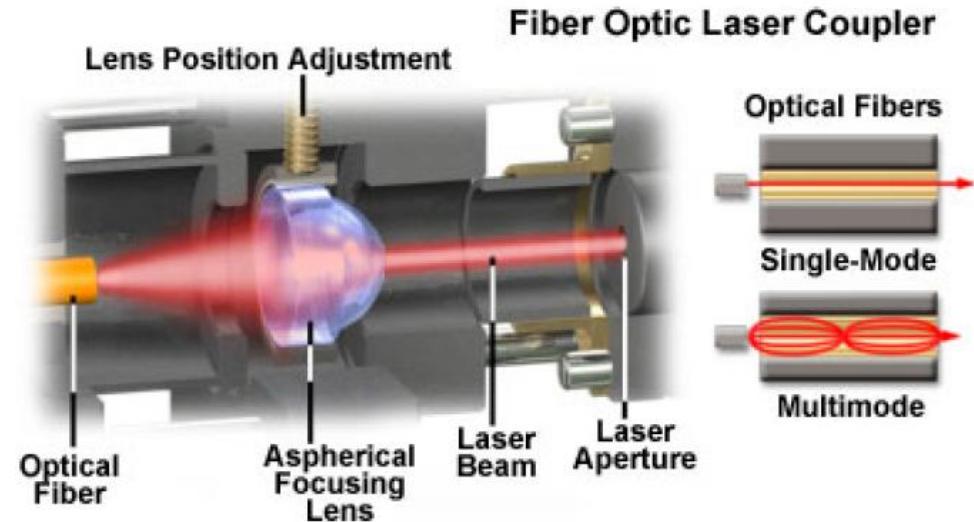
AOTF : Acousto Optical Tunable Filter

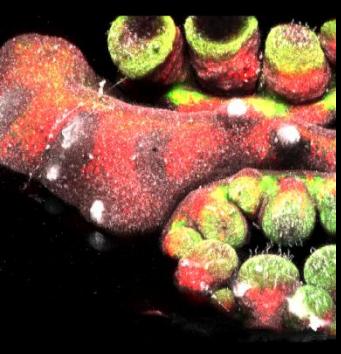


Sélection de la longueur d'onde d'émission

Modulation de l'intensité

Couplage par fibre optique





Microscopie confocale

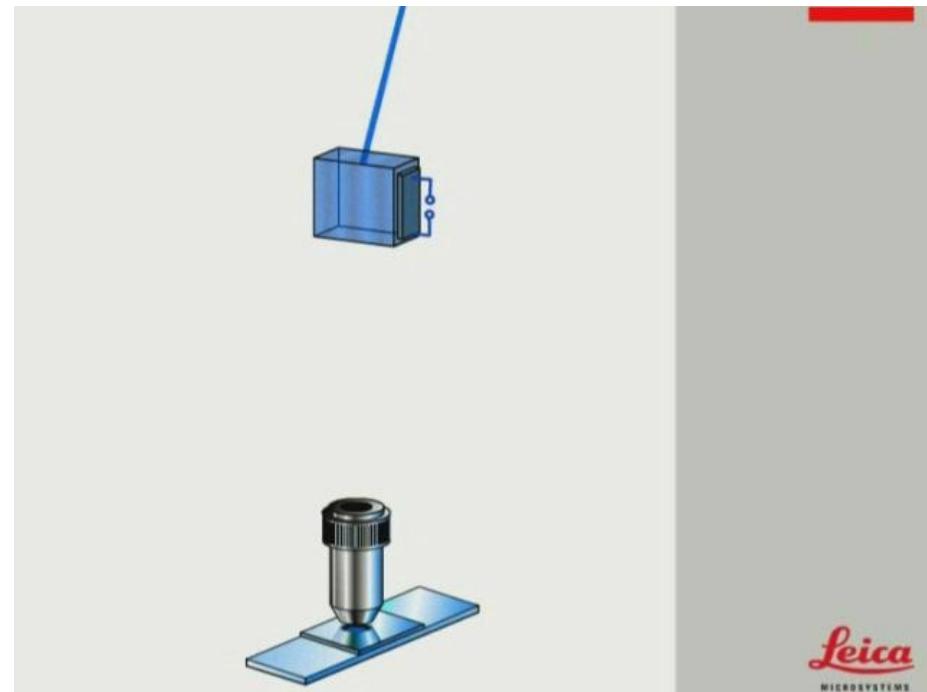
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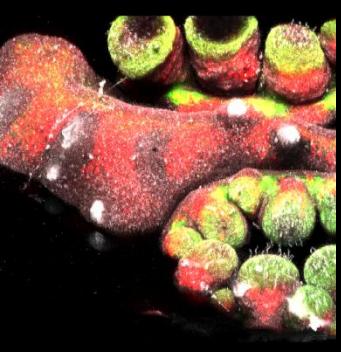
Beam splitter

Miroir dichroïque



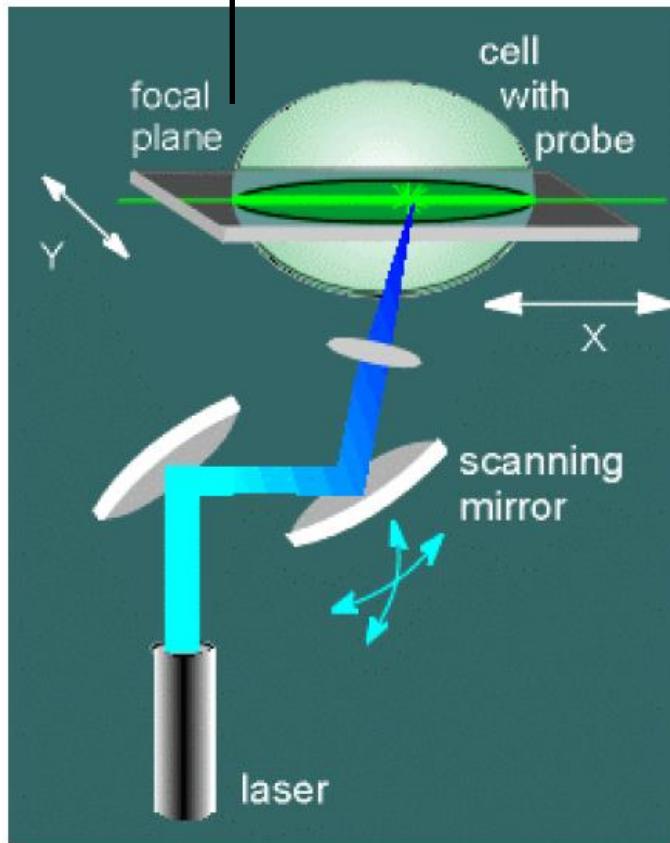
AOBS





Microscopie confocale

Scanner en XY



Comment faire de l'imagerie point par point ?

↳ Miroirs rotatifs (galvanomètres)

Zoom ?



Amplitude de balayage

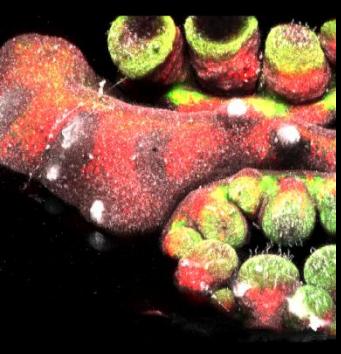


Limites sur la vitesse de balayage :
récupération des photons et effets photo-induits

Scanning the Sample

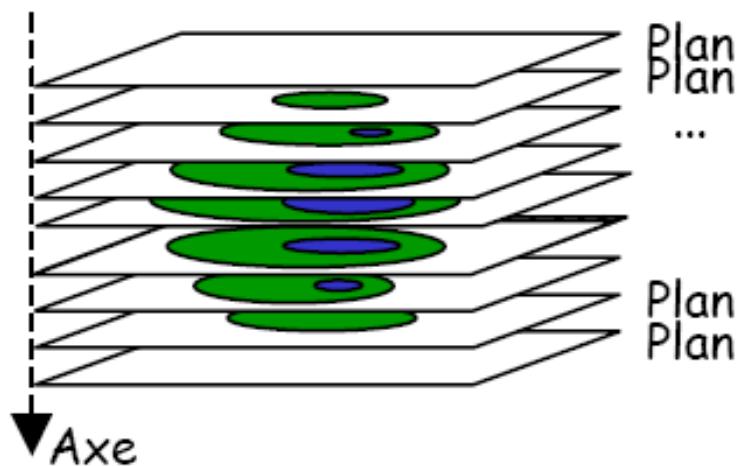
Secciones Ópticas





Microscopie confocale

Sectionnement optique



Imagerie plan / plan en XY



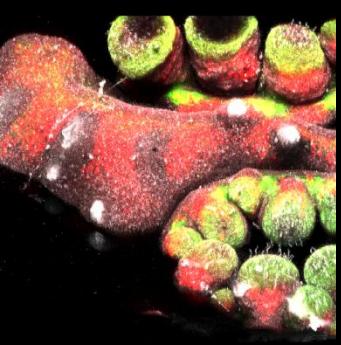
Echantillonnage : Critère de Nyquist
Taille pixel $\leq 2,3$ Res



Déplacement en Z du microscope



Reconstruction 3D



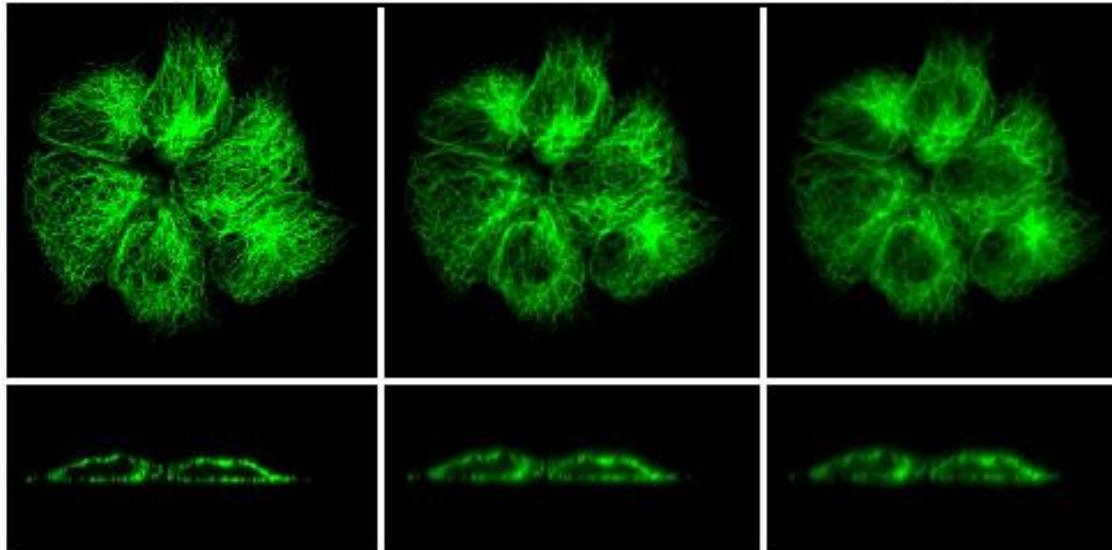
Microscopie confocale

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Pinhole

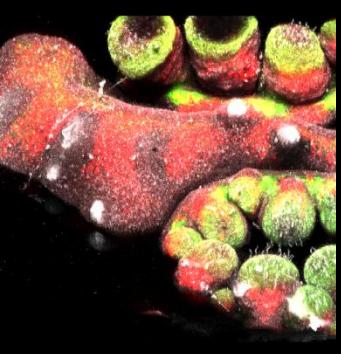


Ouverture fonction de :
 λ : longueur d'onde
NA : ouverture numérique



Résolution optimale

Intensité de fluorescence
maximale

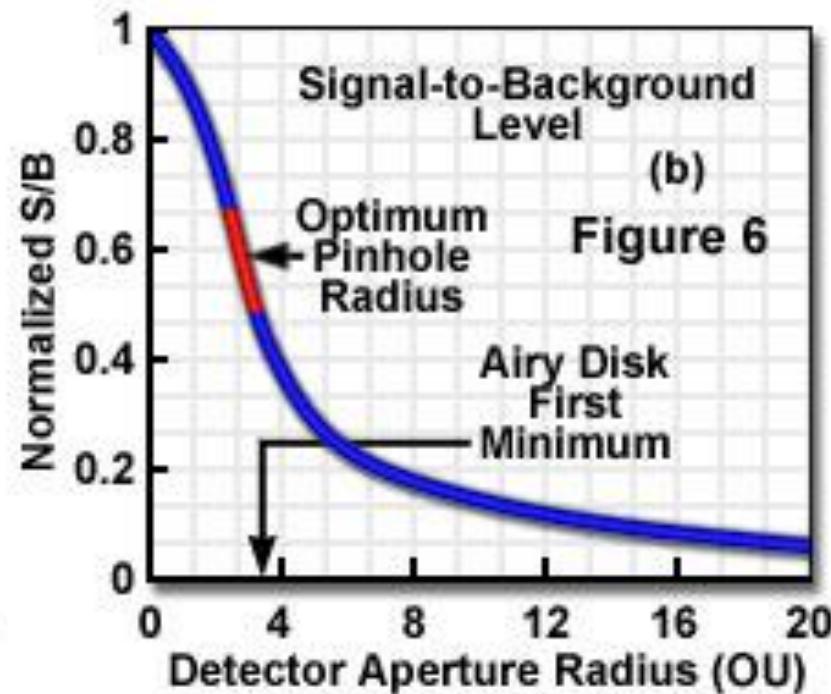
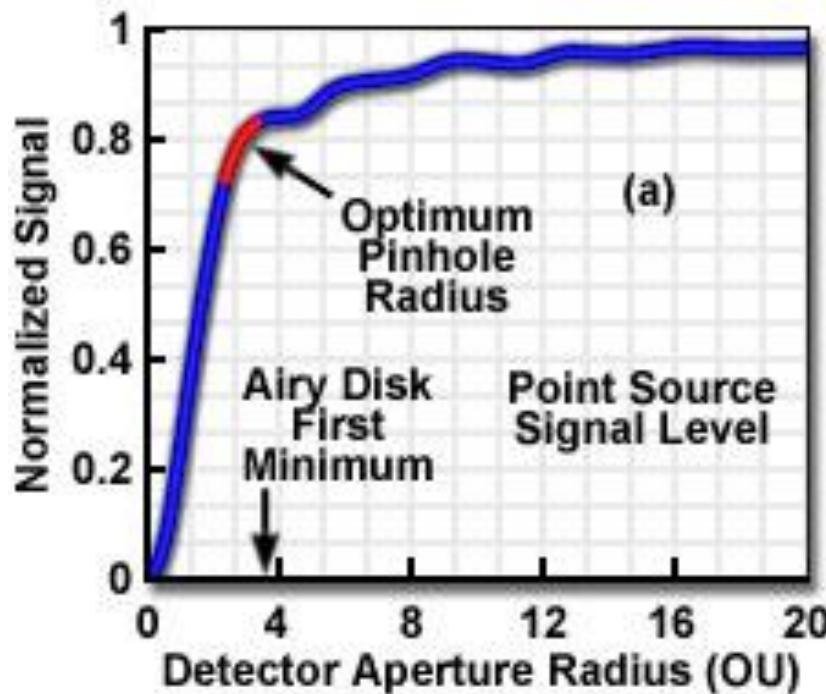


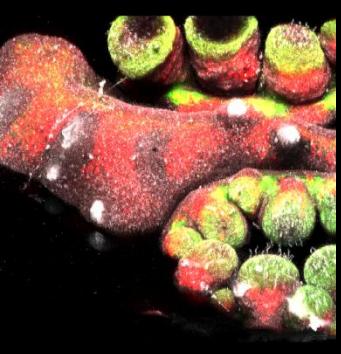
Microscopie confocale

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Pinhole

Pinhole Aperture Size Effects on Signal and S/B Levels

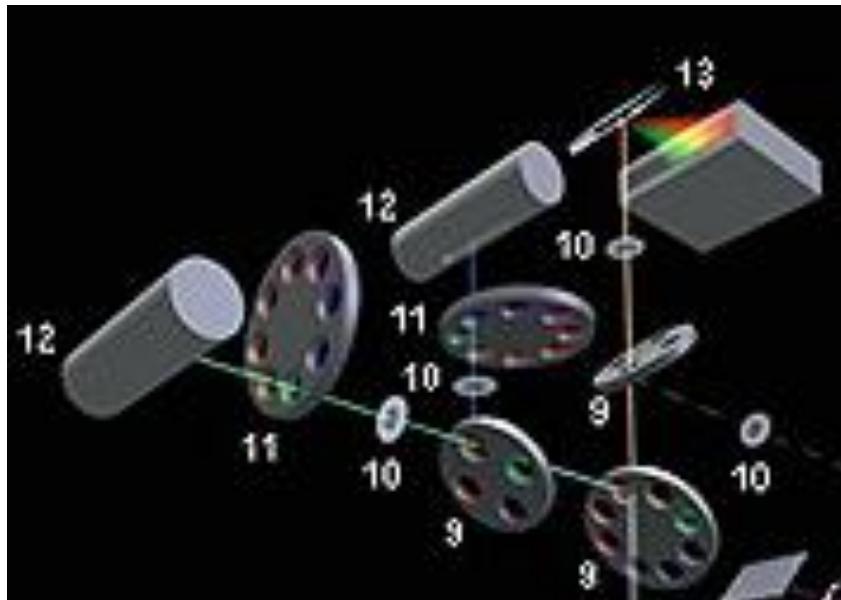




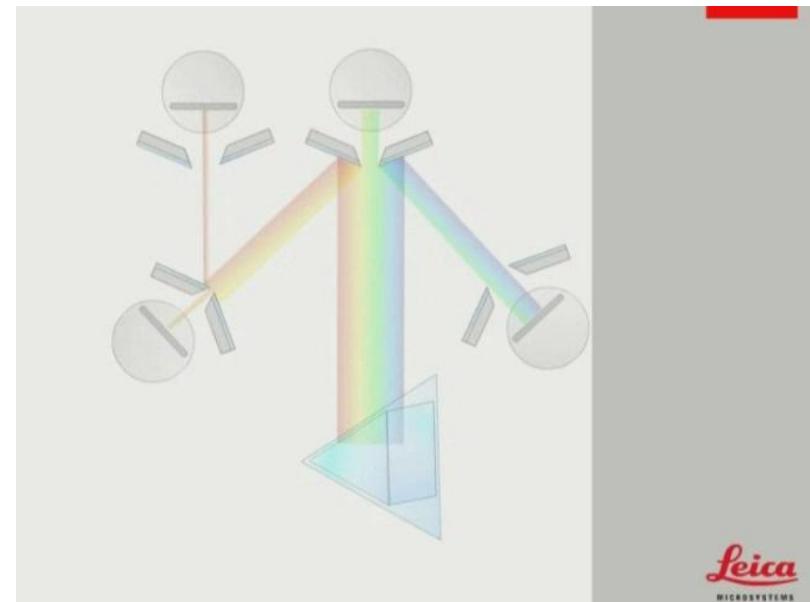
Microscopie confocale

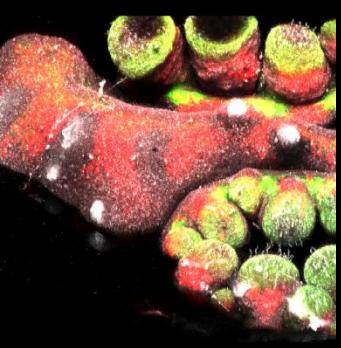
Filtrage spectral

Cascade de dichroïques



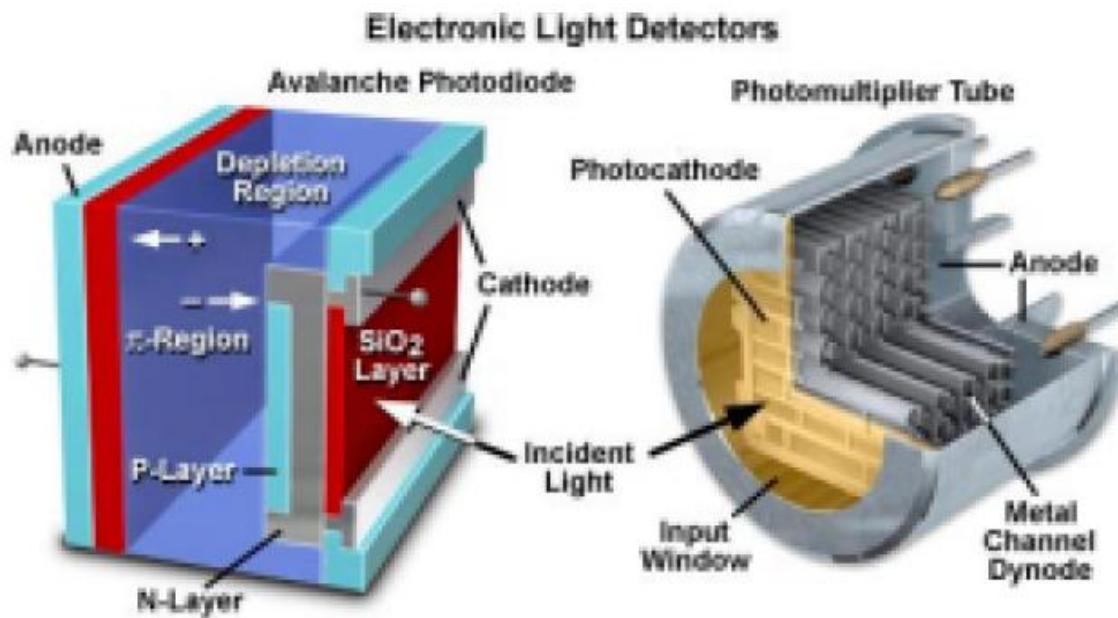
Système spectral





Microscopie confocale

Détecteur

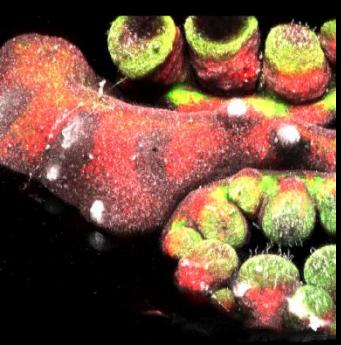


Gain variable 0 à 1250 V

Echantillonage

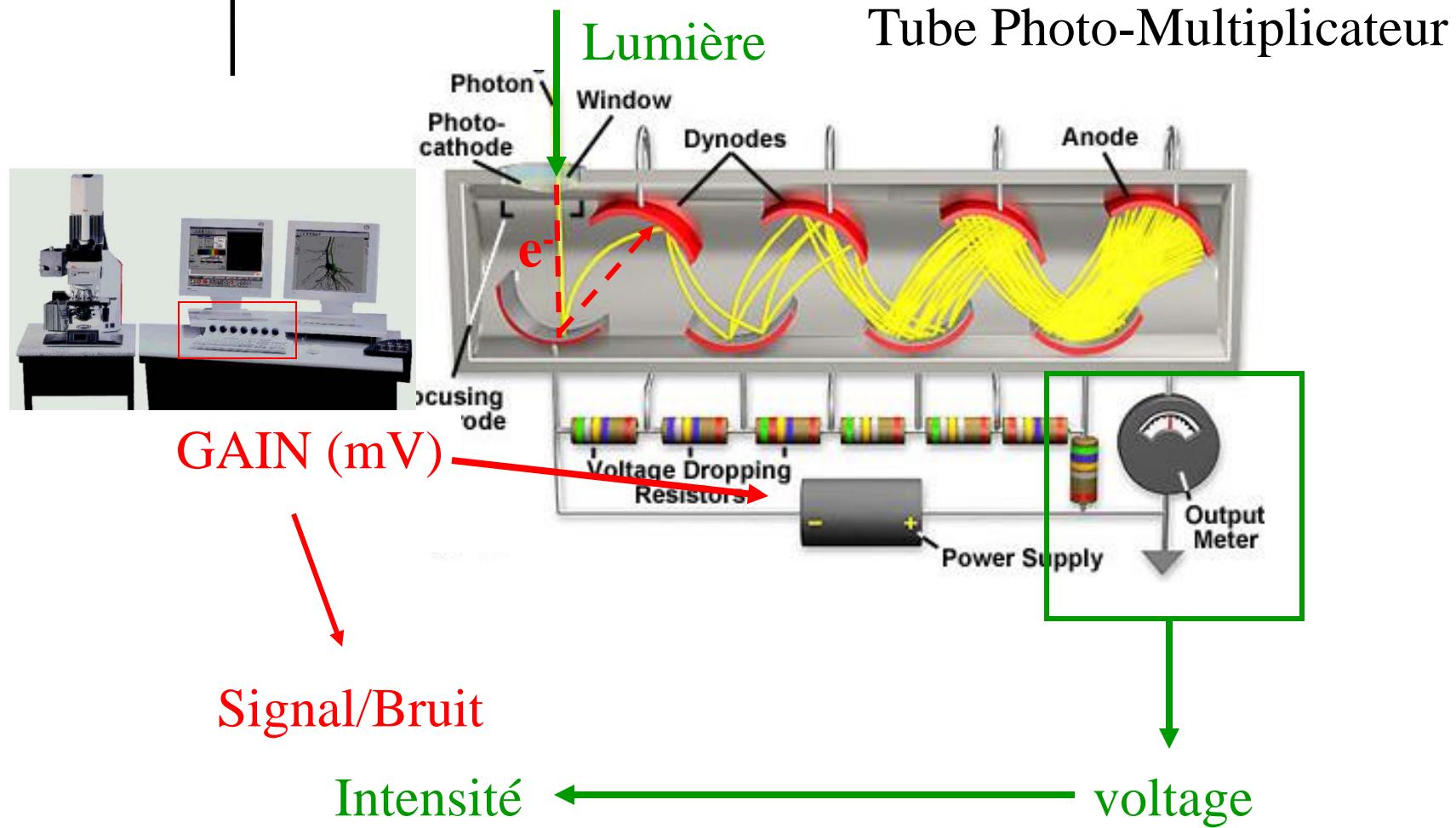
Quantification

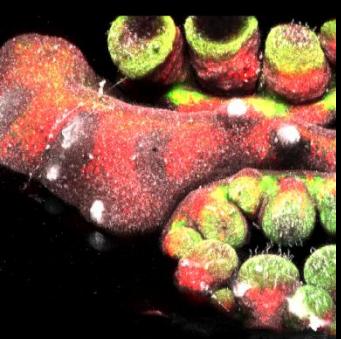
Transformation du signal en niveau de gris 8 bits 12 bits...



Microscopie confocale

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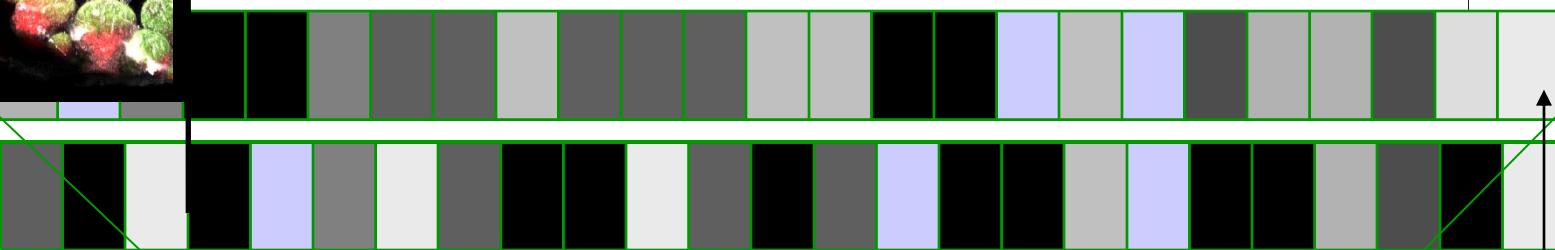




Microscopie confocale : Numérisation

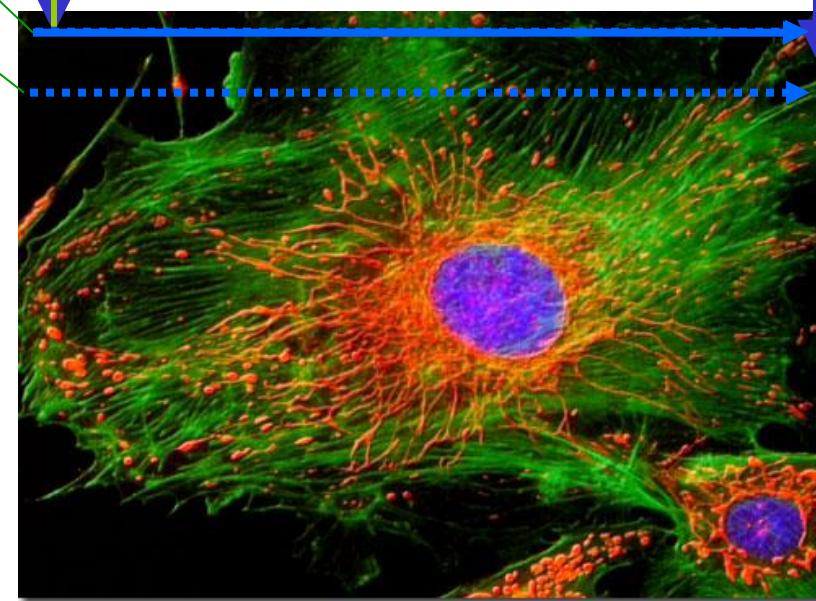
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29



Pixel

Y
512

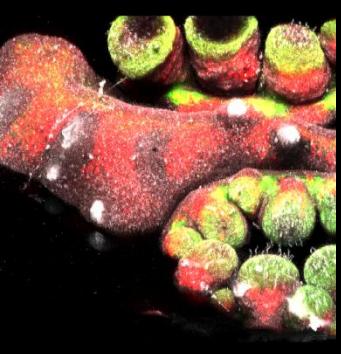


X 512

CAN Converter
8bit / 12 bit (= 256 / 4096 Greyvalues)

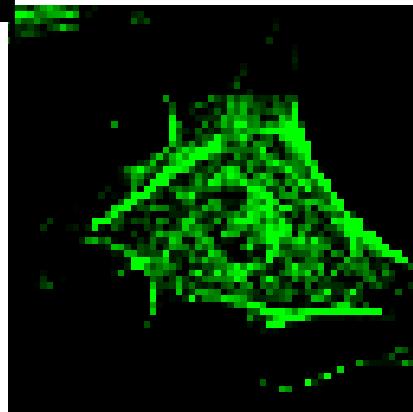
Frame Store
Data Files (e.g. TIF)

38

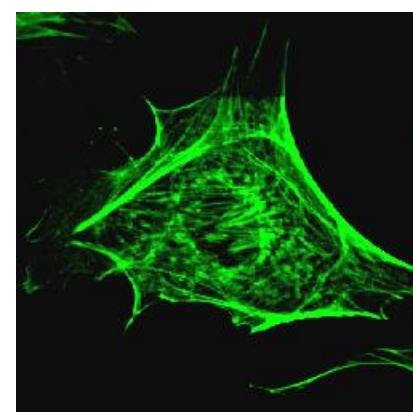


Microscopie confocale : pixelisation

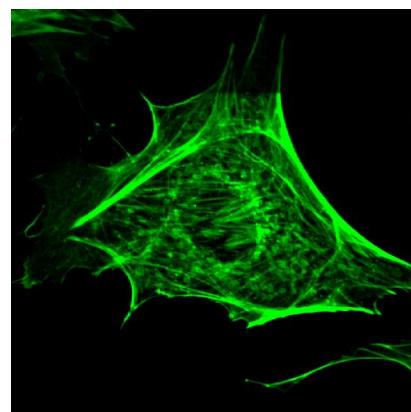
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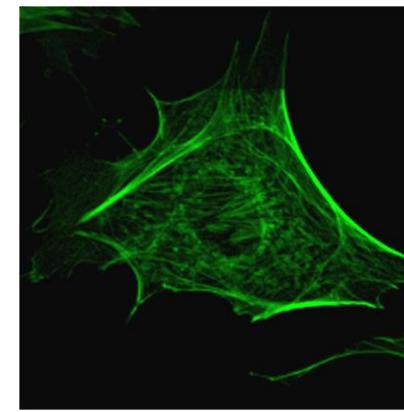
800x800nm



200x200nm

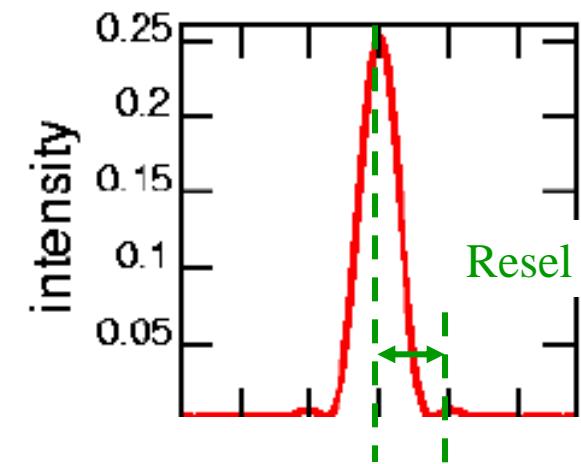


100x100nm

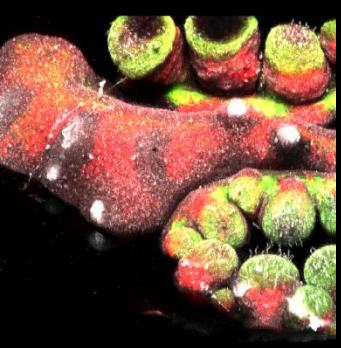


50x50nm

Travailler avec une taille
optimal de pixel



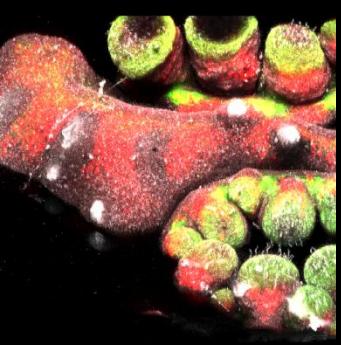
Théorie de Nyquist :
2,3 pixels /resel



Microscopie confocale

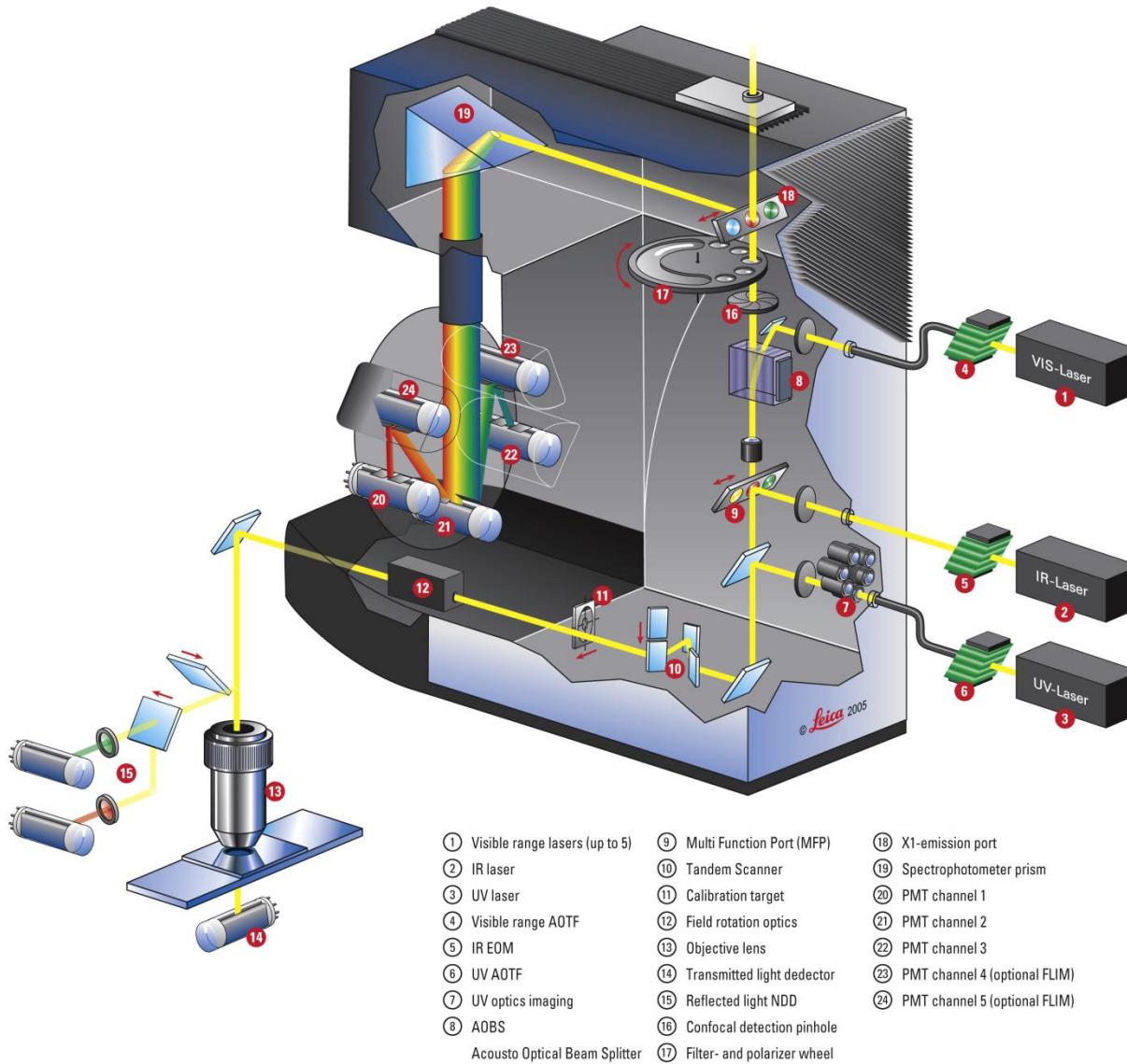
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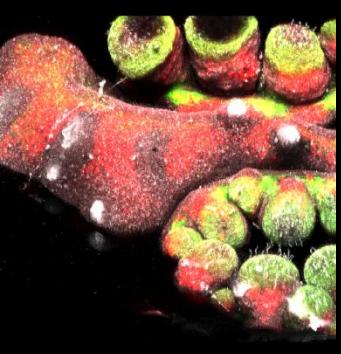




Microscopie confocale

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Microscopie confocale

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Sectionnement optique de l'échantillon

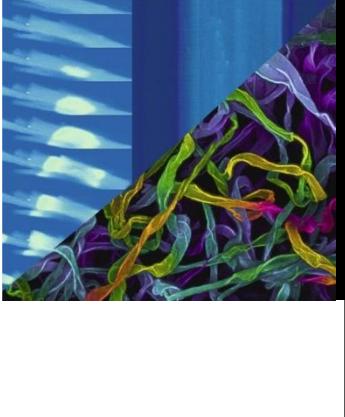
Suppression de la fluorescence en dehors du plan focal

Amélioration de la résolution latérale et axiale

Amélioration du contraste

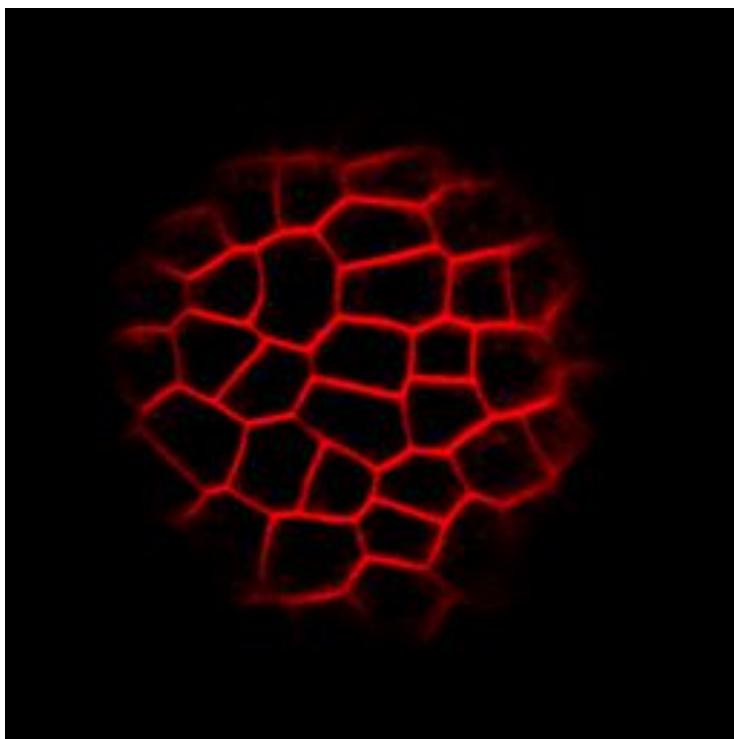
Microscopie Confocale

- Introduction
 - Historique
 - Fluorescence
 - Résolution
 - Microscopie Confocale
- Applications et exploitation des données
 - Immunomarquages
 - Réflection
 - Time-Lapse
 - Etudes spectrales
 - F-Techniques
 - FCS/FLIM
- Conclusion

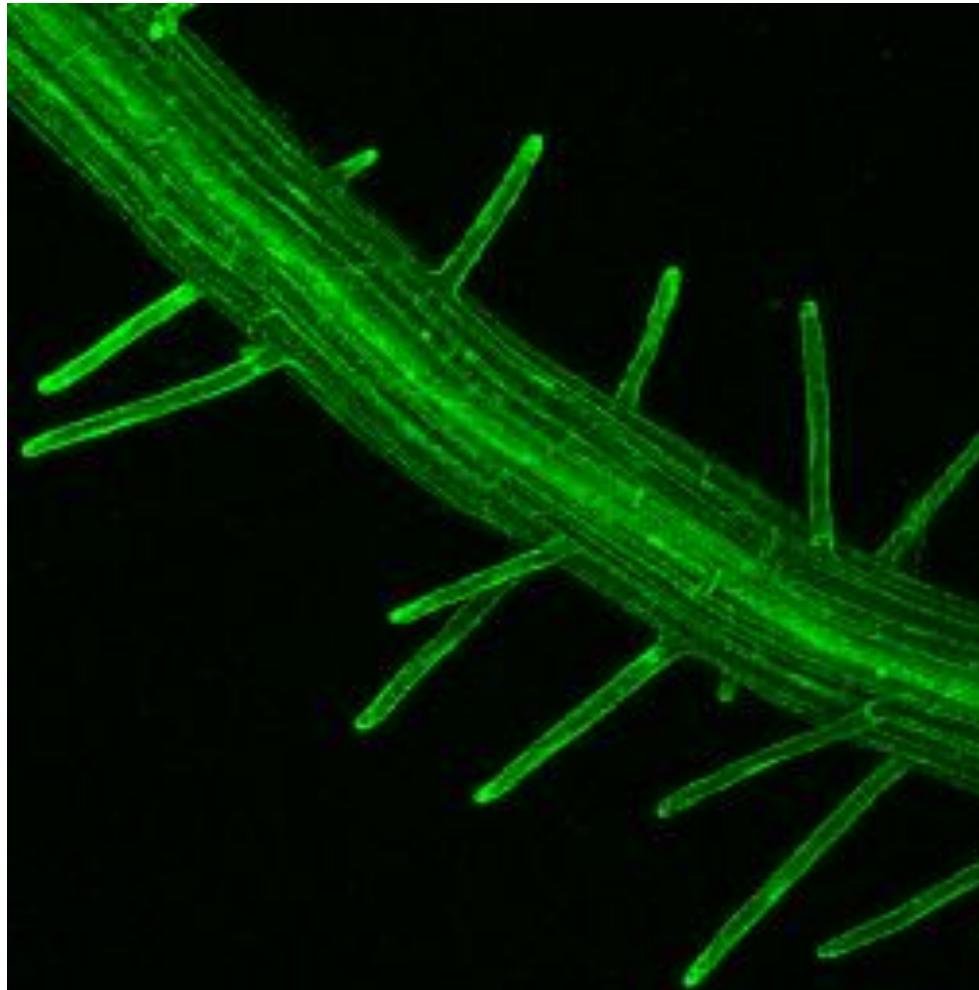


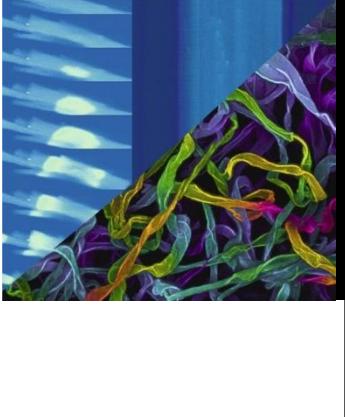
Immunohistochimie

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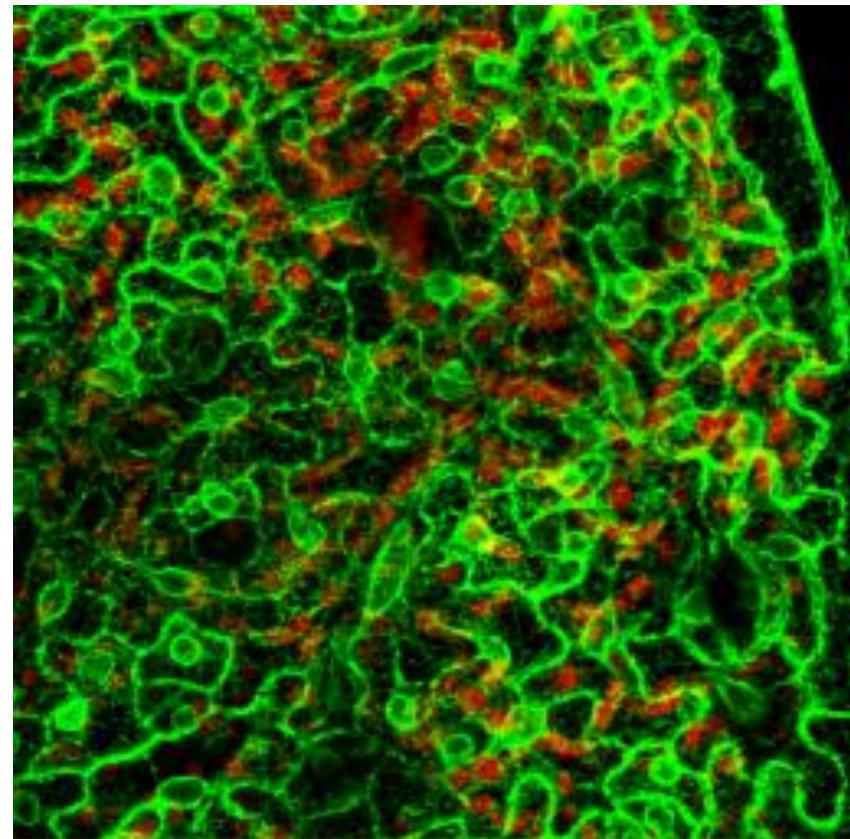
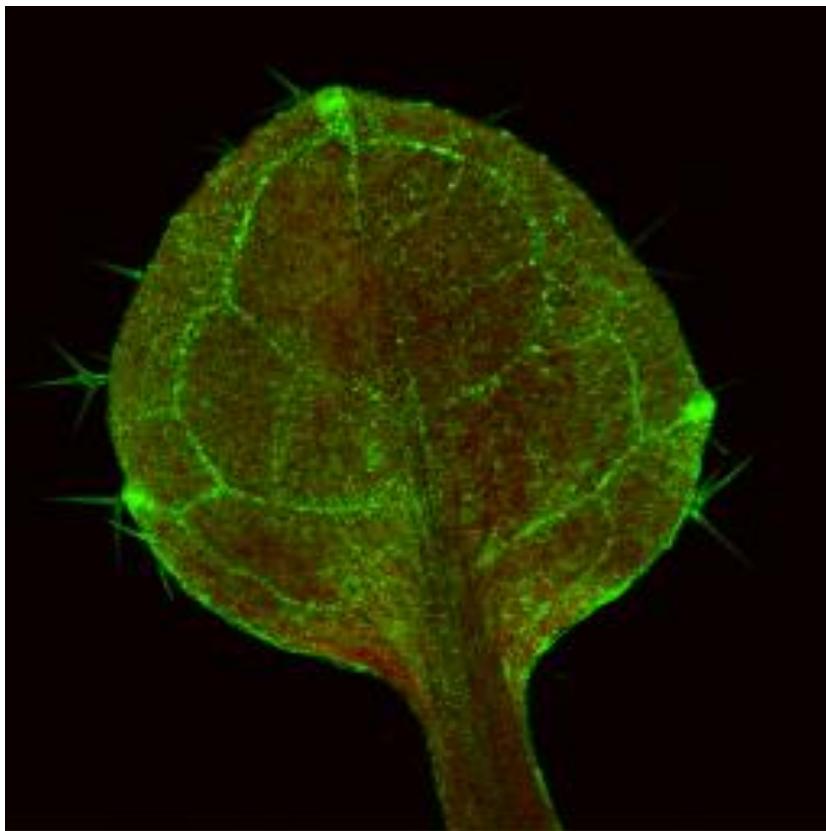
Immunohistochemie



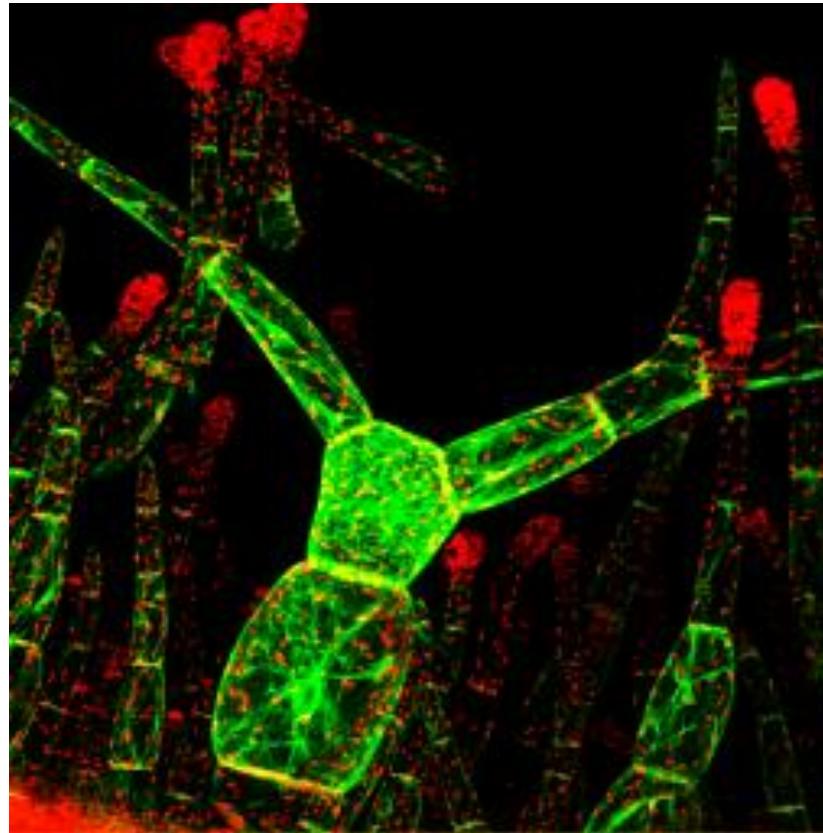


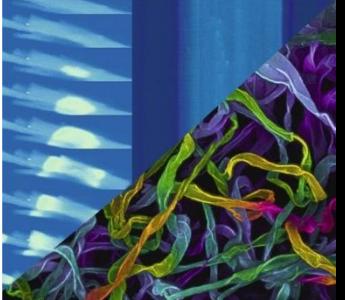
Immunohistochemie

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Immunohistochimie

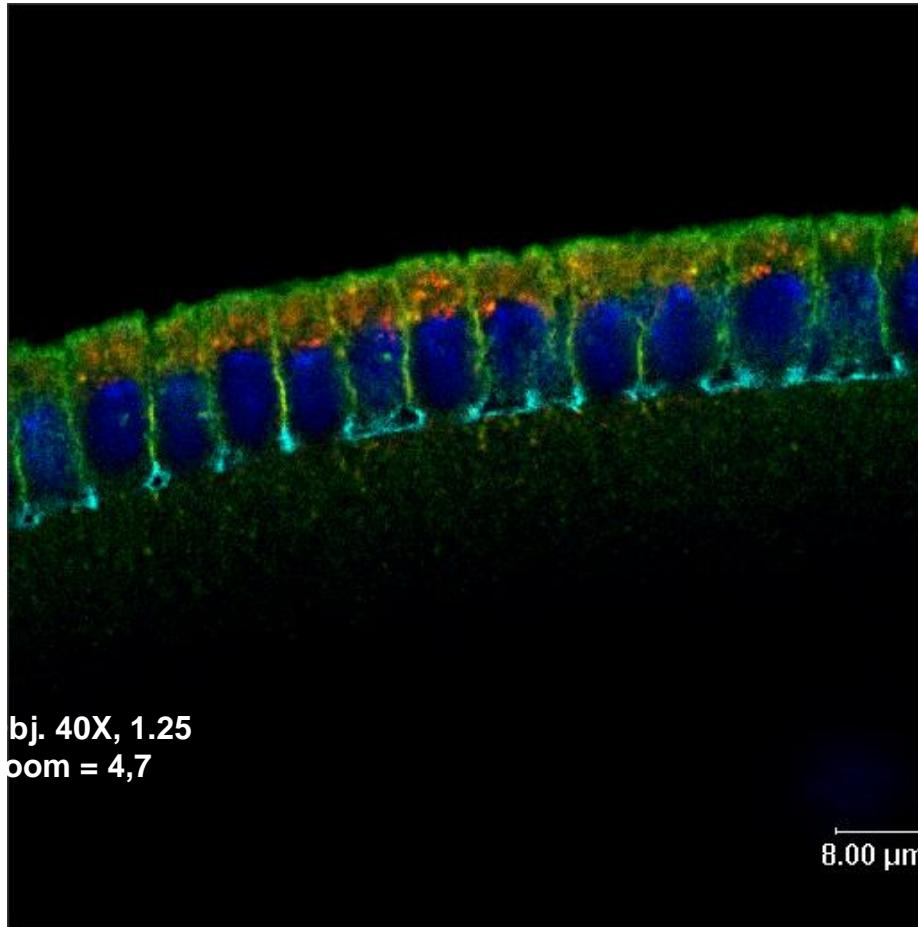




Immunohistochimie

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Embryon Drosophile



λ exc = 405 nm
 λ ém. = 422-496

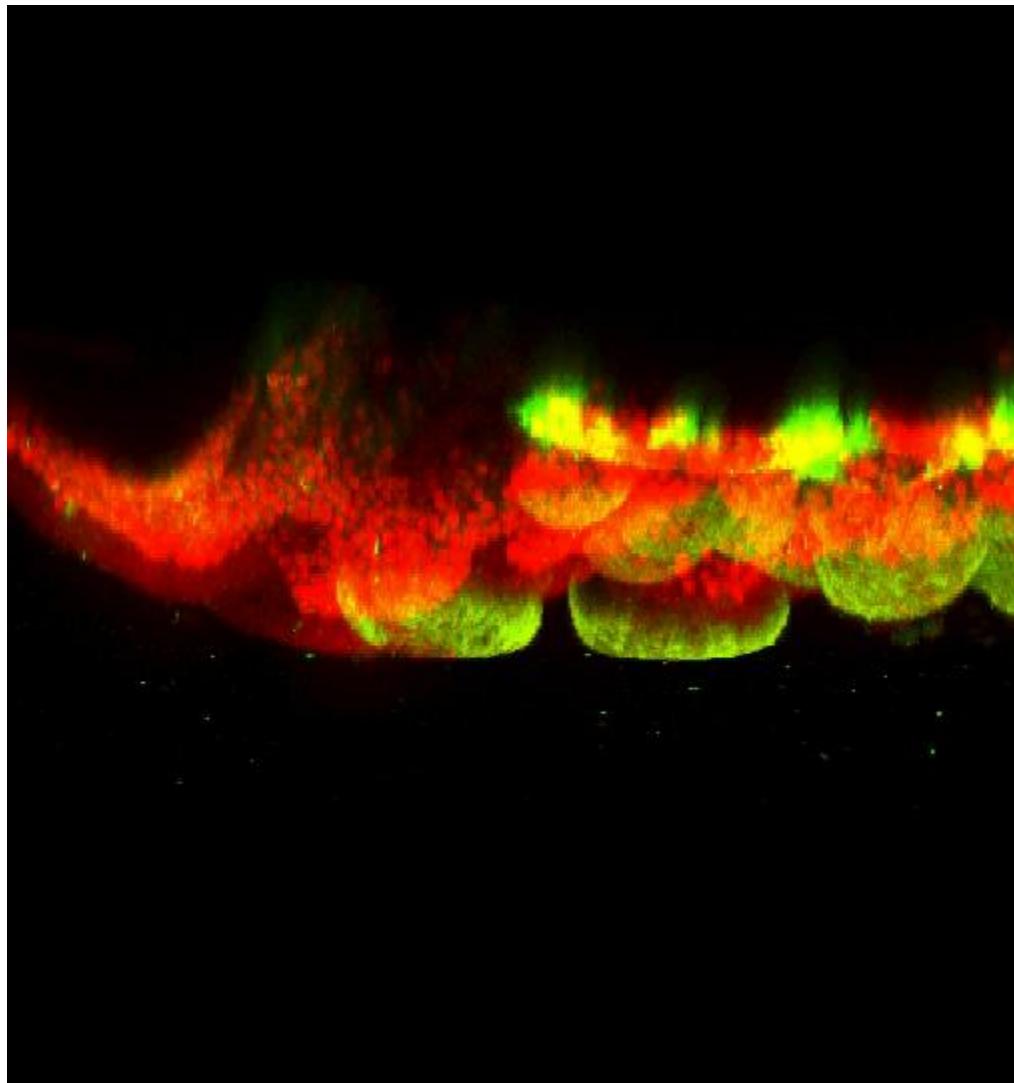
λ exc = 488 nm
 λ ém. = 496-533

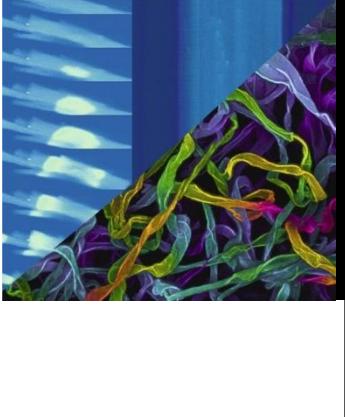
λ exc = 543 nm
 λ ém. = 556-628 nm

λ exc = 633 nm
 λ ém. = 661-690 nm

T. Lecuit, Luminy, Marseille

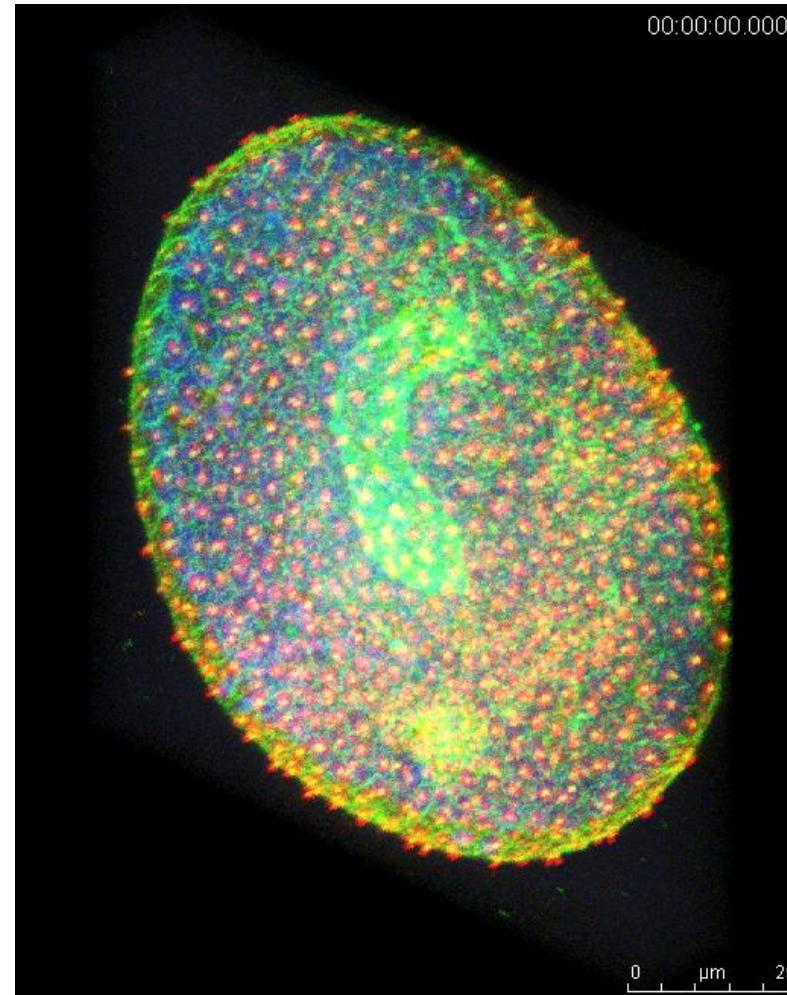
Immunohistochimie

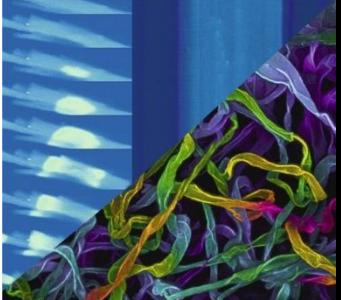




Immunohistochemie

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Immunohistochimie

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Etude de colocalisation

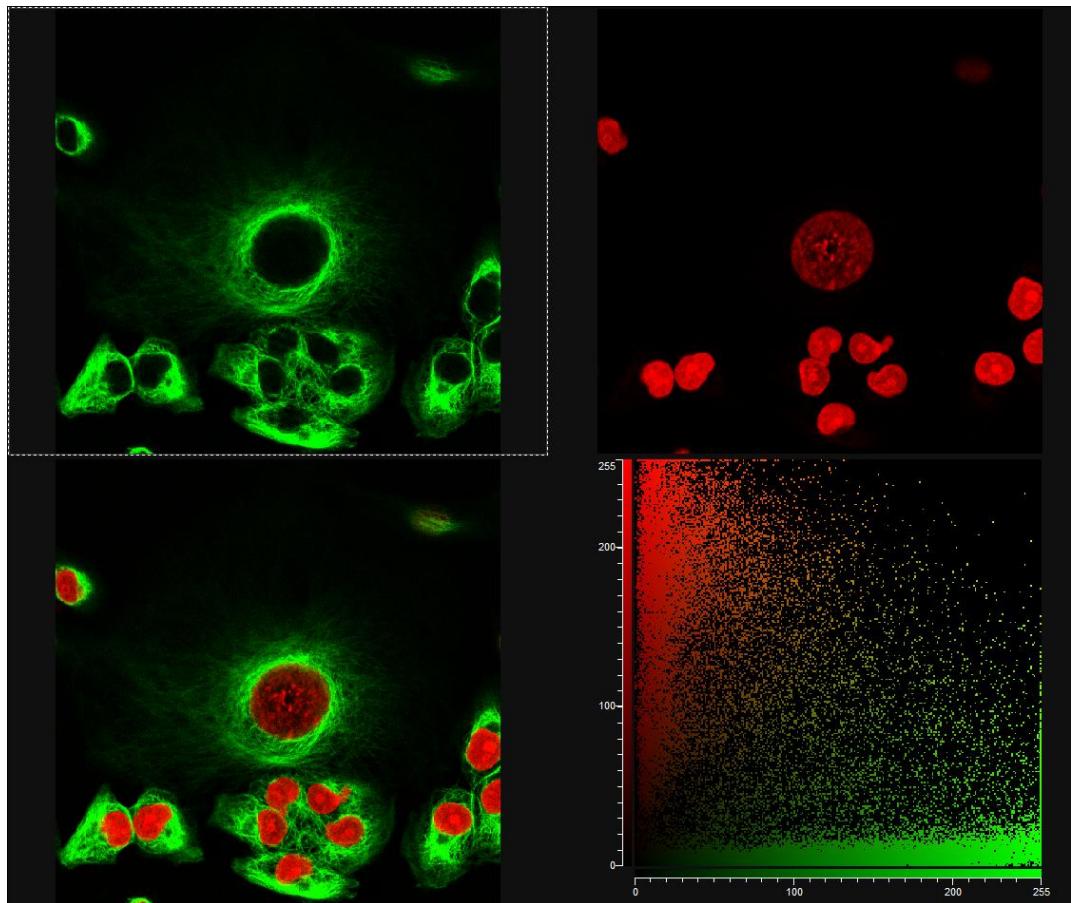
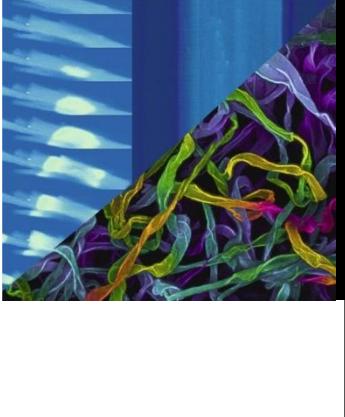


Image	
Geometric Analysis	
#Pixels	262,144
#Pixels, mask	21,397
Area [µm ²]	5,112.01
Area, mask [µm ²]	417.26
Mask area rate	8.16%
Densitometric Analysis:	
Channel 1	
Intensity sum	7,744,006
Intensity sum, mask	1,624,968
Mean intensity	29.54
Mean intensity, mask	75.94
Mask intensity rate	20.98%
Channel 2	
Intensity sum	16,348,619
Intensity sum, mask	1,484,046
Mean intensity	62.37
Mean intensity, mask	69.36
Mask intensity rate	9.08%

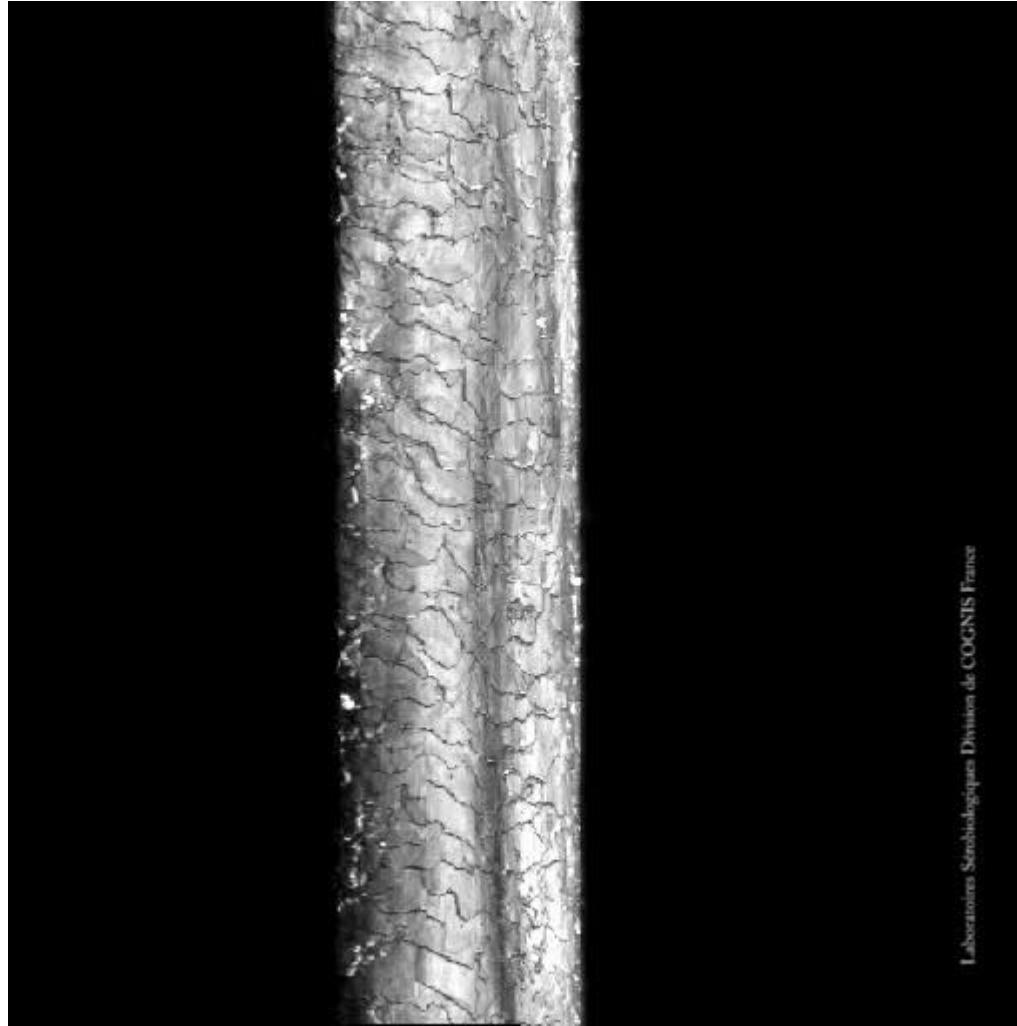


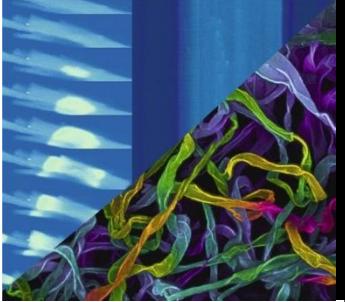
Réflexion



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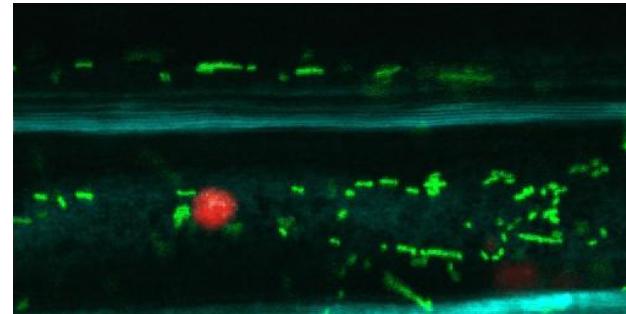
Réflexion





Time-Lapse

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Arabidopsis thaliana

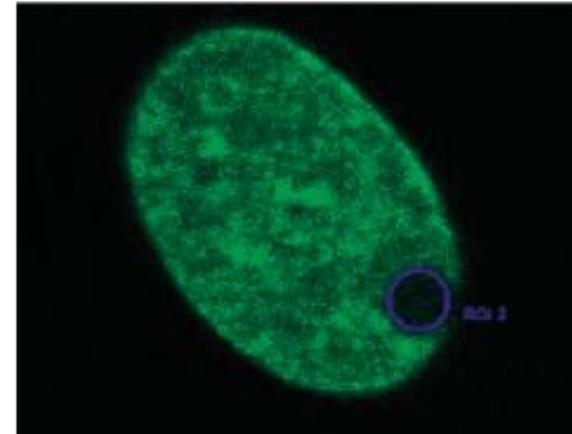
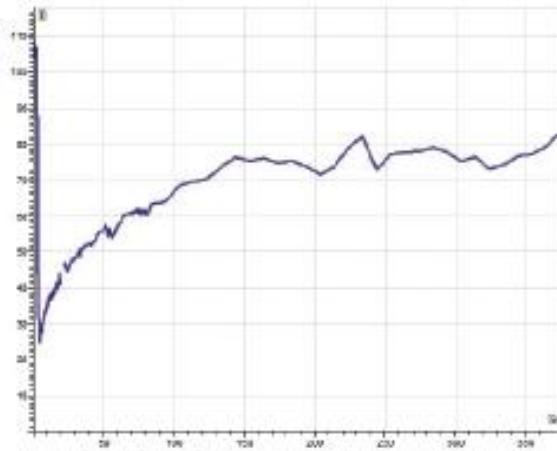
First channel: Cell wall in reflection.

2 & 3 channel: Monitoring mitochondrial (GFP-green) and plastid (autofluorescence-red) movement.

22 fps

Courtesy of Prof. Dr. D. Menzel, Institut für Zelluläre und Molekulare Botanik
Zellbiologie der Pflanzen, Bonn University.

Fluorescence Recovery After Photobleaching



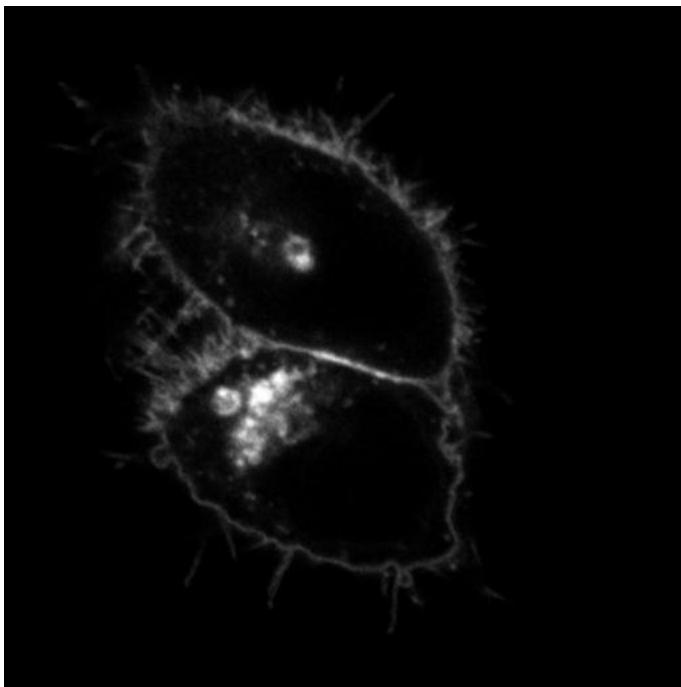
	FD464	FD464 _{theor}	H1-GFP arbitrary ROI	H1-GFP circular ROI	H1-GFP literature
M _f [%]	103	100	91	—	~ 90
t _{1/2} [s]	2.3	(1.0)	138.6	59.9	~ 55
τ [s]	3.3	(1.4)	200.9	41.5	—
D _{eff} [$\mu\text{m}^2/\text{s}$]	1.6	3.7	—	0.01	—

τ: Time constant of recovery (calculated by LCS, circular ROI)

t_{1/2}: Half-life of recovery (calculated by LCS, circular ROI)

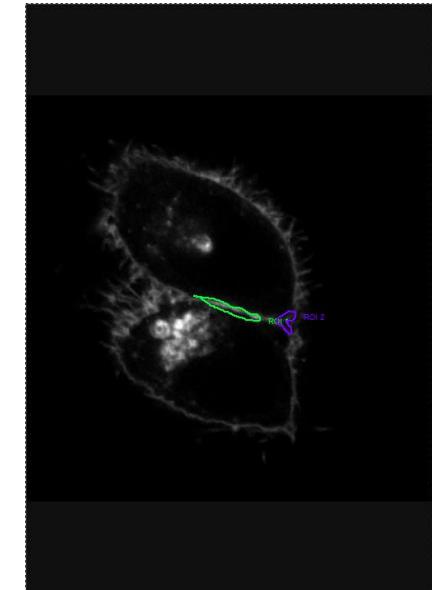
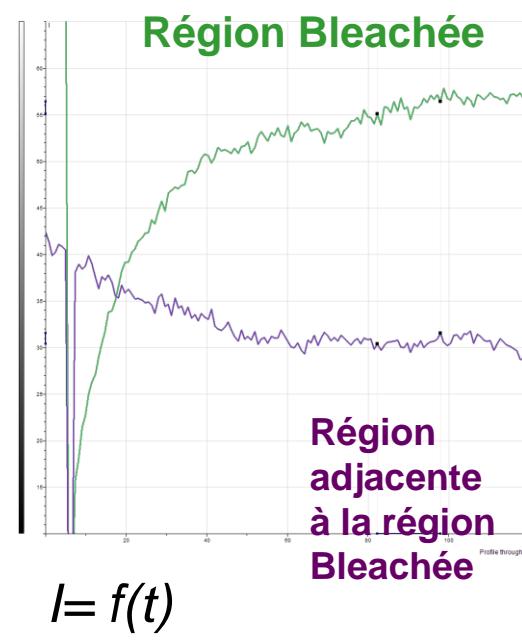
D_{eff}: Effective diffusion coefficient (Axelrod et al. 1976)

Fluorescence Recovery After Photobleaching

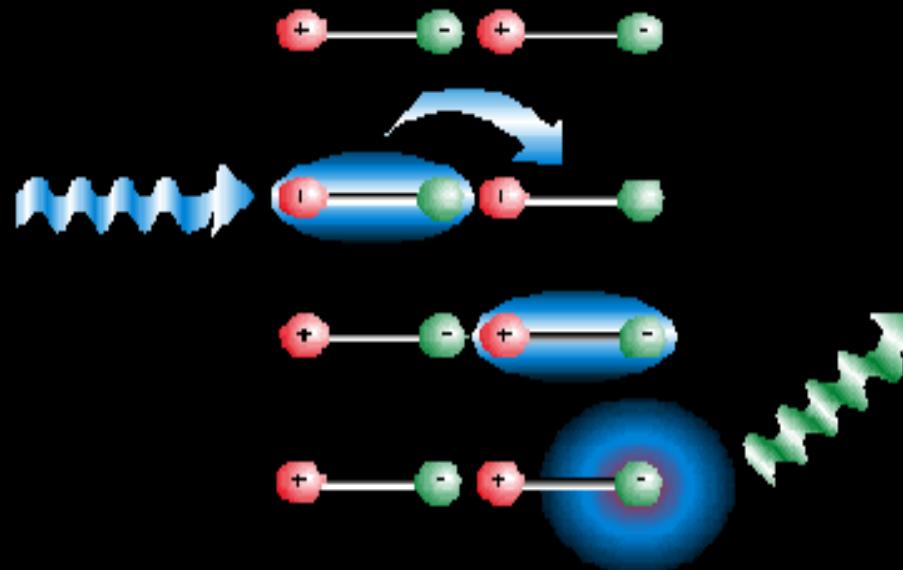


$\lambda_{\text{exc.}} = 488 \text{ nm}$
Obj. 63X, 1.32
Zoom = 4,6
 $\Delta t = 823 \text{ ms}$

T. Lecuit, Luminy, Marseille



Fluorescence Resonance Energy Transfer



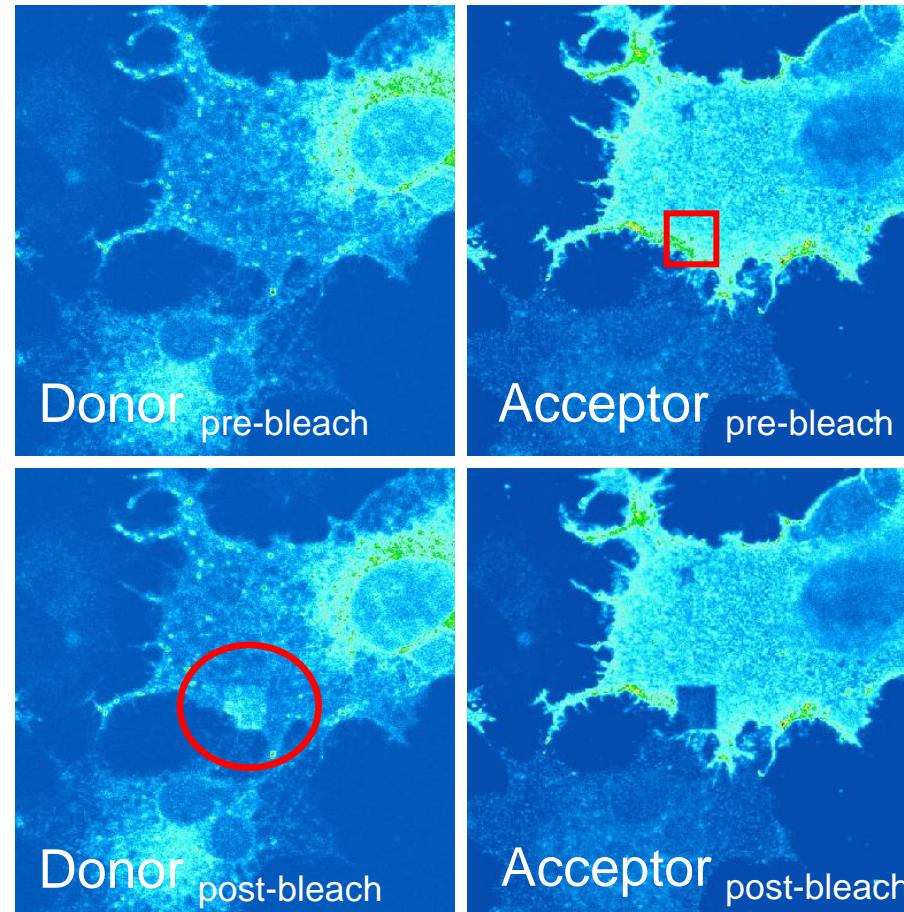
Fluorescence Resonance Energy Transfer

Bleaching de l'accepteur

Etude des modifications des interactions moléculaires

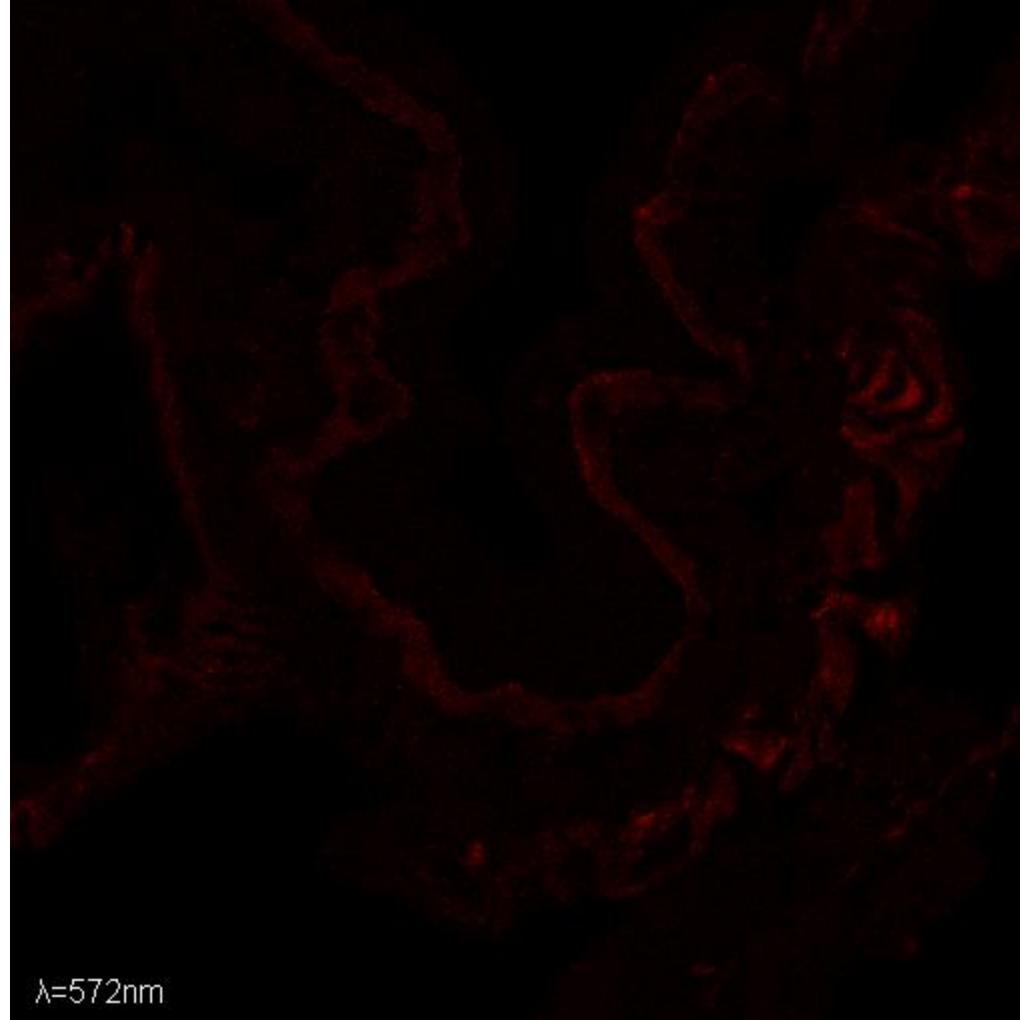
Proximité donneur-accepteur 10–100 Å

Augmentation de l'intensité de fluorescence du donneur



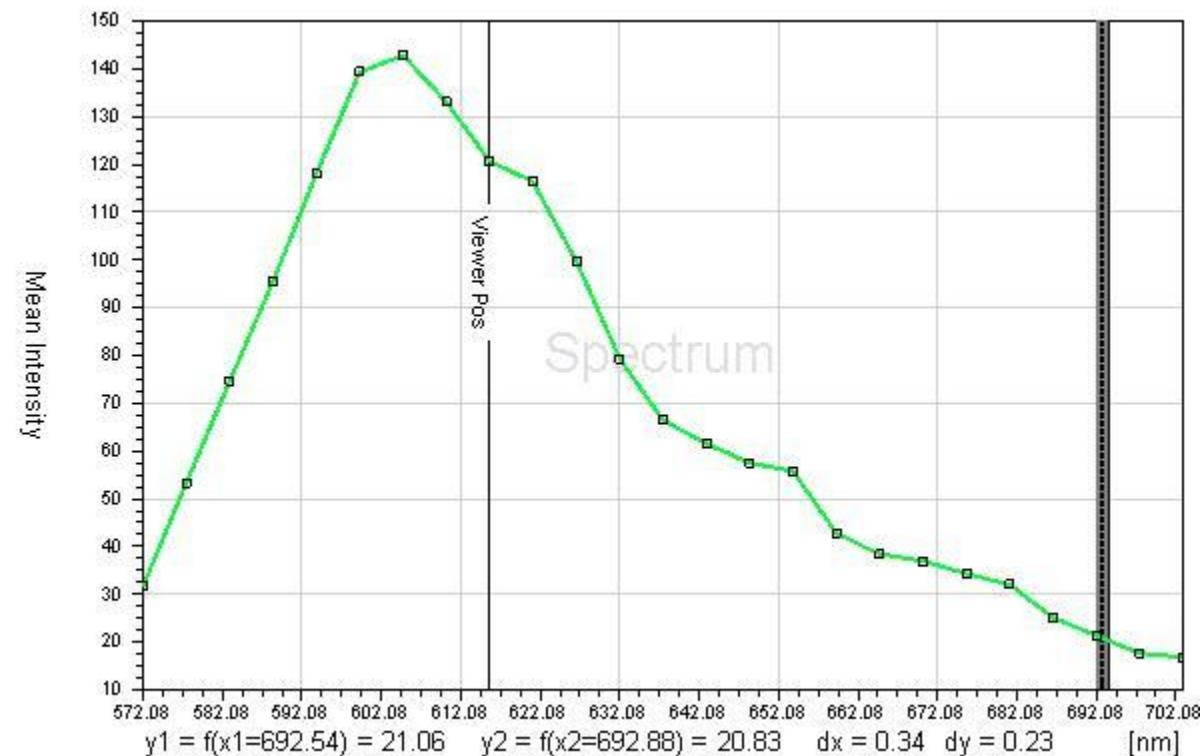
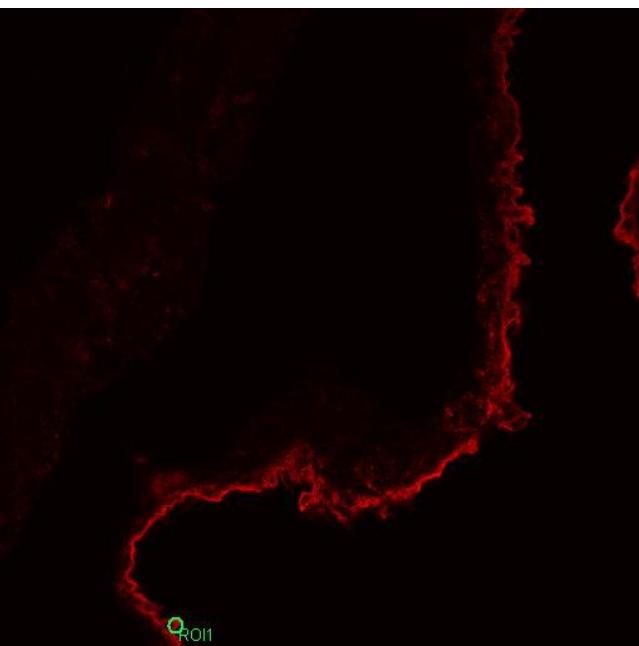
Etudes Spectrales

Spectre
d'émission de
fluorescence



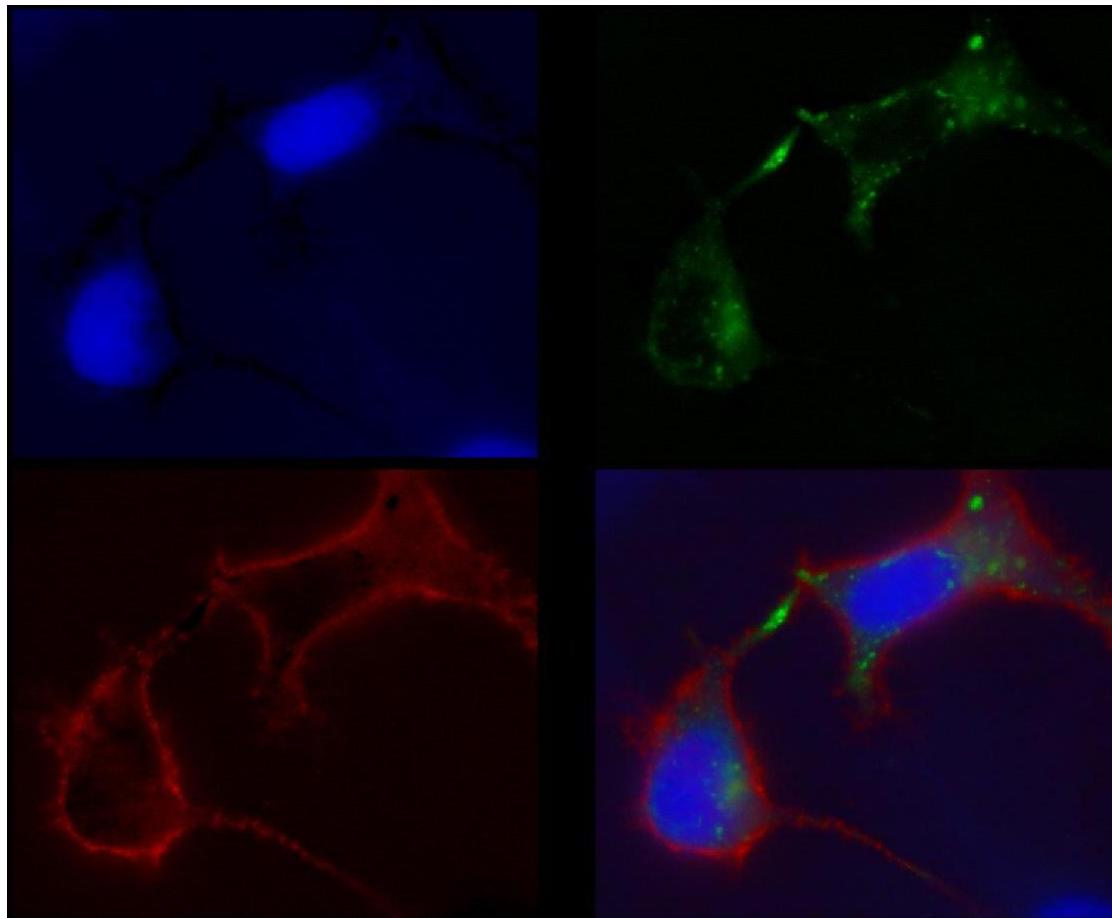
Etudes Spectrales

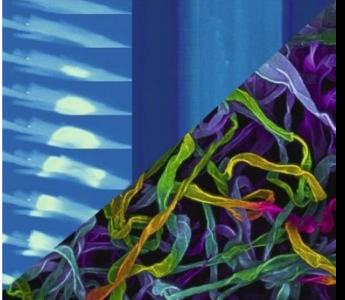
Spectres d'émission de fluorescence



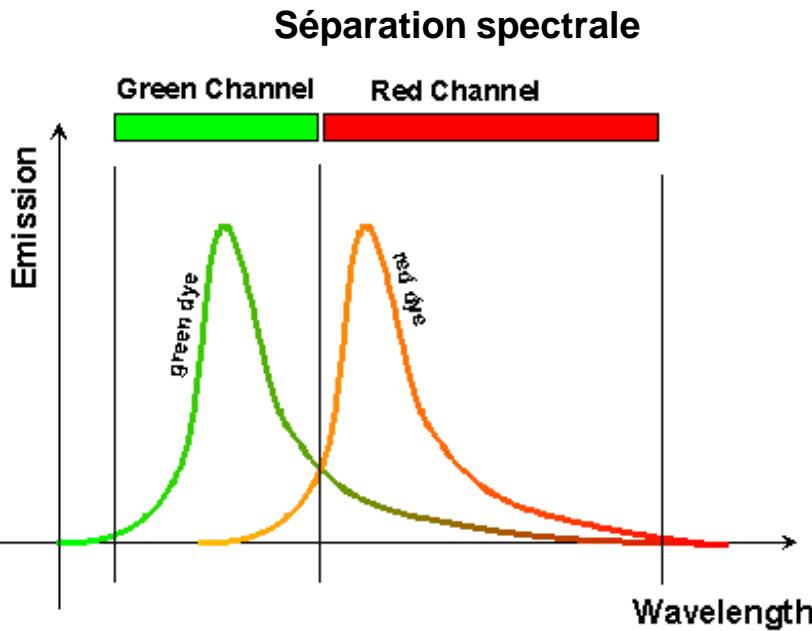
Etudes Spectrales

Séparation spectrale





Etudes Spectrales

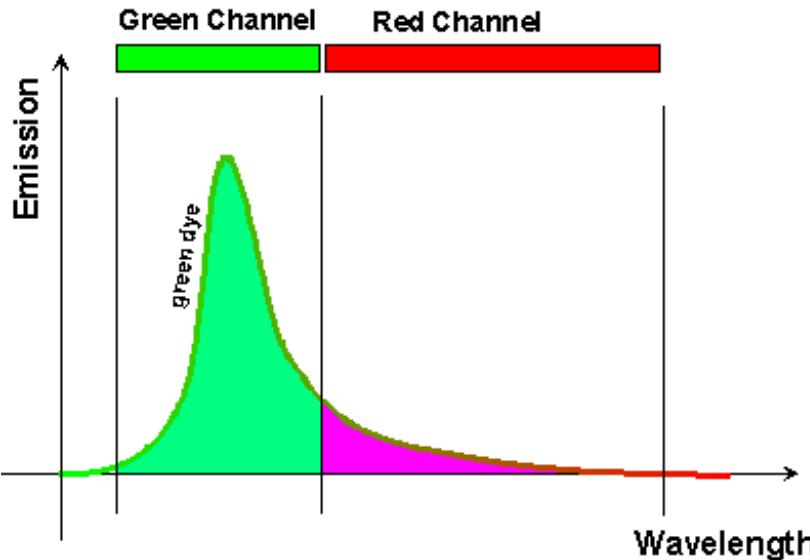


FITC/TxR sample

- 2 channel recording:
- Detection bands fine tuned
 - No gaps between bands
 - High efficient prism
 - High efficient PMTs
 - AOBS® applied

Etudes Spectrales

FITC



The total of all light collected from FITC molecules will be distributed into both channels.

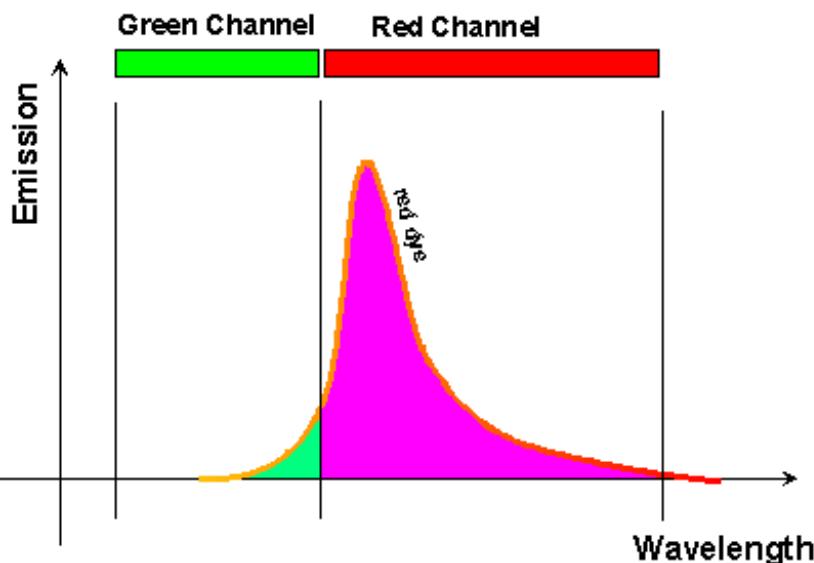
We assume here:

$\frac{3}{4}$ of all FITC emission go into the green channel (G)

$\frac{1}{4}$ of all FITC emission goes into the red channel (R)

Etudes Spectrales

TxR



The total of all light collected from TxR molecules will be distributed into both channels.

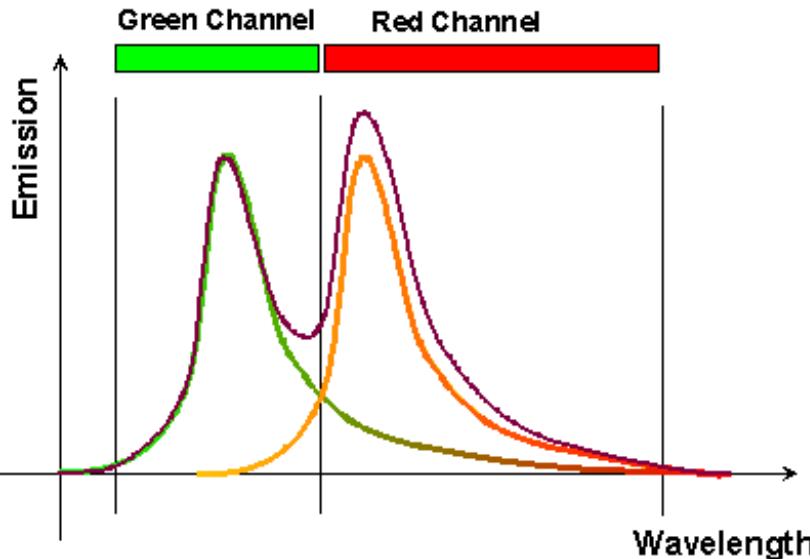
We assume here:

1/5 of all TxR emission goes into the green channel (G)

4/5 of all FITC emission goes into the red channel (R)

Etudes Spectrales

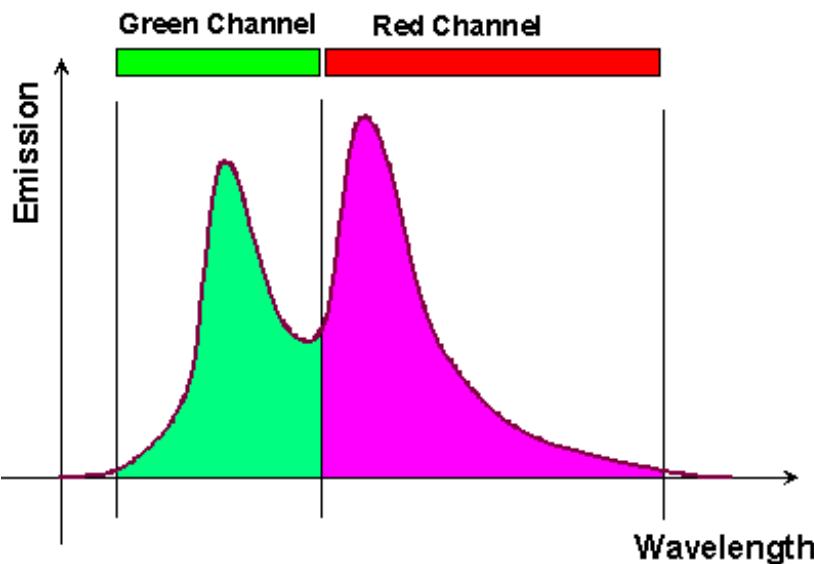
Both dyes



In a real experiment, we will have both dyes simultaneously in the sample and therefore get signals from both dyes in both channels.

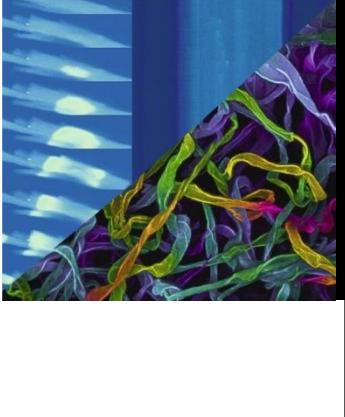
Etudes Spectrales

A calculated measurement

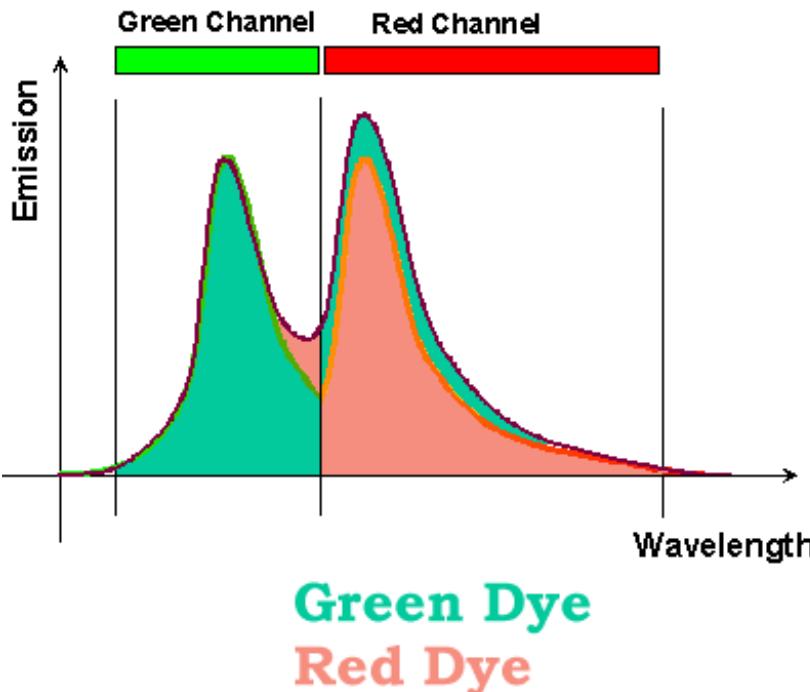


$$G = \frac{3}{4} \text{FITC} + \frac{1}{5} \text{TxR}$$

$$R = \frac{1}{4} \text{FITC} + \frac{4}{5} \text{TxR}$$



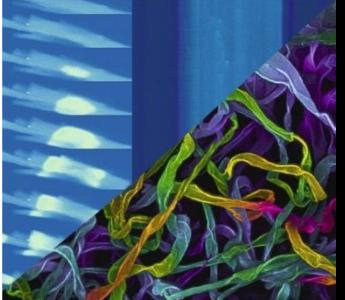
Etudes Spectrales



Unmixing is:
Solving sets of n linear
equations with n unknowns.

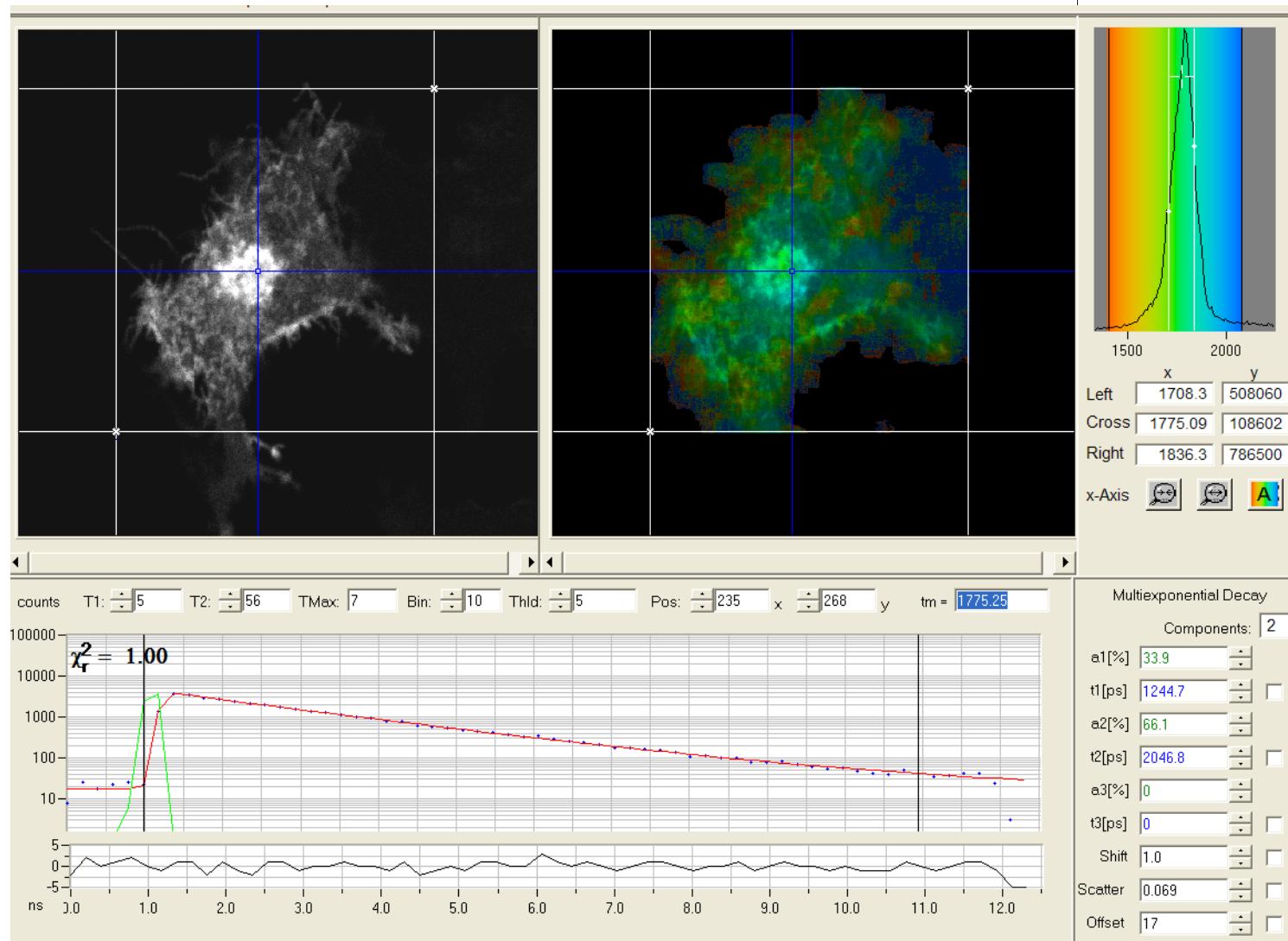
First proven records of
solutions go back some 4000
years (Egypt)

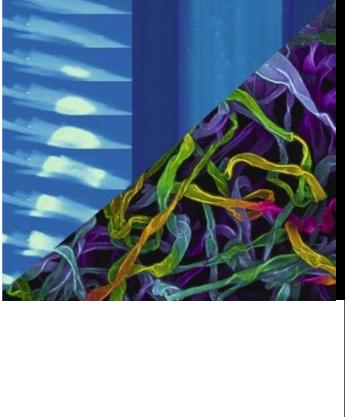
For a reference see:
[http://www.ETH\EducETH - Mathematik -
Leitprogramm Lineare
Gleichungssysteme.htm](http://www.ETH\EducETH - Mathematik - Leitprogramm Lineare Gleichungssysteme.htm)



Fluorescence Lifetime Imaging Microscopy FLIM

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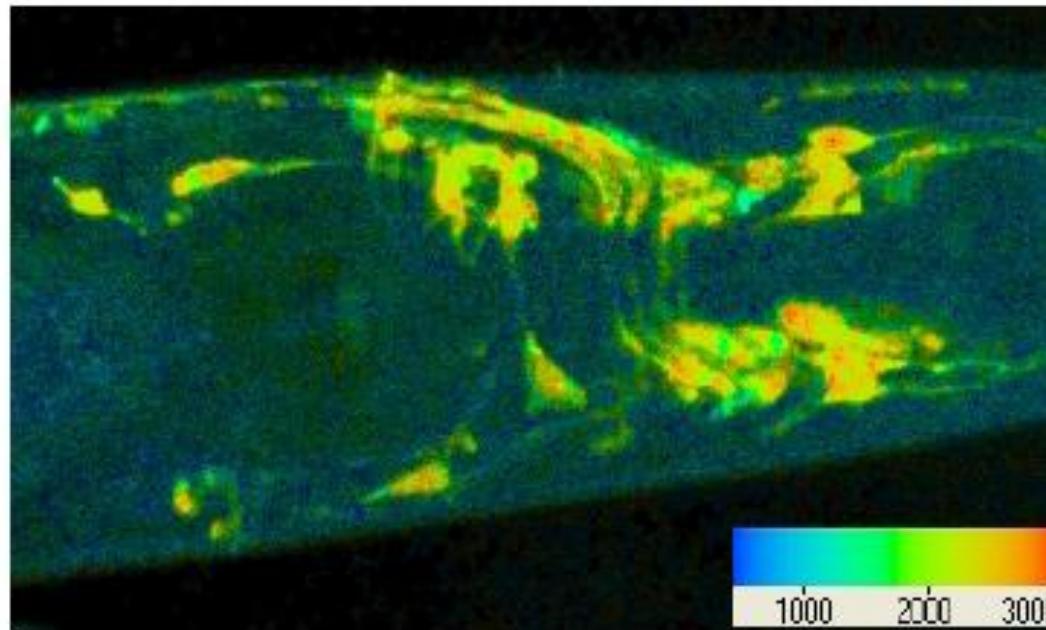




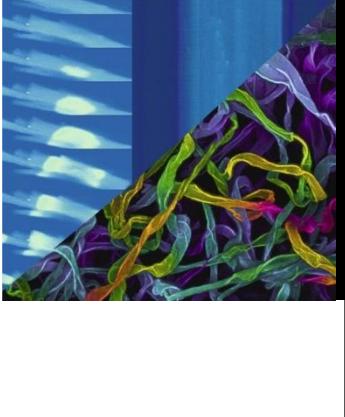
Fluorescence Lifetime IMaging

FLIM

Leica
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Fluorescence lifetime image of a *C. elegans*. The different lifetime colours derive from various fluorescent proteins (CFP, GFP, YFP). Courtesy H. Hutter.



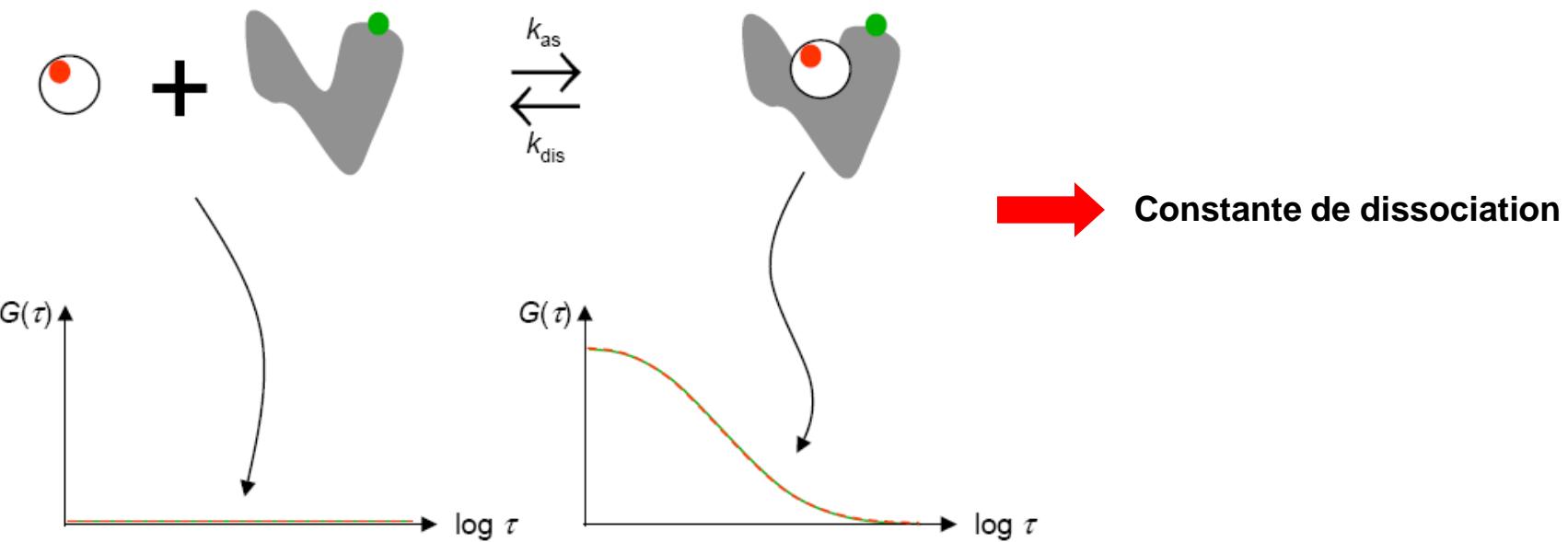
Fluorescence Correlation Spectroscopy

Leica
MICROSYSTEMS

Lien entre la diffusion de molécules et la fluctuation de l'intensité de fluorescence dans un volume donné

→ Concentration

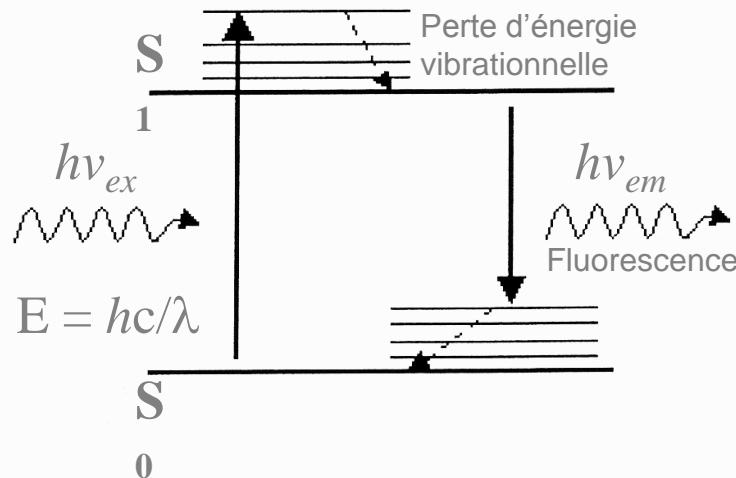
→ Coefficient de diffusion



Principe de l'excitation à deux photons

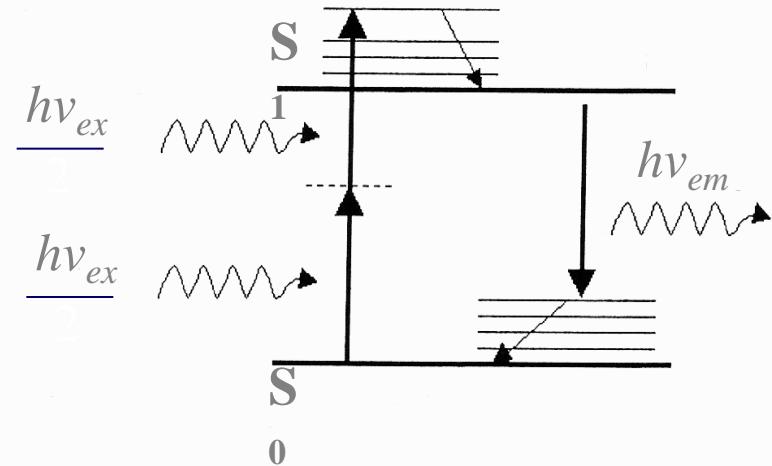
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Processus de fluorescence en excitation à un photon



L'énergie d'un seul photon est absorbée par un fluorochrome pour passer d'un état d'énergie basal (S_0) à un état excité (S_1)

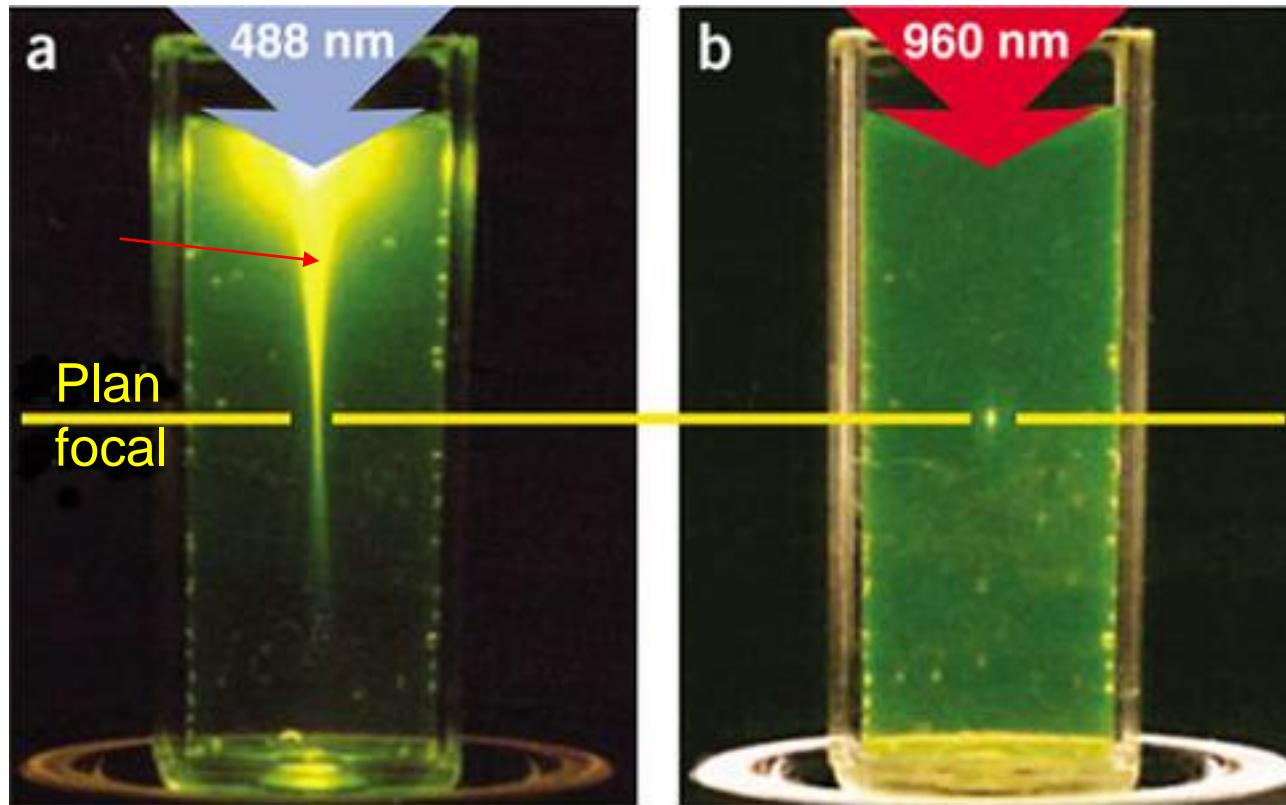
Processus de fluorescence en excitation à deux photons



Deux photons d'énergie deux fois plus faible (et donc de longueur d'onde deux fois plus élevée) sont absorbés par la molécule dans un laps de 10^{-16} s

- Les caractéristiques du rayonnement émis par le fluorochrome en excitation à deux photons sont inchangées

En microscopie à balayage laser à deux photons, l'excitation est
strictement restreinte au volume focal



Fluorescence suite à une
absorption à un photon

Fluorescence suite à une
absorption à deux photons

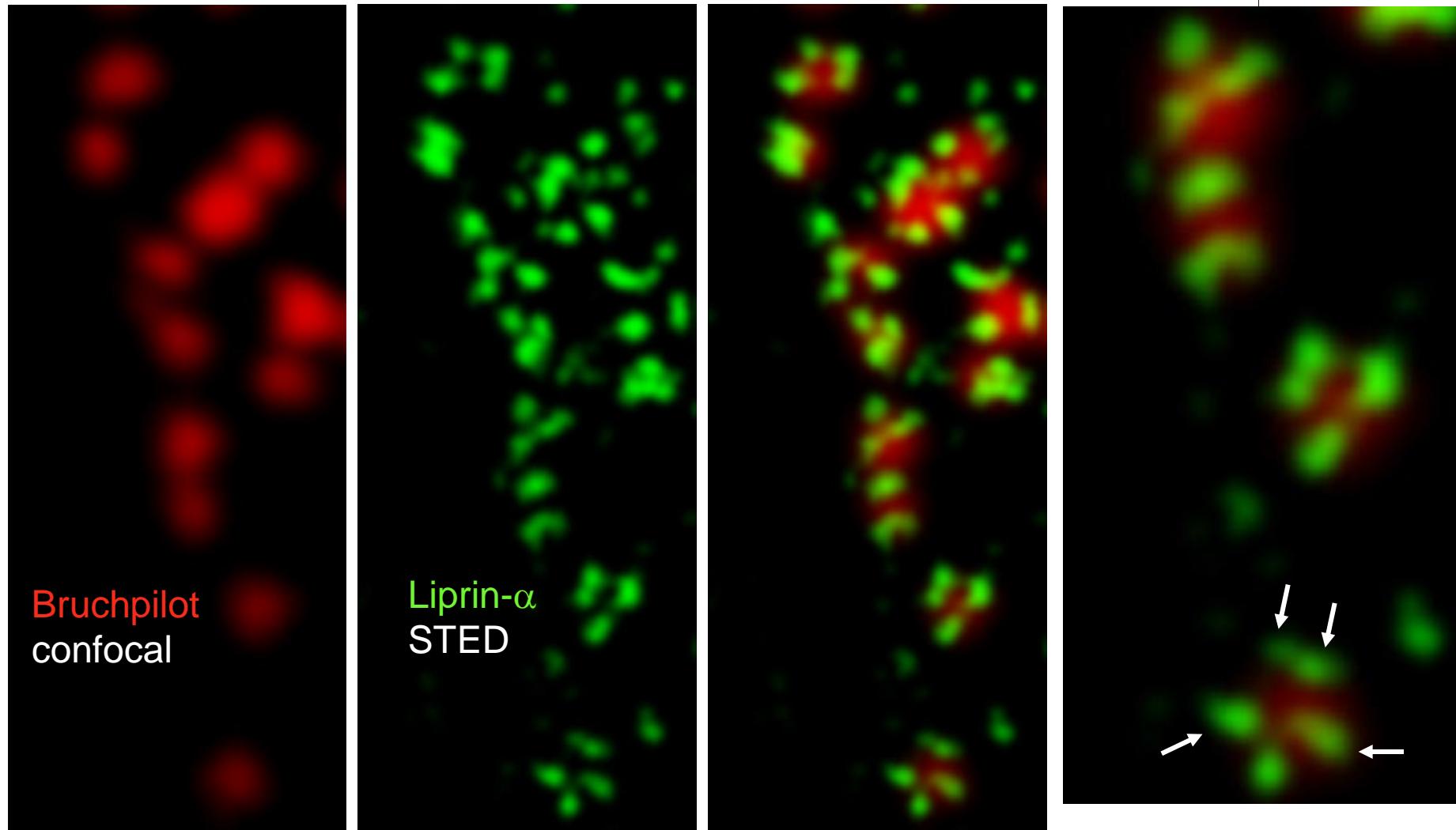
Leica TCS STED



Leica
MICROSYSTEMS

Multicolor Image of the NMJ

Leica
MICROSYSTEMS



Courtesy of Prof. Stephan Sigrist

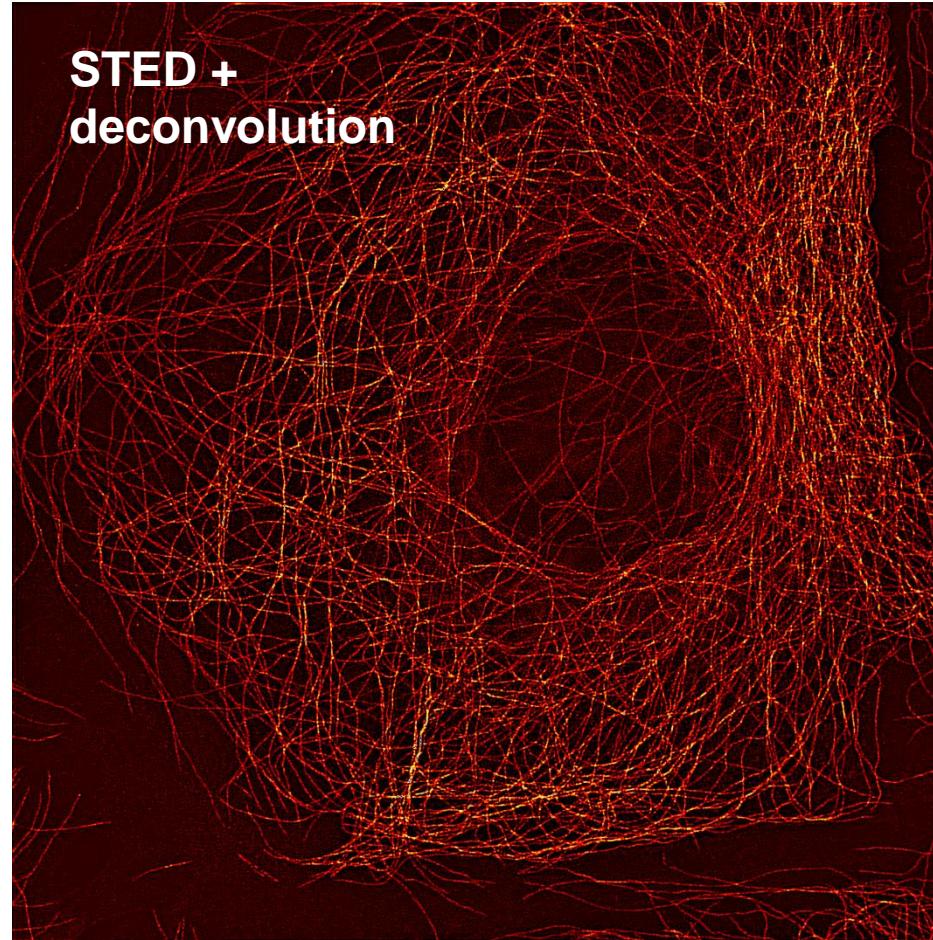
500 nm

74

Resolution Increase by STED: Pure Physics!

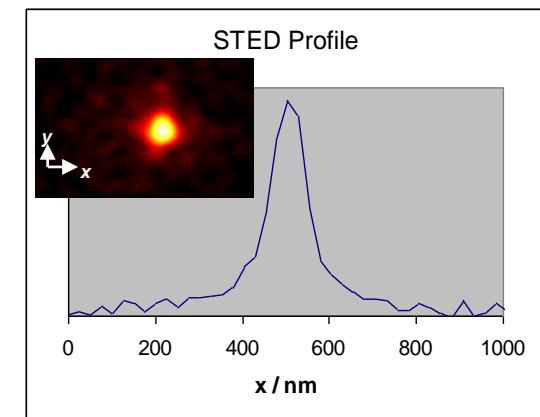
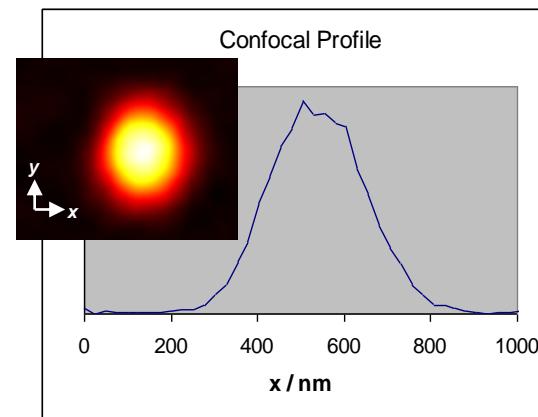
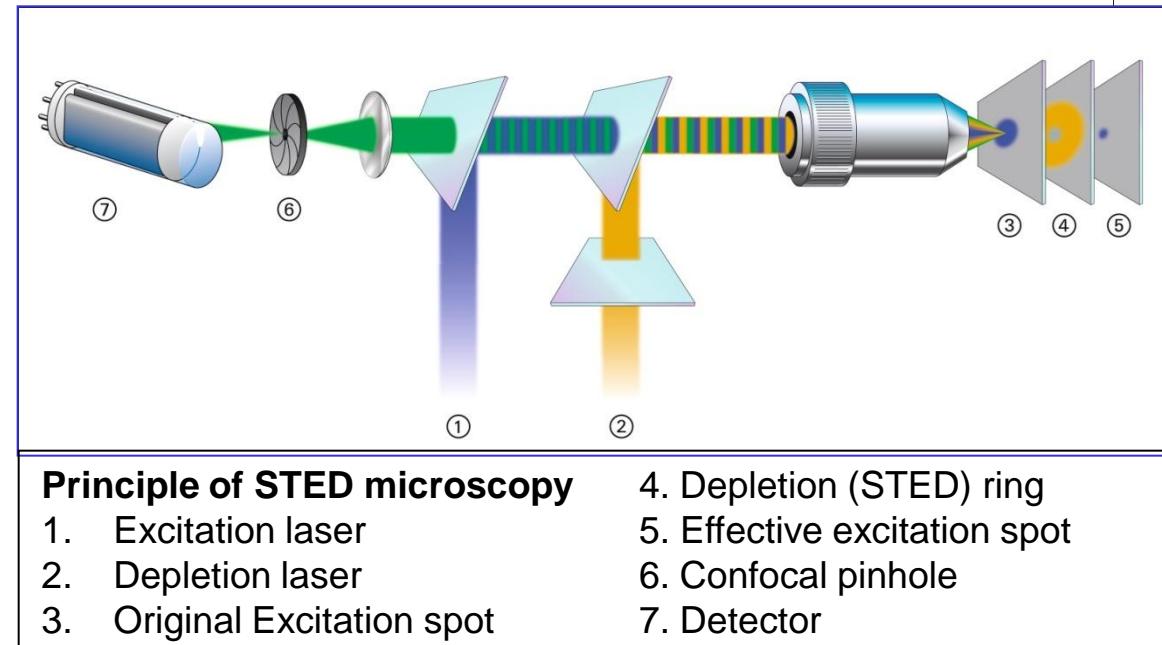
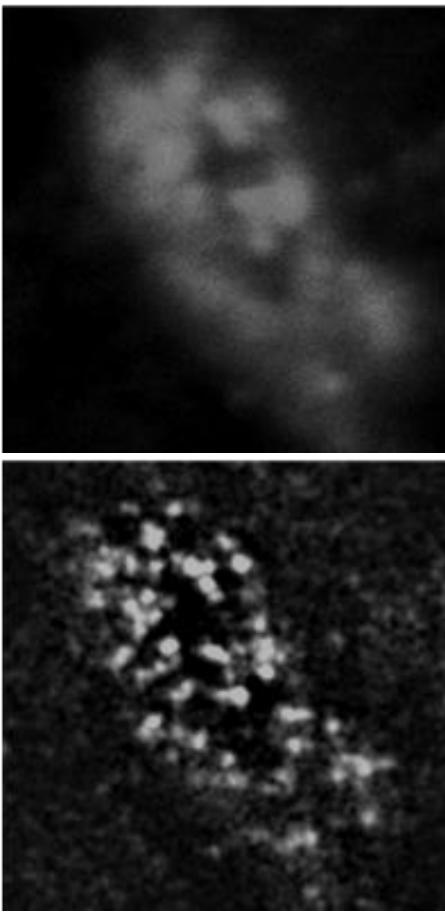
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STED is pure physics! But you can add mathematics on top!



Optical pathway

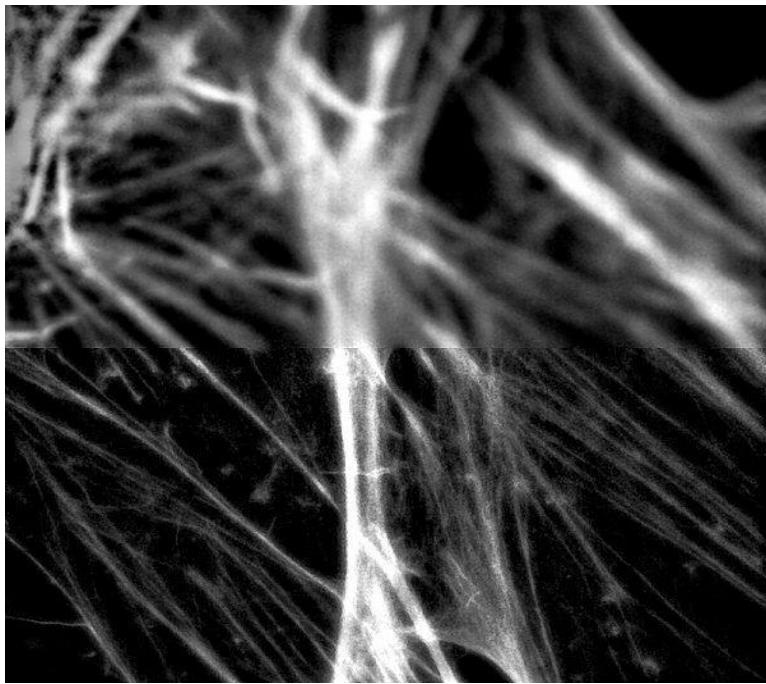
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Formation of presynaptic active zone (Liprin)
Courtesy S. Sigrist,
Wuerzburg

Typical lateral resolution: **200x200 nm**

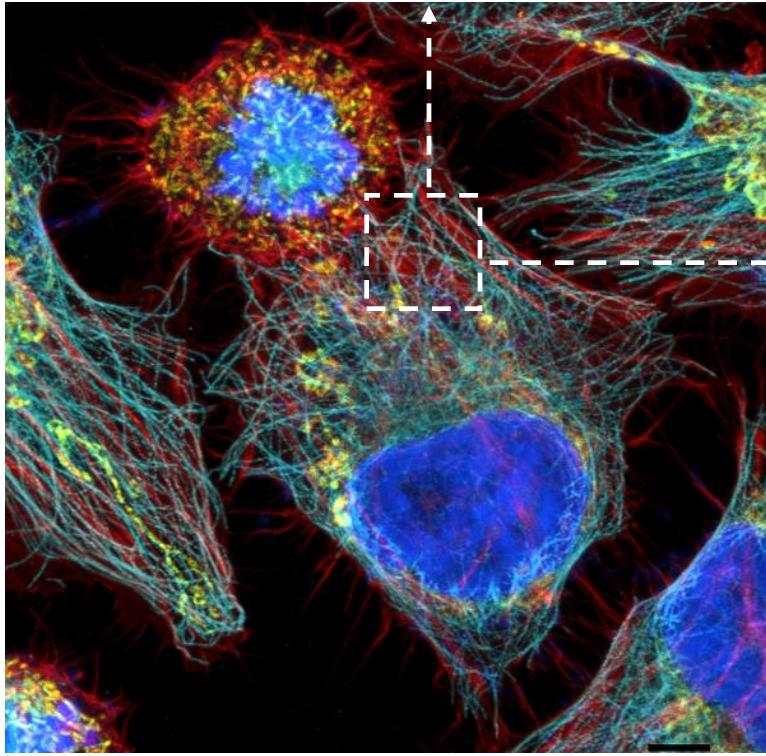
Typical lateral FWHM in STED is **90x90 nm⁷⁶**



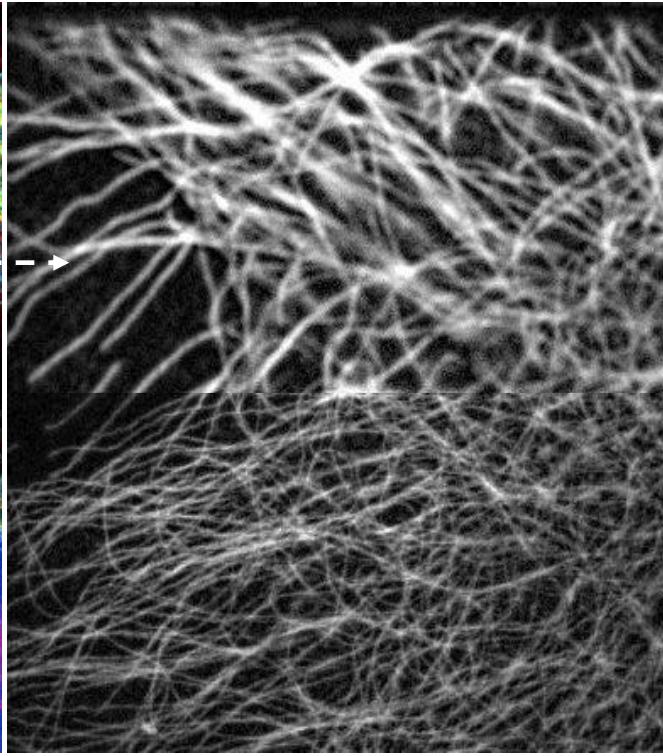
ACTIN

Confocal

Leica
MICROSYSTEMS



STED



MICROTUBULES

Confocal

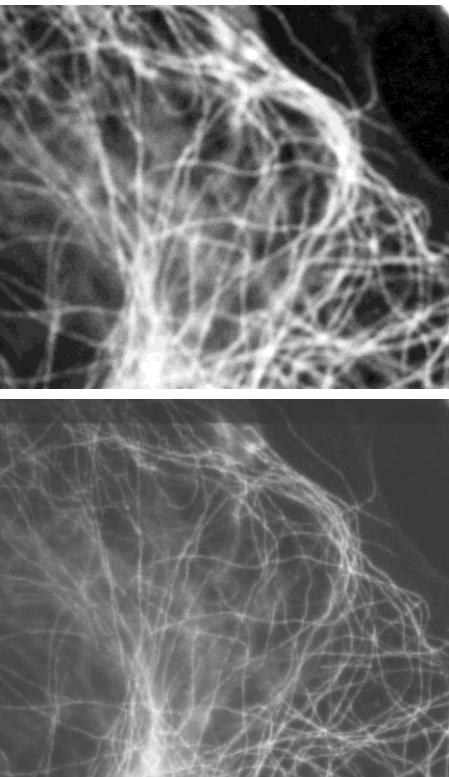
STED

The task

Increase xy resolution in fluorescence microscopy over classical Abbe limits:

$$d_{xy} = \frac{\lambda}{2n \cdot \sin \alpha}$$

FWHM_{confocal, xy}: 200 nm



Microtubules of a
Vero cell

SOME EXAMPLES:

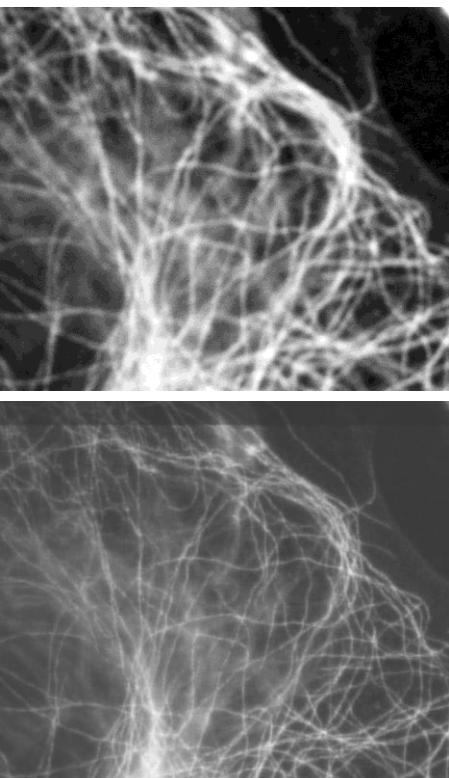
- Neurophysiology (Synapse-cell-interactions, motoneurons etc.)
- Endocytotic processes
- Virus biology (Malaria, AIDS)
- Pathology (Multiple Sclerosis etc.)

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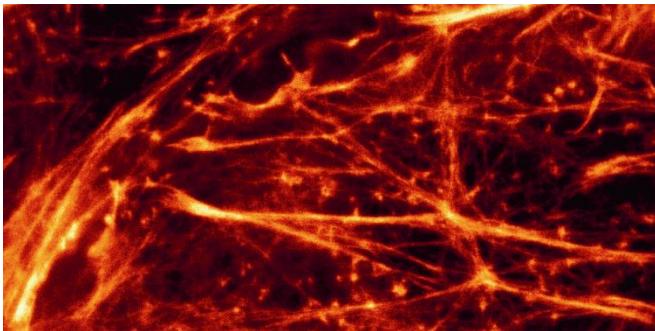
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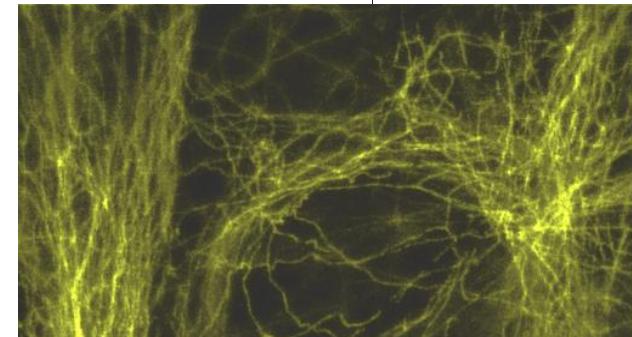
Applications Example - Cell Biology

Leica
MICROSYSTEMS

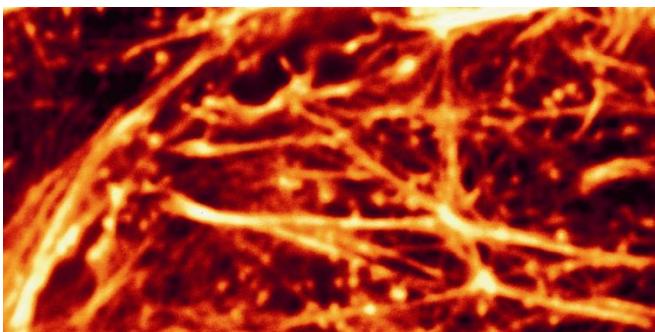


STED

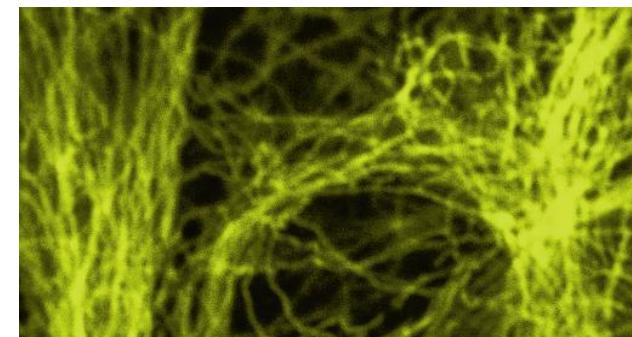
F-Actin



β -Tubulin

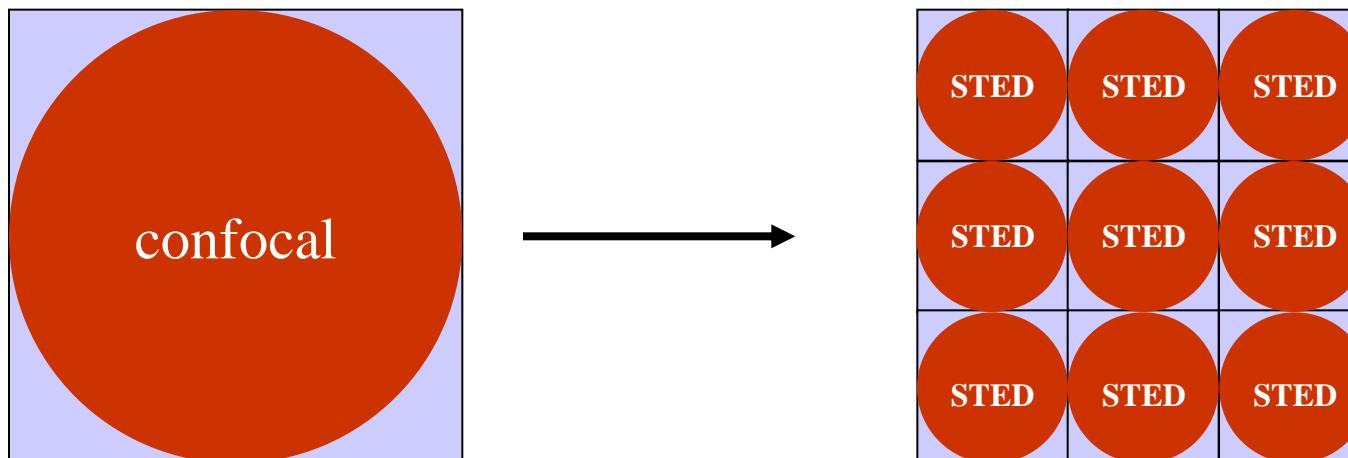
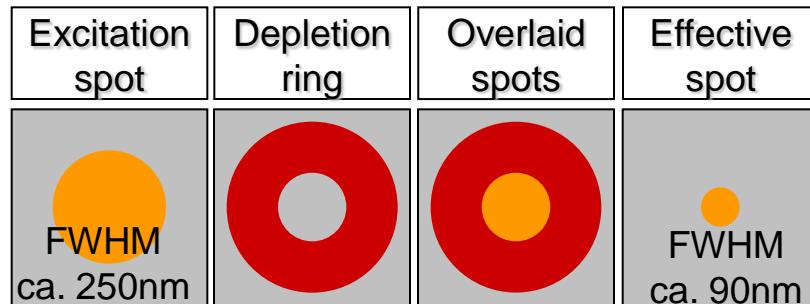


Confocal



Nice for demonstrational purposes

Resolution enhancement by STED:



A threefold improved resolution can make 9 spots out of 1 !

Microscopie Confocale

- Introduction
 - Historique
 - Fluorescence
 - Résolution
 - Microscopie Confocale
- Applications et exploitation des données
 - Immunomarquages
 - Réflection
 - Time-Lapse
 - Etudes spectrales
 - F-Techniques
 - FCS/FLIM
- Conclusion

Conclusion

- **Technique d'imagerie à haute résolution**
- **Large domaine d'application**
- **Exploitation des images brutes**
- **Système commercial entièrement motorisé**
- **Système évolutif**

Ca y est vous êtes libres !!!